



The enriched connectome:  
*From* links between  
**structural** and **functional**  
connectivity  
*to* quantitative plasticity of  
brain connectivity

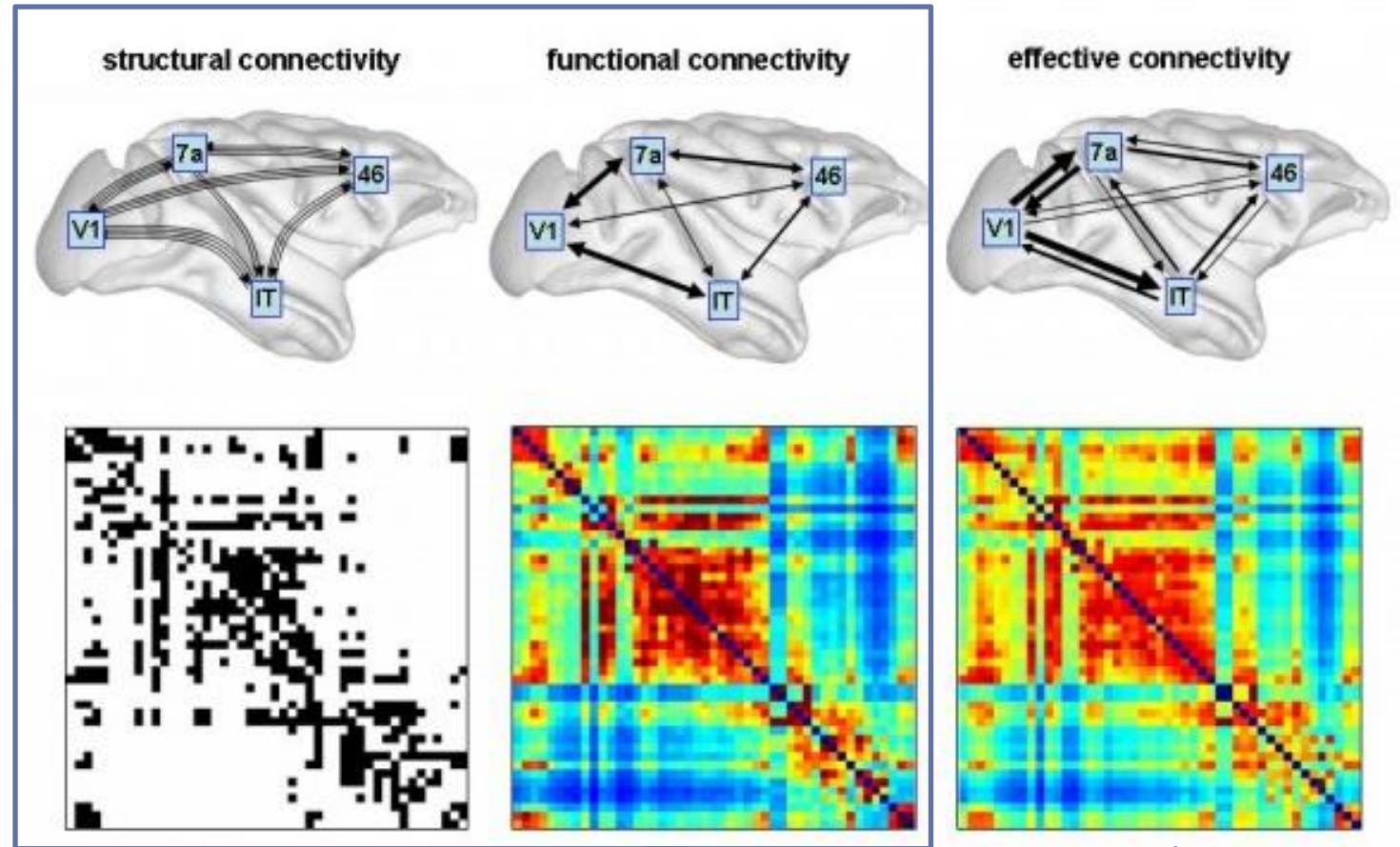
Alfred Anwander

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for Human Cognitive and Brain Sciences  
Leipzig, Germany



## Two ways to measure the humane connectome with (MRI)

- Based on the brain structure: white matter fiber structure
- Based on brain activity: **symmetric statistical relationship**

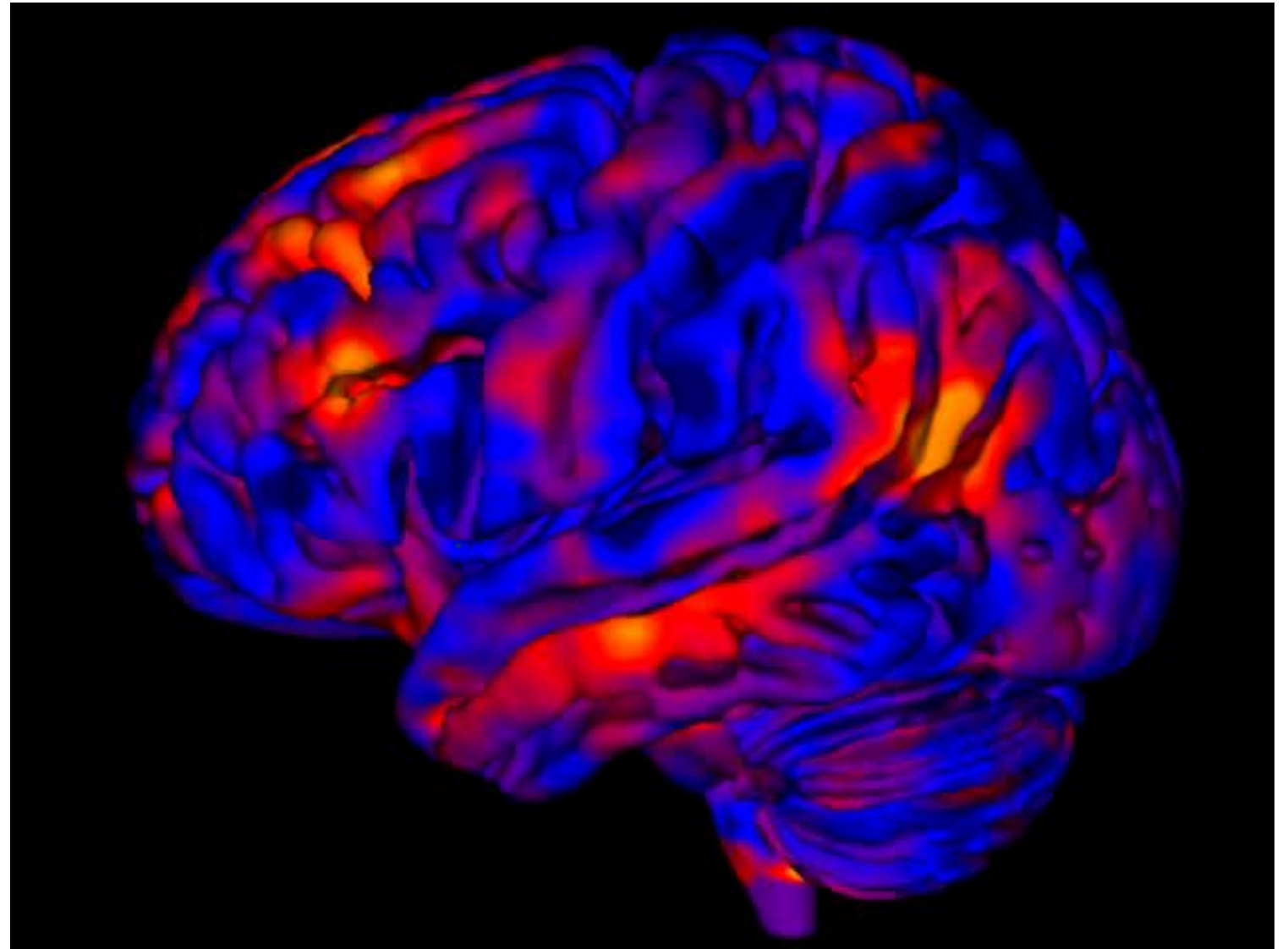


*Sporns Scholarpedia 2007, Sporns Discovering the Human Connectome 2012*



## Low frequency brain activity – rs fMRI

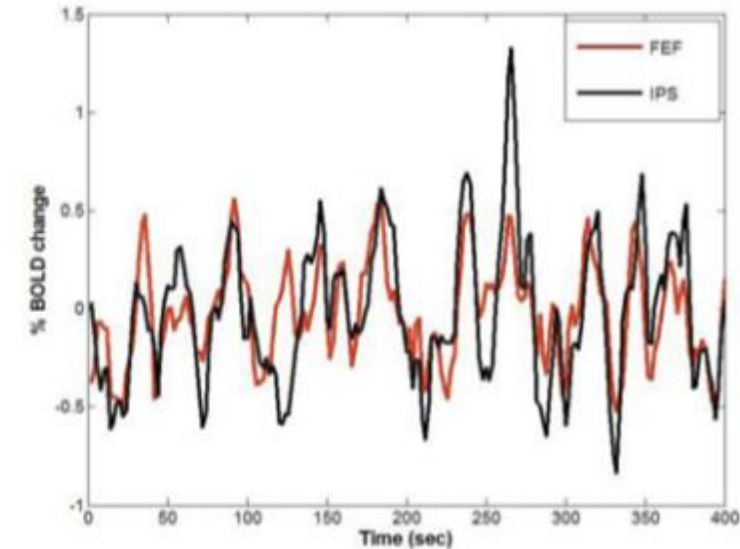
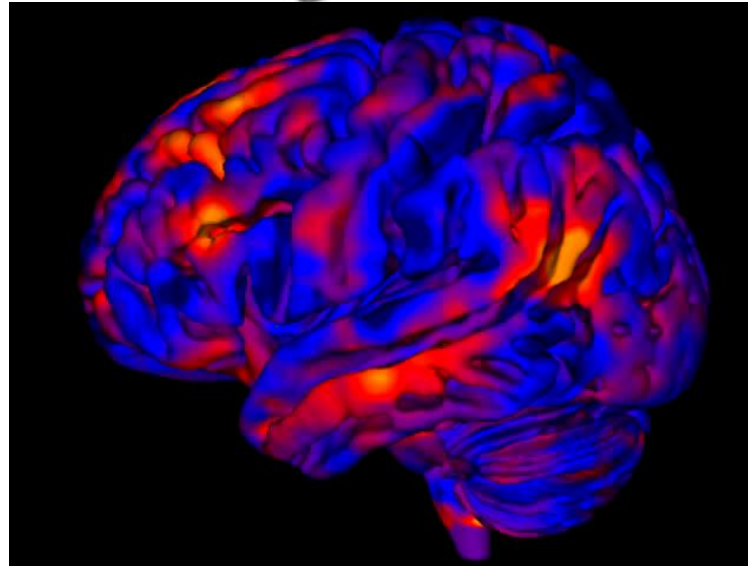
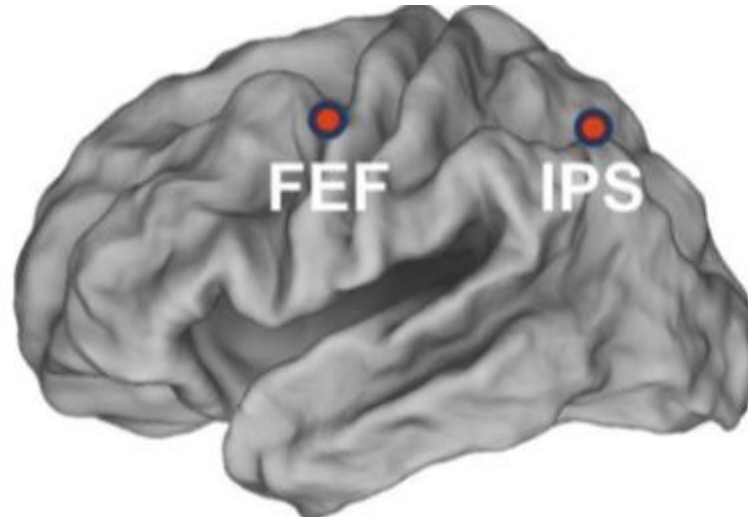
- Hemodynamic signal fluctuations
- Task-free “resting state” fMRI BOLD signal (blood oxygen level dependent)





## Synchronization of the functional MRI time series

- Statistical dependence:
  - Cross-correlations between nodes
- Example:
  - Seed voxel in the frontal eye field and in the intraparietal sulcus

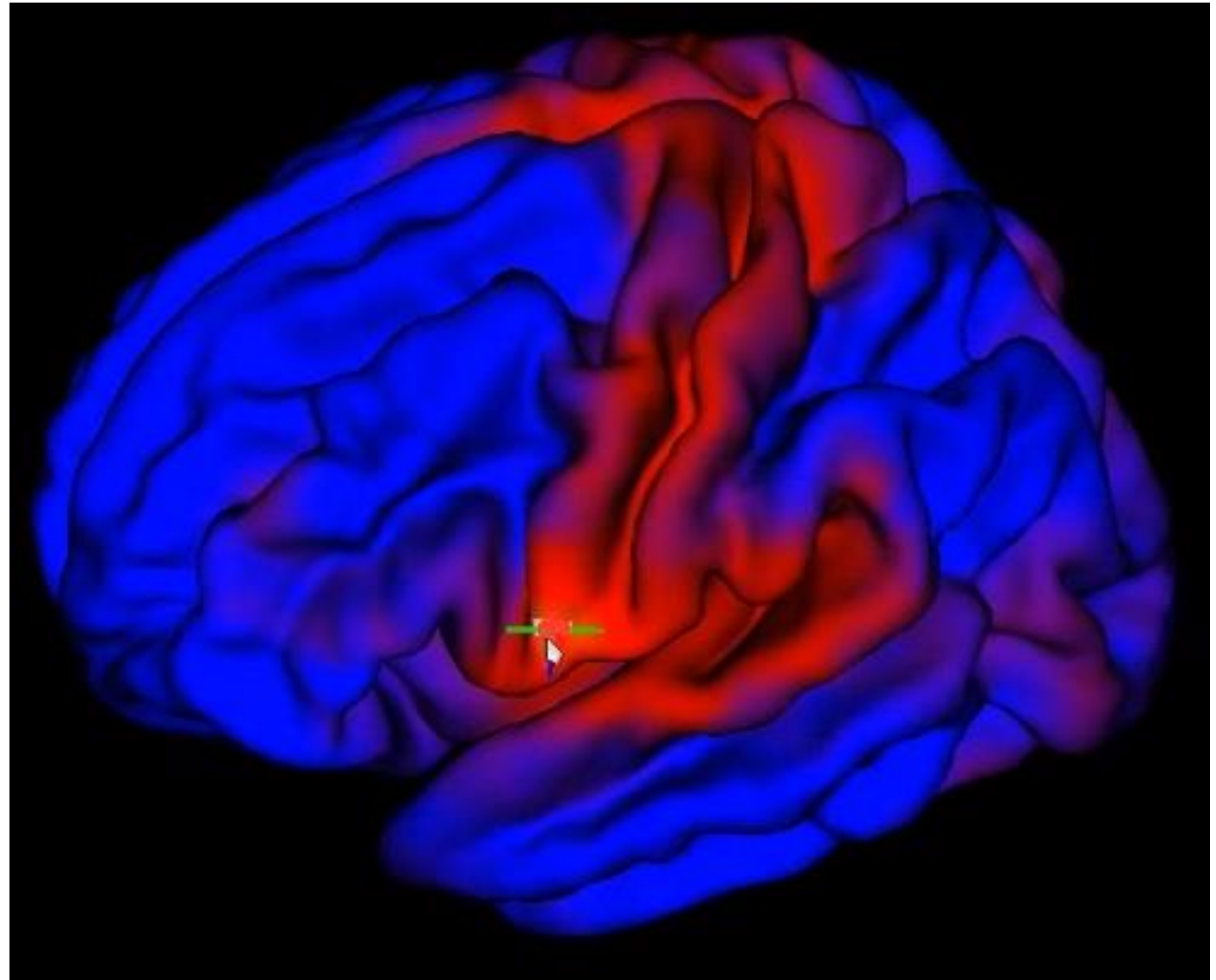


*Shimony et al. 2009; Fox – Raichle 2007; van den Heuvel et al. 2010 Raichle, 2011*



## Functional connectivity: Similarity of the fMRI time series

- Correlations of individual seed voxels show synchronized areas
- Statistical dependencies over long sampling epochs (6-10 min)



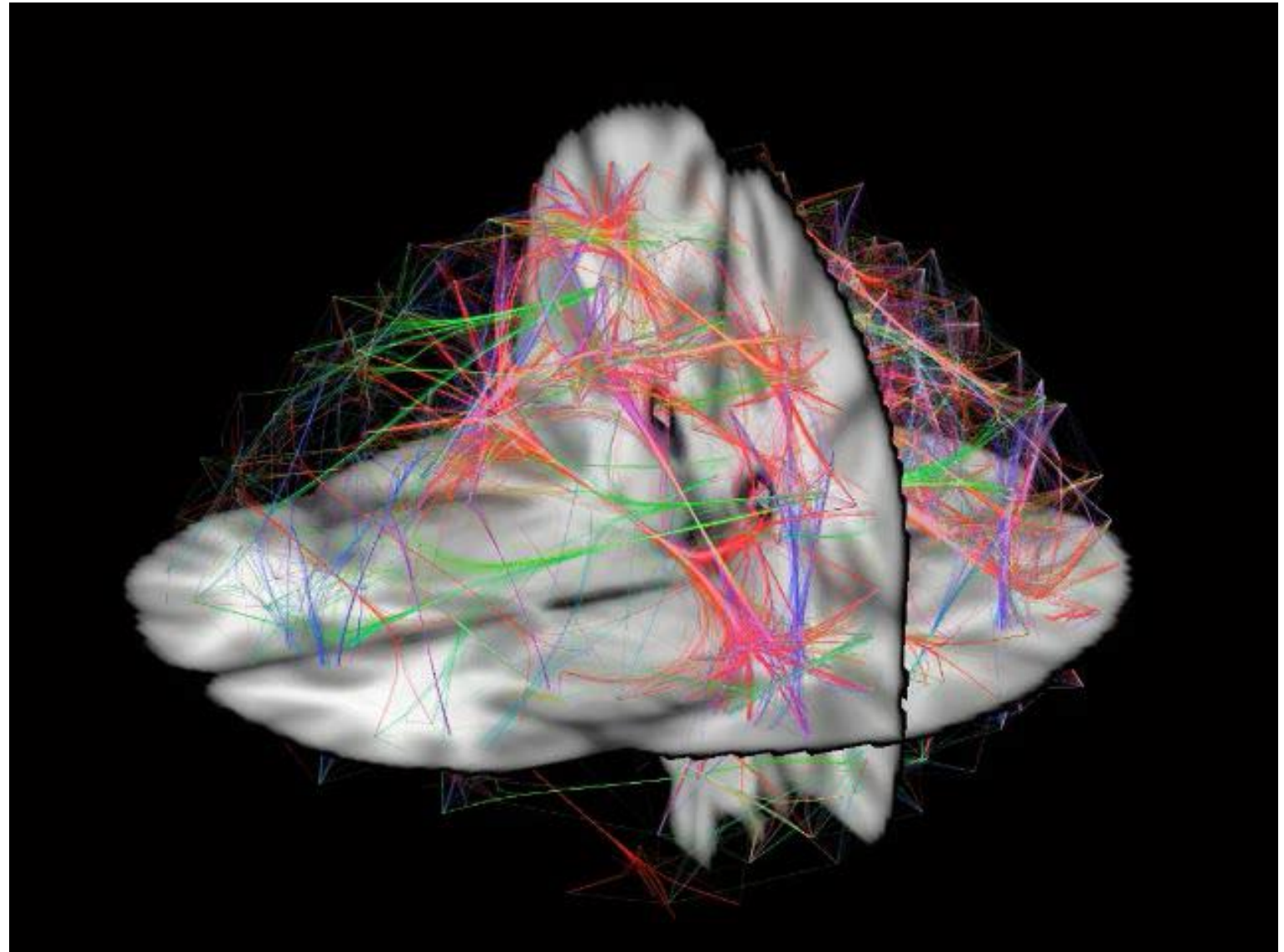
## Graph of connections: The functional **Connectome**

- Network of highly correlated areas
- Link between neural basis of low frequency **spontaneous fluctuations** and **oscillations in power and synchrony of neuronal activity**



*Nir Nat Neurosci 08*

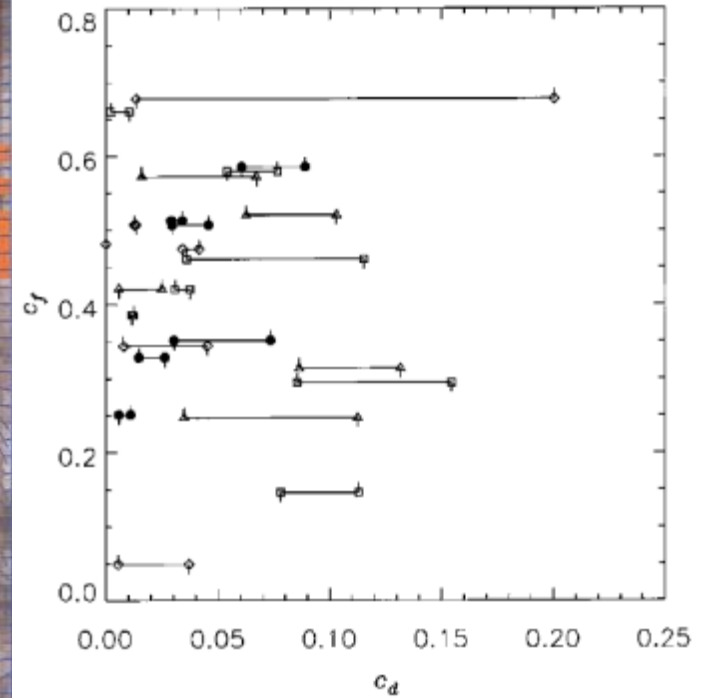
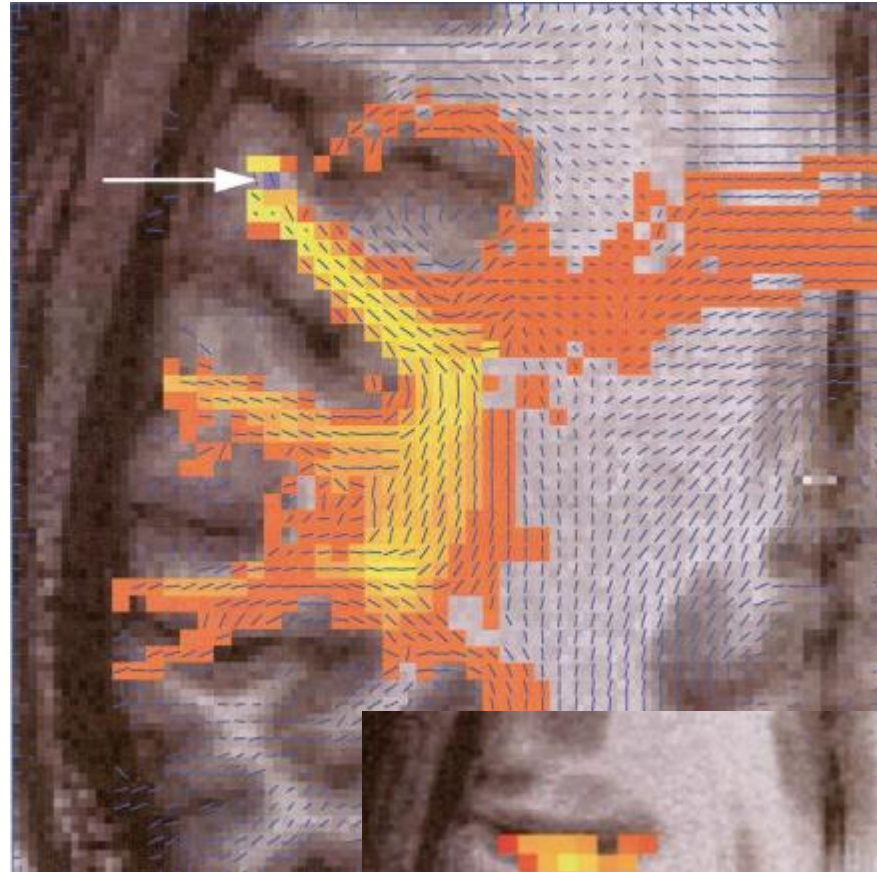
*Böttger et al. IEEE TVCG 2013*





# First link between tractography and functional connectivity

- Probabilistic tractography between adjacent gyri (cd)
- Correlation coefficient (cf) between connected areas

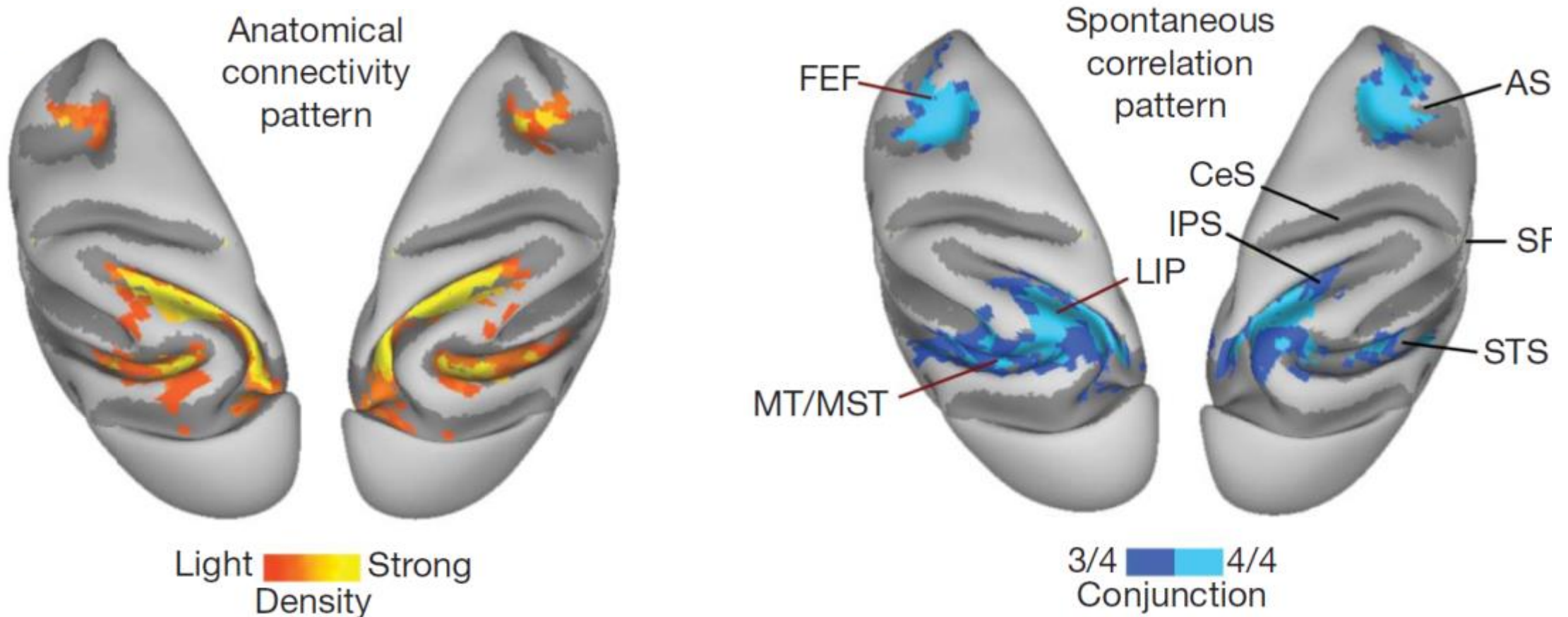


*Koch et al. Neuroimage 2002*



# Structure-function correspondence

- Macaque monkey: overlap between neuroanatomical connections (tracer injections) and correlations in fMRI signal



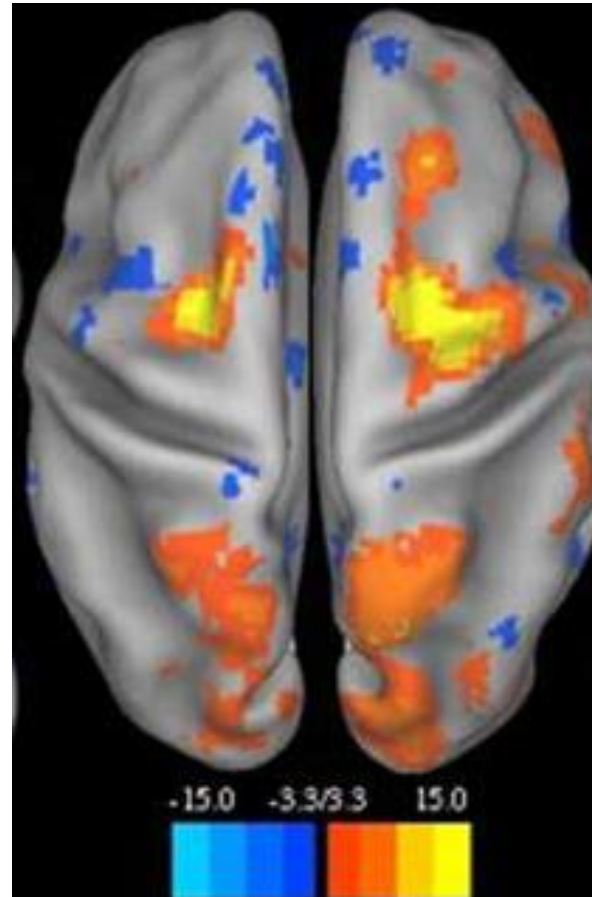
*Vincent et al. Nature 2007*



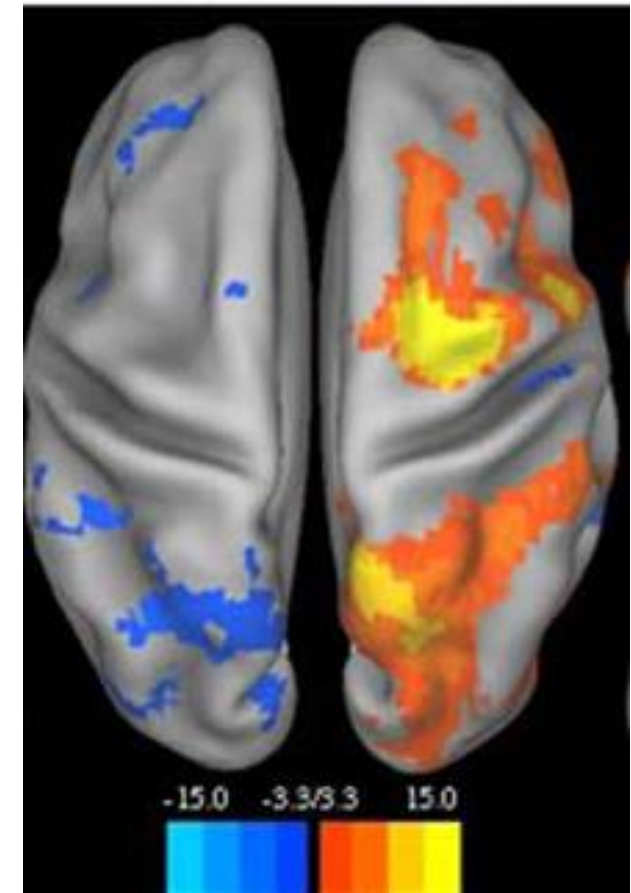


# Role of the corpus callosum for functional connectivity across hemispheres

- Functional connectivity before and after callosotomy
- Complete sectioning of the corpus callosum of a 6y old child
- Z-score of the correlation map
- Seed in the right frontal eye field
- Lost positive functional connectivity in both hemispheres



before



after

*Johnston et al. J Neurosci 2008*

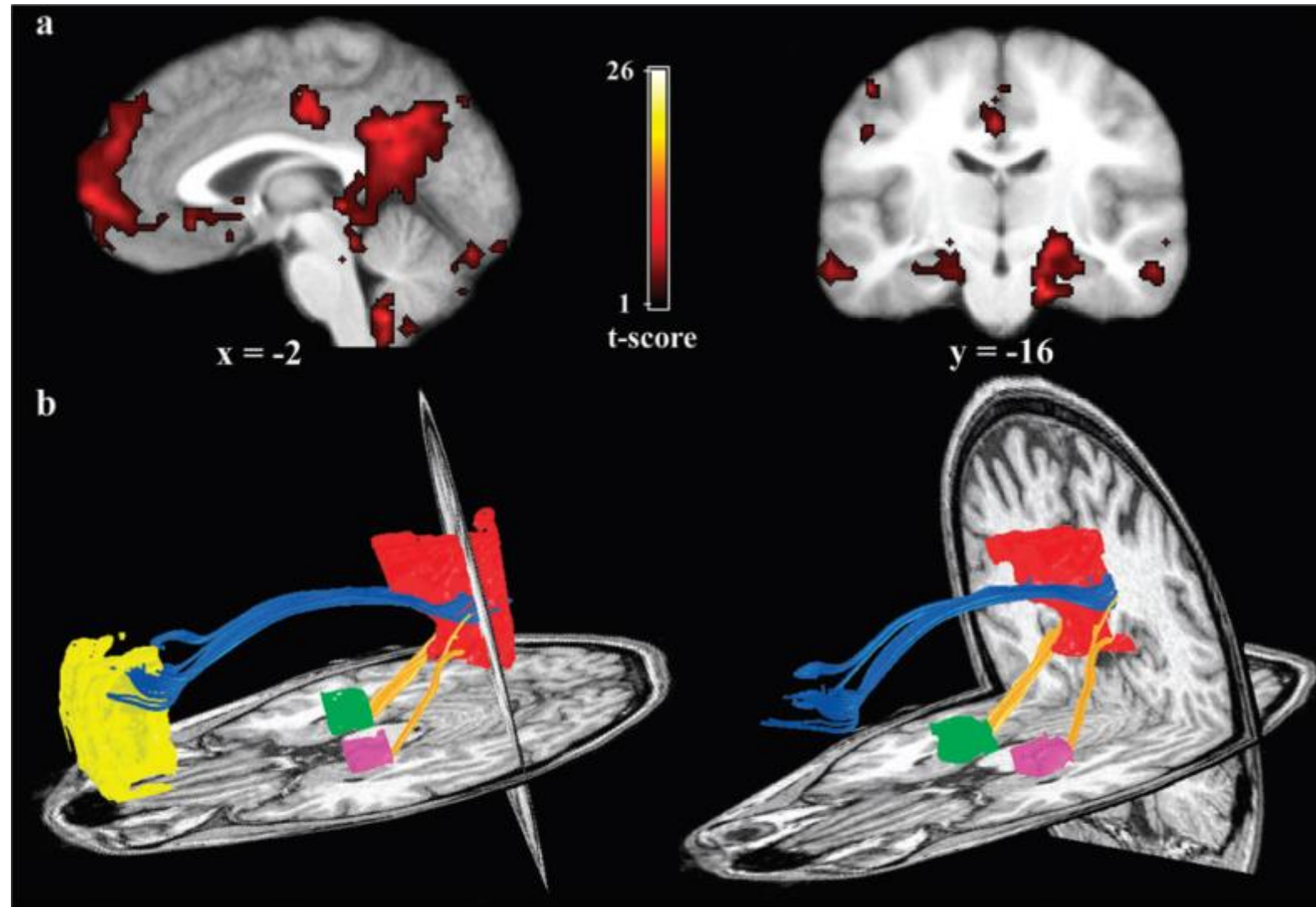


# Correspondence with tractography



# Tractography of the cingulum in the default mode network

- Resting-state functional connectivity can be decomposed into networks
- Structural connectivity in the default mode network corresponds to the cingulum bundle

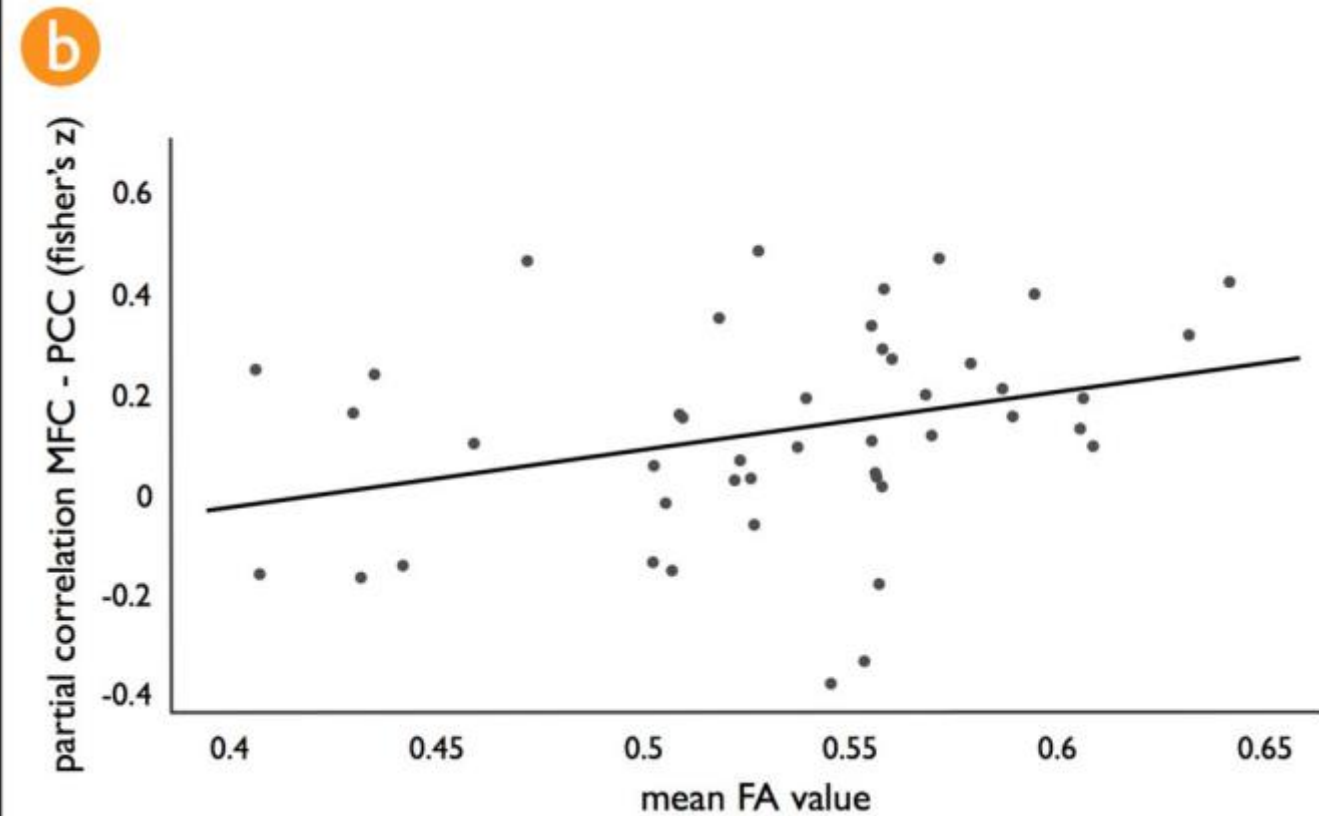
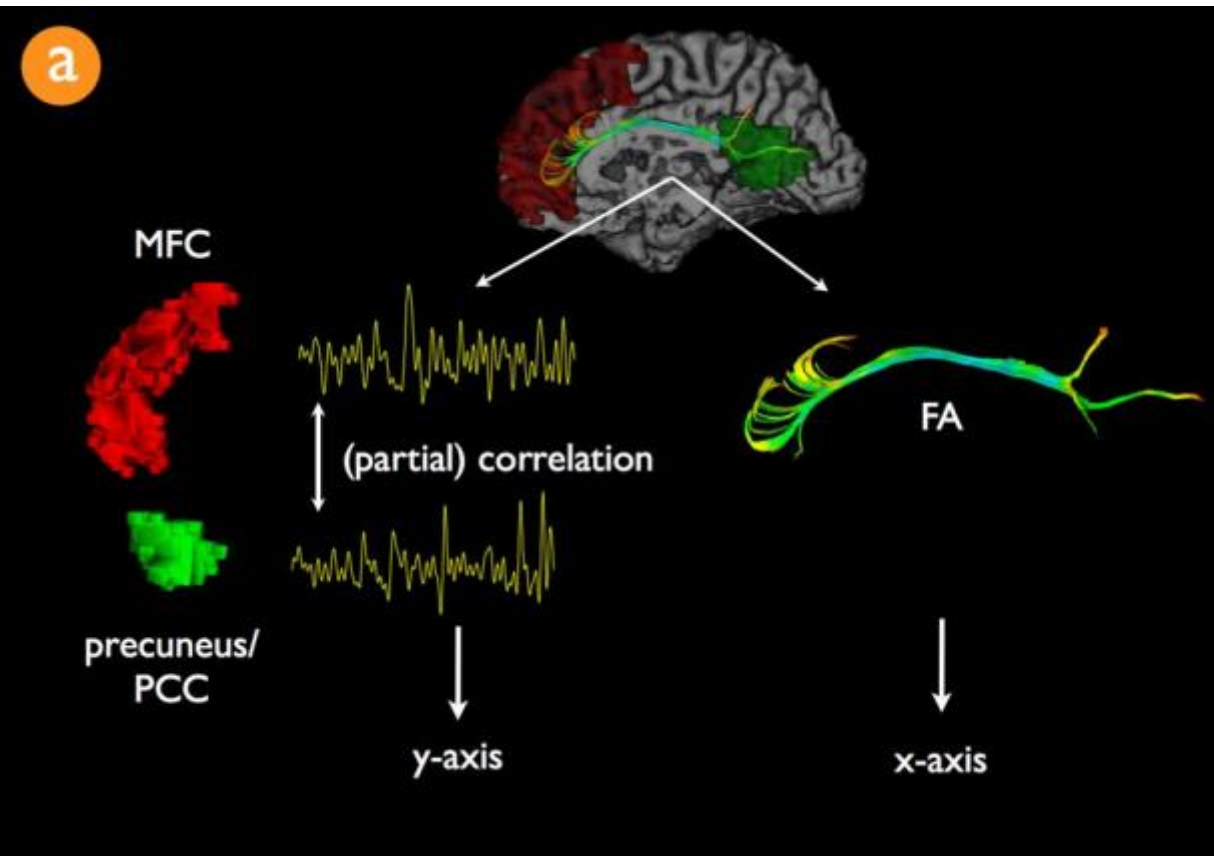


*Greicius et al. Cereb Cortex 2009*





# Microstructural organization of the cingulum tract



- Association between the level of default mode functional connectivity and the microstructural organization of the cingulum tract.

*van den Heuvel et al J Neurosci 2008*

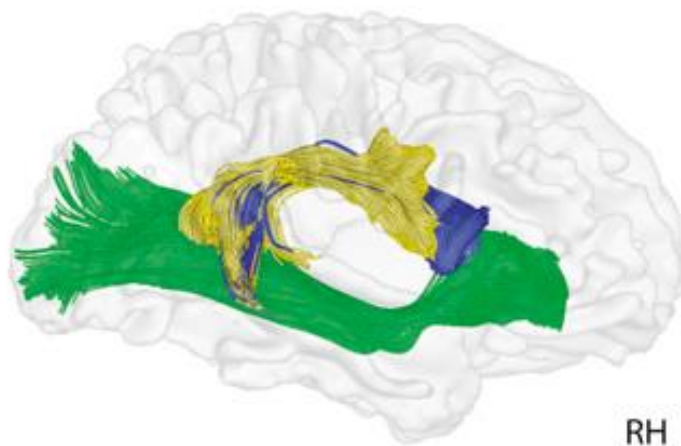
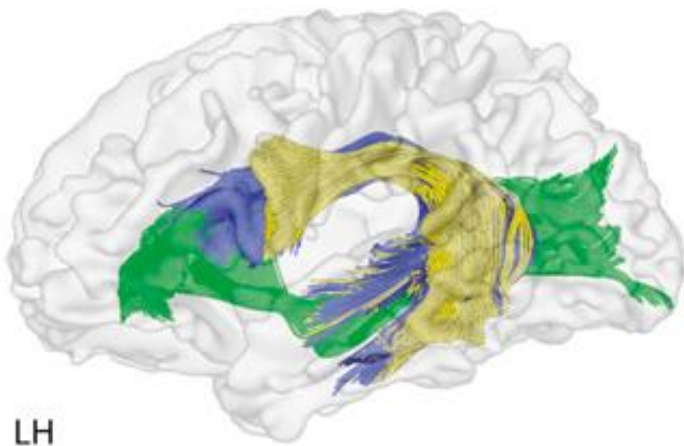


# Development of functional and structural networks



# Development: from inter-hemispheric to intra-hemispheric connectivity

Adults

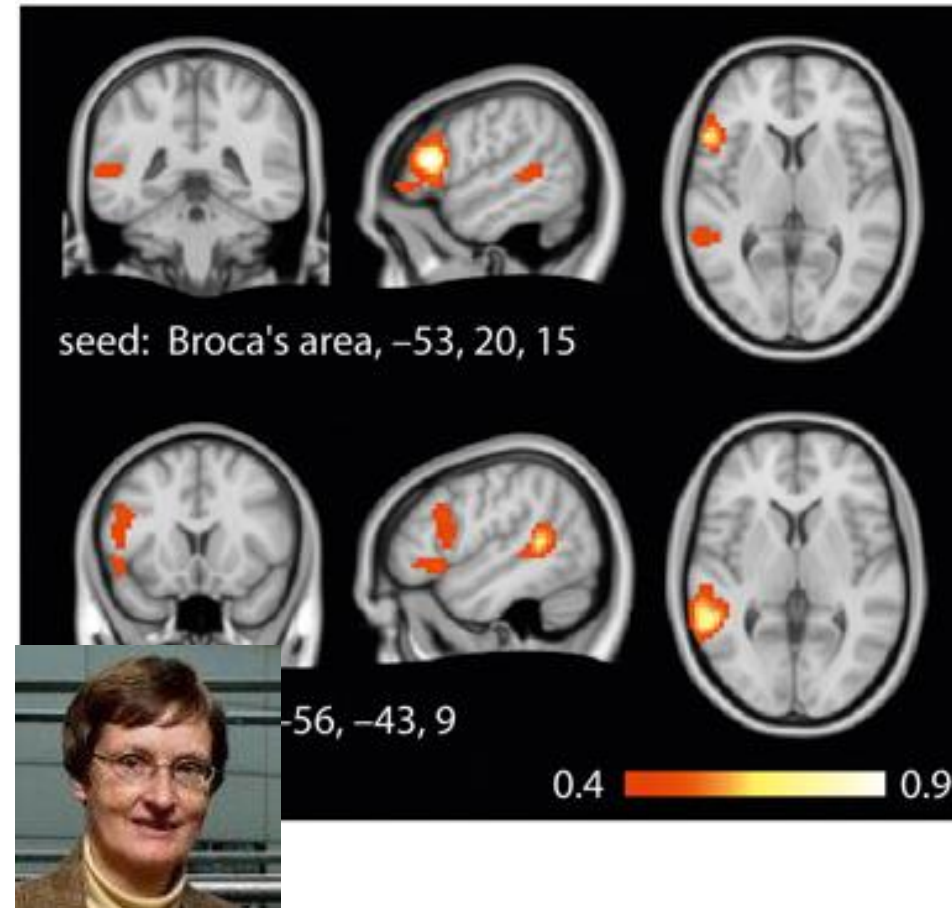


LH

RH

- Strong intra- and interhemispheric connections in the adult language network
- Diffusion MRI tractography and seed based resting state correlations

Adults



*Perani et al. PNAS 2011, G. Lohmann*

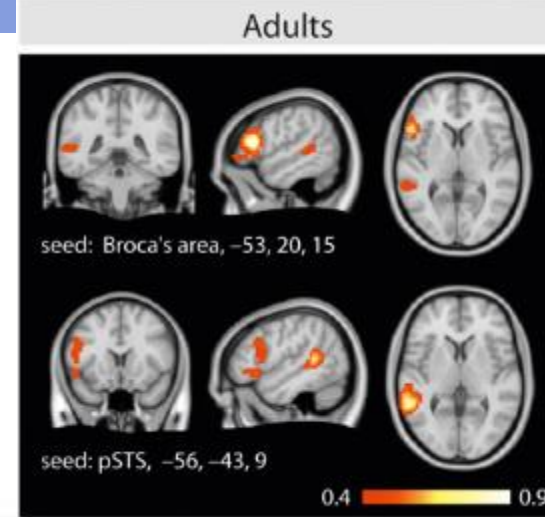
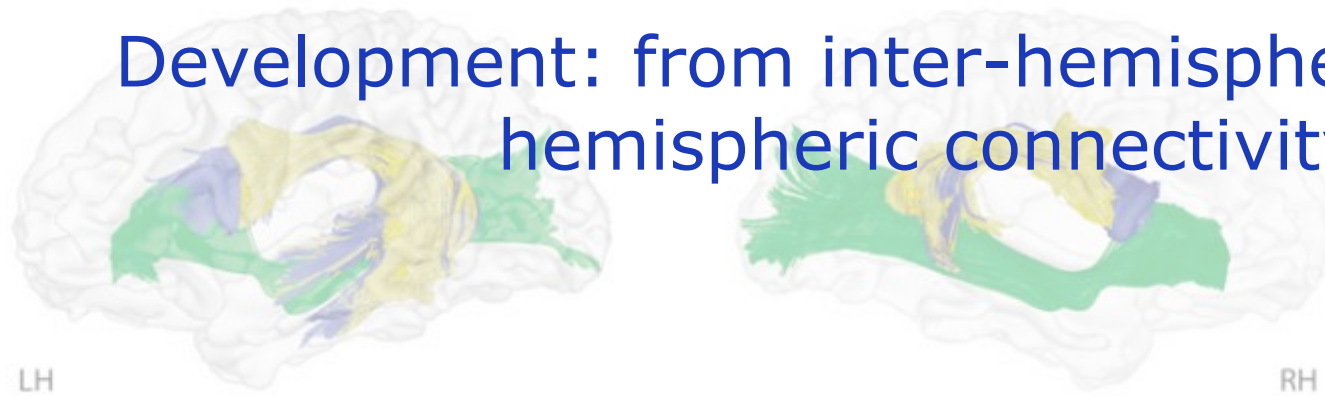




A

Adults

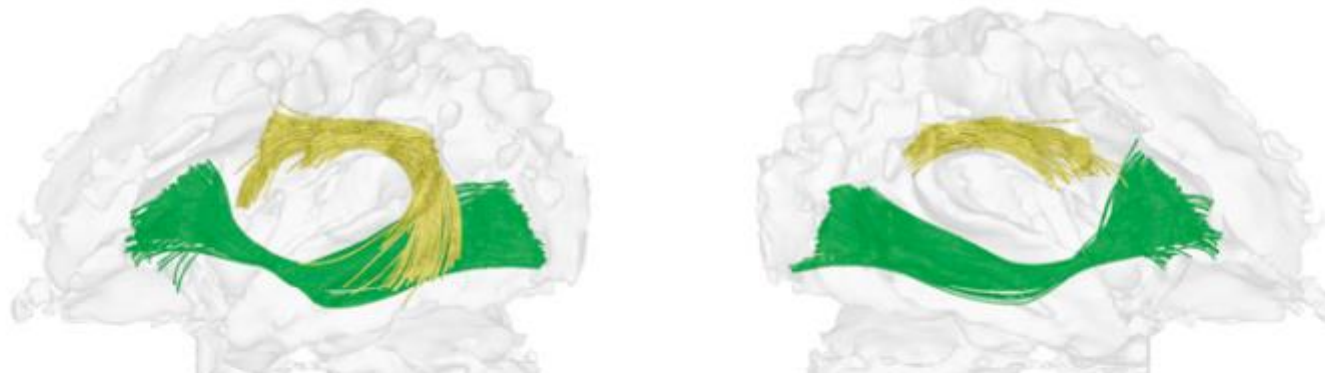
Development: from inter-hemispheric to intra-hemispheric connectivity



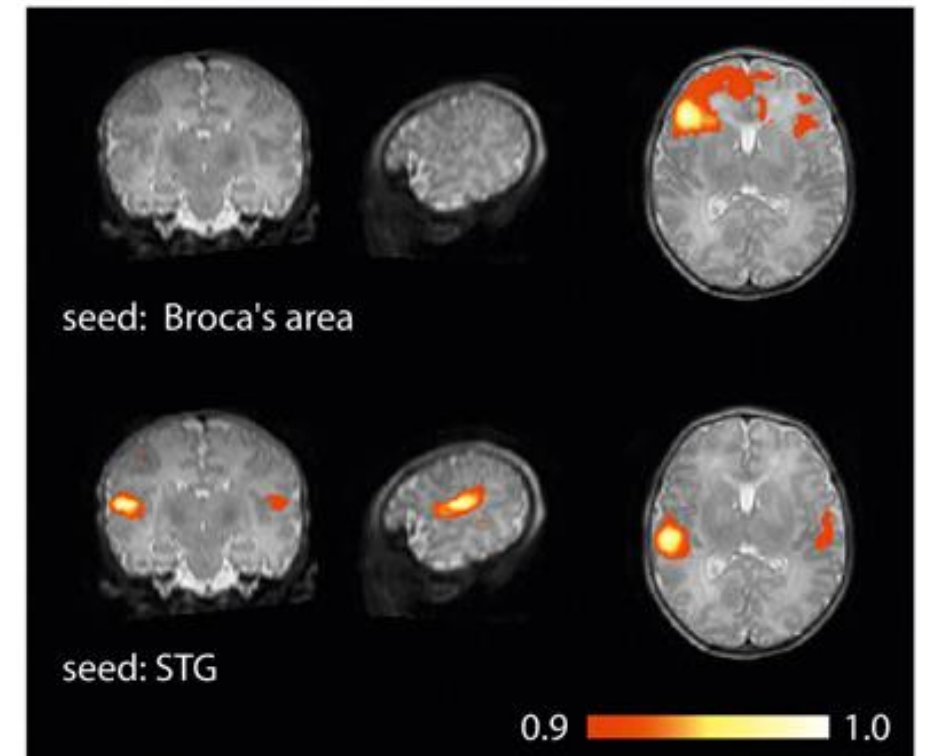
B

B

Newborns



Newborns



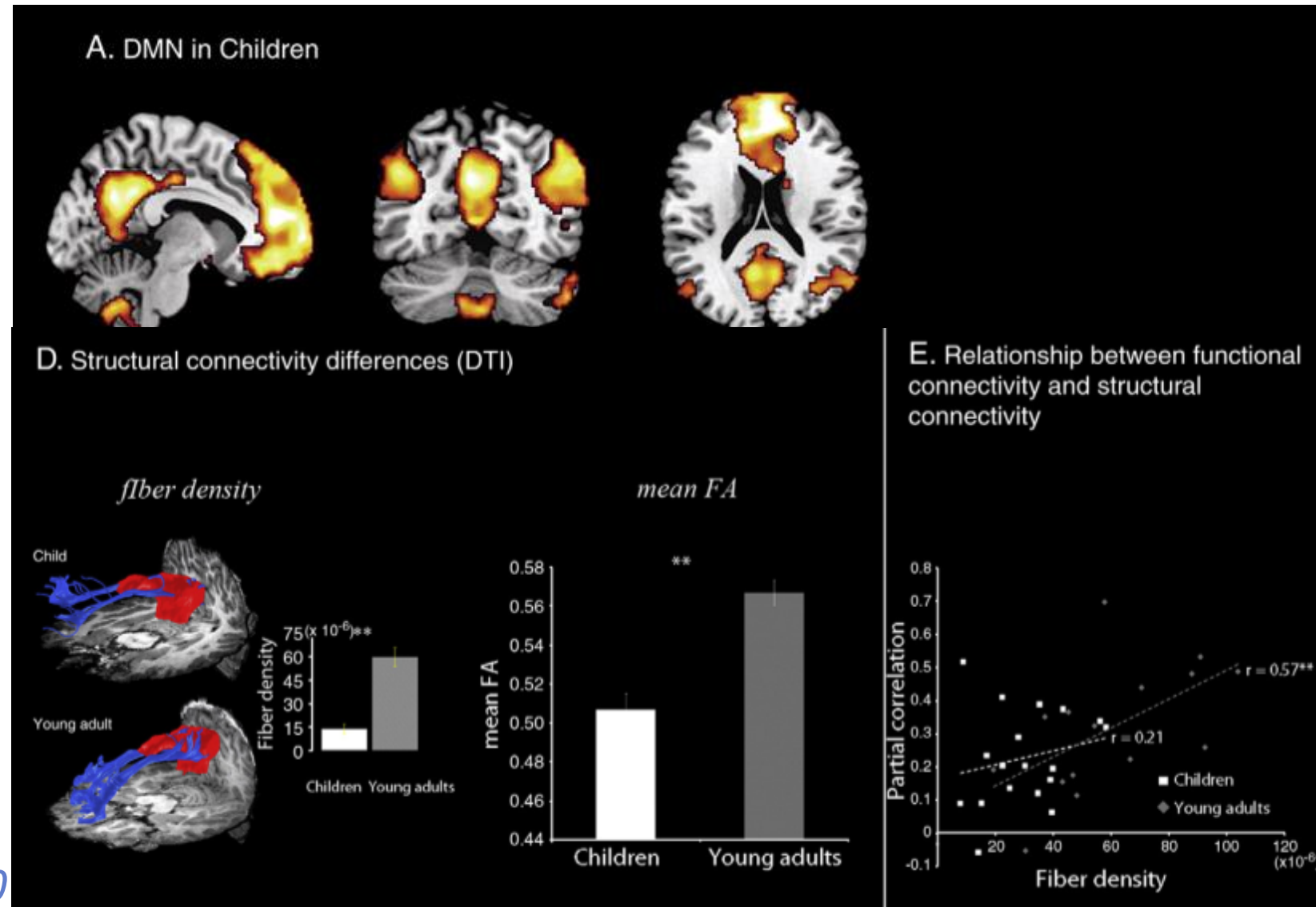
- In newborns we find only inter-hemispheric connections between the language regions
- The network of connections is molded from the external world during development

*Perani et al. PNAS 2011*



# Development of the default mode network (DMN)

- PCC-mPFC connectivity:
  - most immature link
  - microstructural differences
- Funct. connectivity to temporal lobe mature but not the structural connectivity

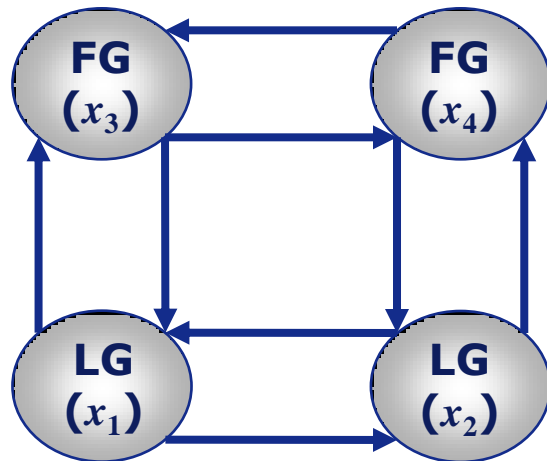


Supecar et al. Neuroimage 2010



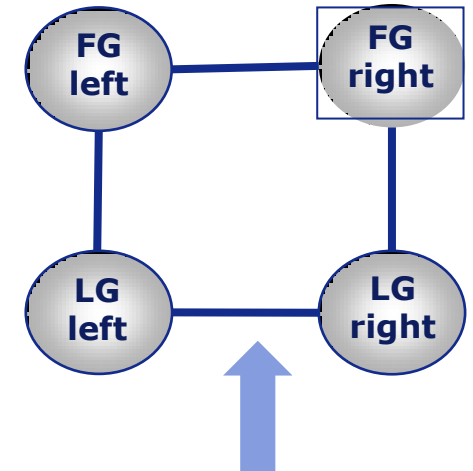
# Quantification of Connectivity – Use in DCM

## DCM Structure

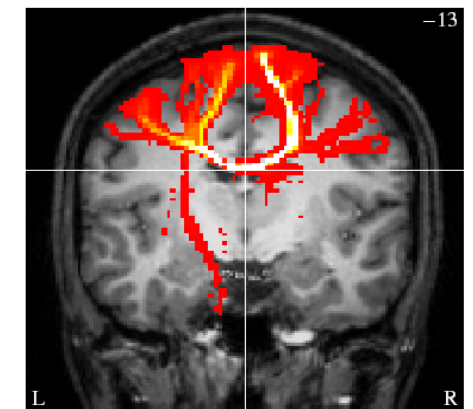


Effective connectivities are estimated using Bayesian inference.

## Anat. Connectivity



Anatomical connectivity is not equivalent to effective connectivity, but quantifies the **potential for information transfer**



Tractography

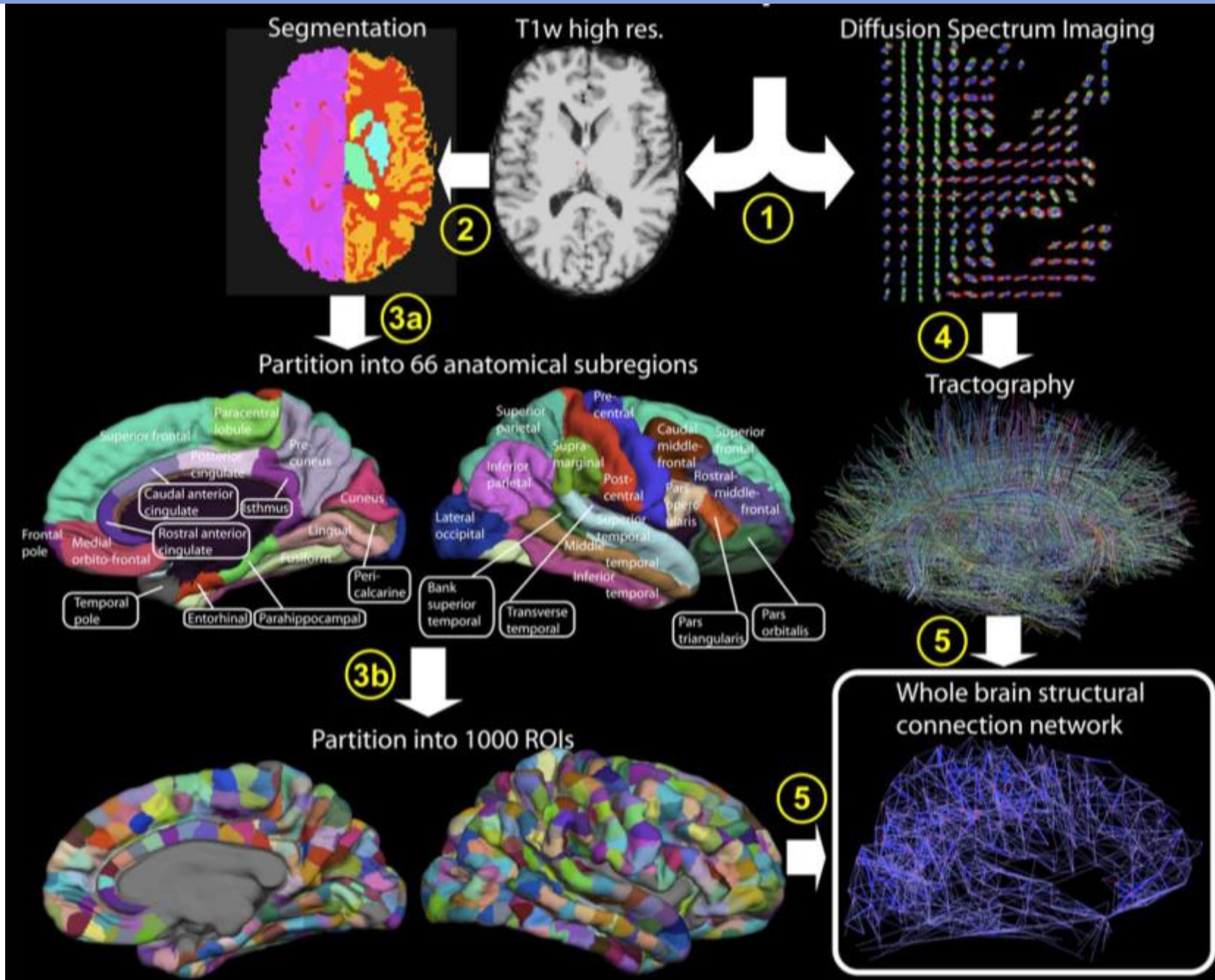


# From networks to connectomes



# Measuring the human connectome in vivo

- Segmentation
- Parcellation
- Subdivision
- Tractography
- Represent as graph:
  - as a connectome

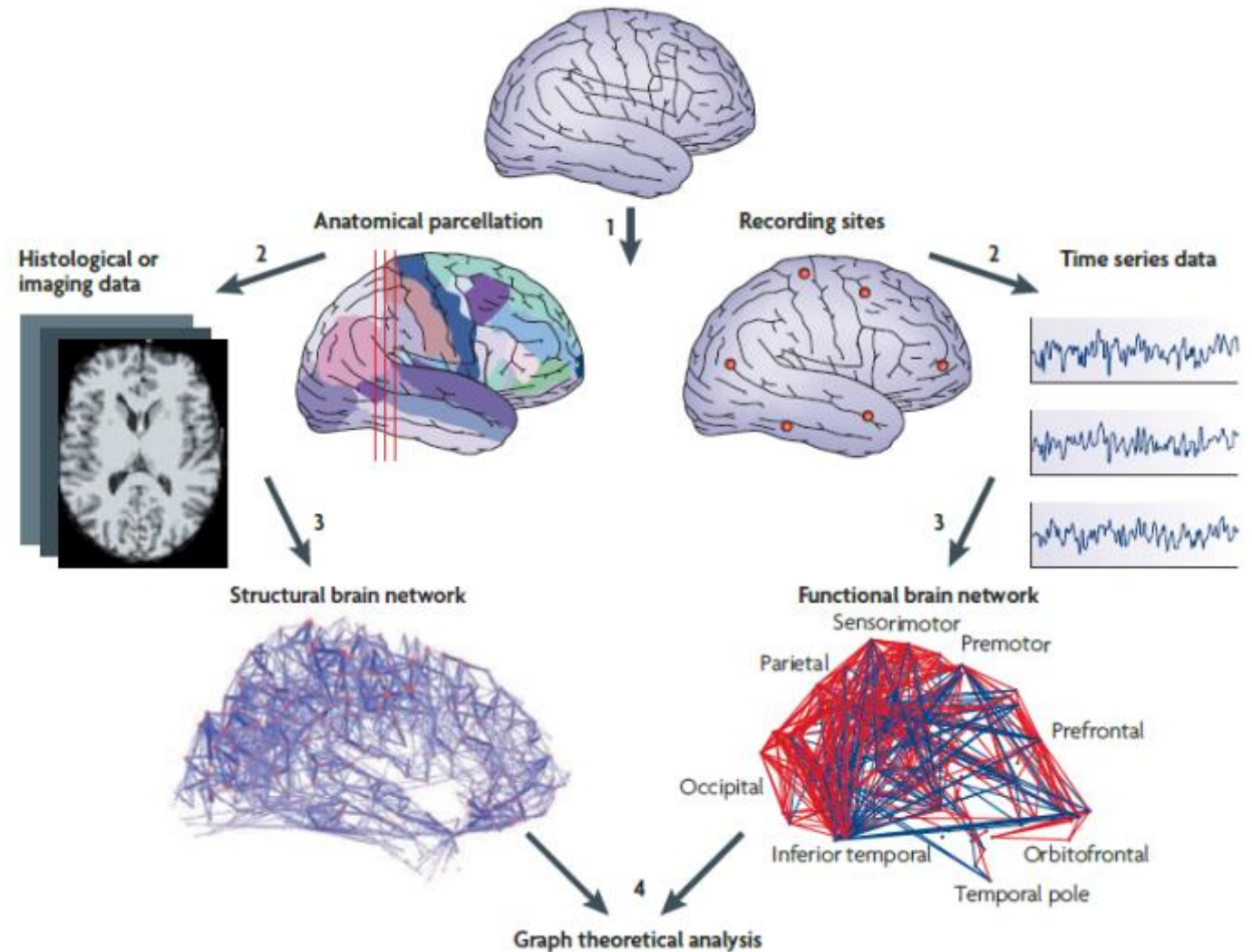


Hagmann et al. PLoS Biol 2008



# Analysis of structural and functional systems

- Whole-brain structural networks derived from diffusion MRI and functional Networks
- Compute functional and structural connectivity from the same parcellation
- Comparison in the same individuals
- Individual voxels or parcellated regions



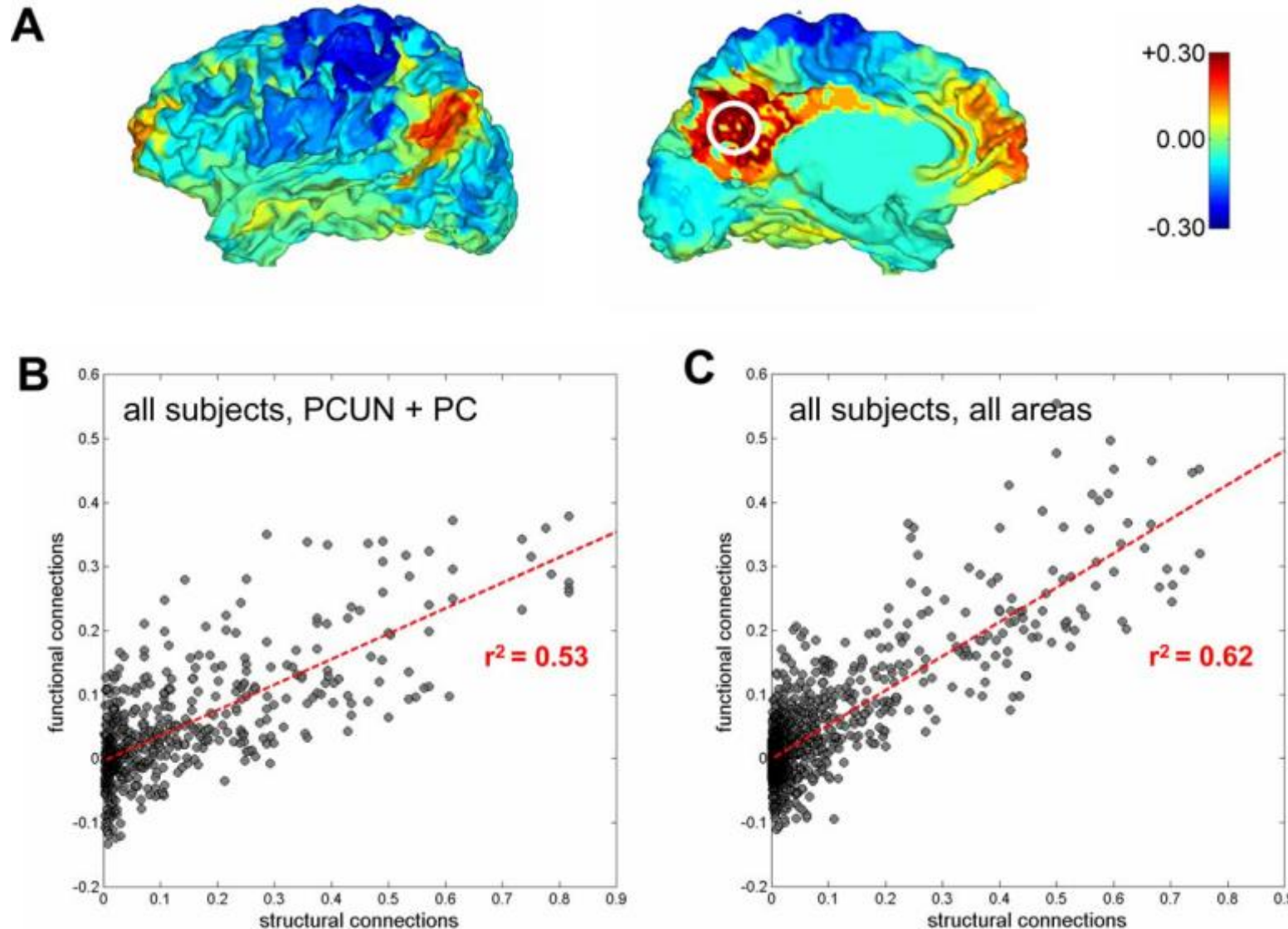
*Bullmore and Sporns, Nat Rev Neurosci. 2009*





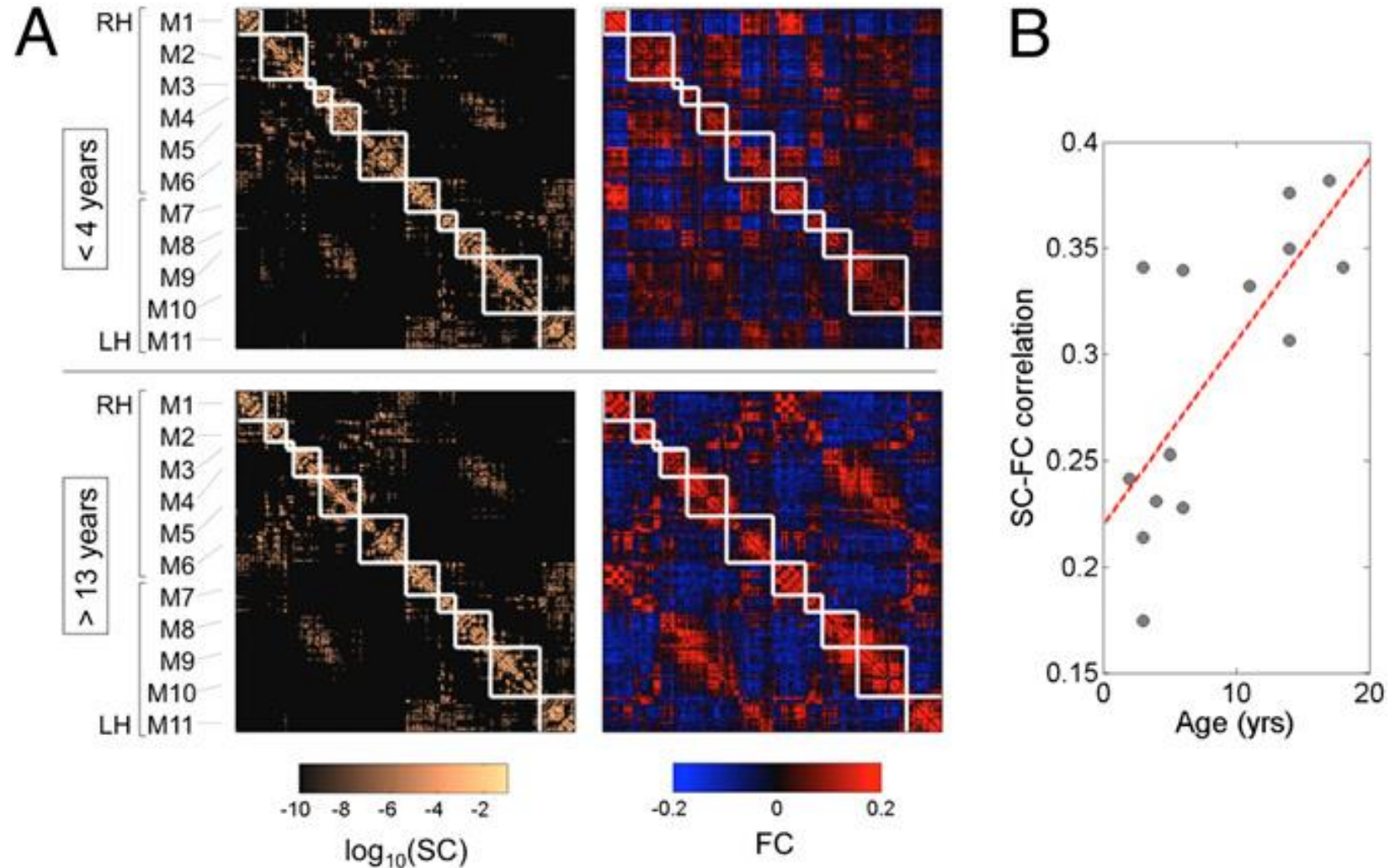
# Comparison of structural and functional connectivity

- functional correlations from resting state fMRI
- structural and functional connections of the precuneus and posterior cingulate cortex
- all anatomical subregions in both hemispheres.



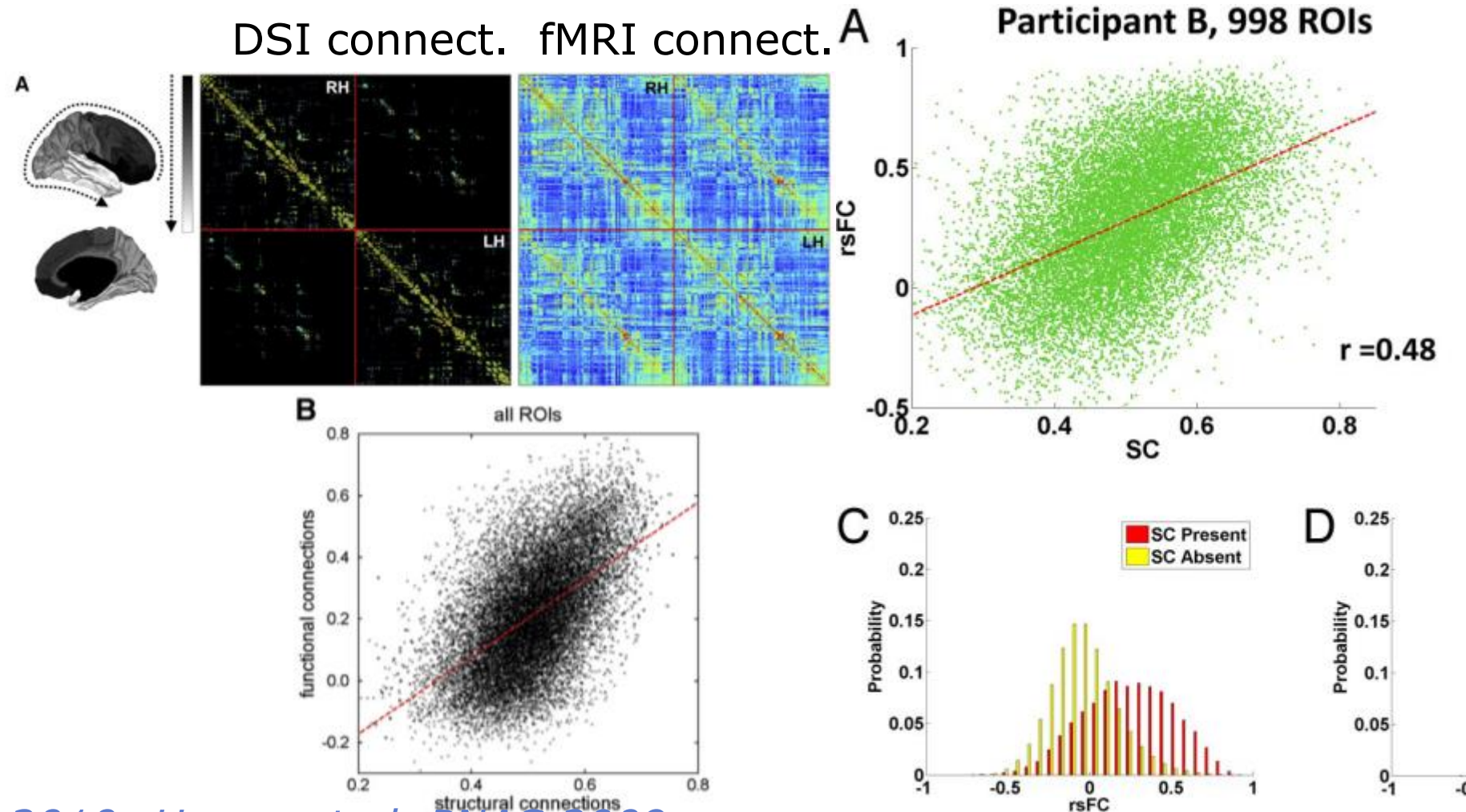
# Structural connectivity – functional connectivity correlations in development

- Strengthening of structural pathway in line with changes in functional interactions.
- Positive correlation between structural and functional connectivity
- Relationship strengthened with age
- White matter connectivity play an important role in creating brain-wide coherence and synchrony



# Structural and functional connectivity matrices

- Significant relationship between structural and functional connectivity
- Right: structurally unconnected (SC absent) regions show low and negative functional connectivity (FC)



*Honey et al. Neuroimage 2010; Honey et al. PNAS 2009*

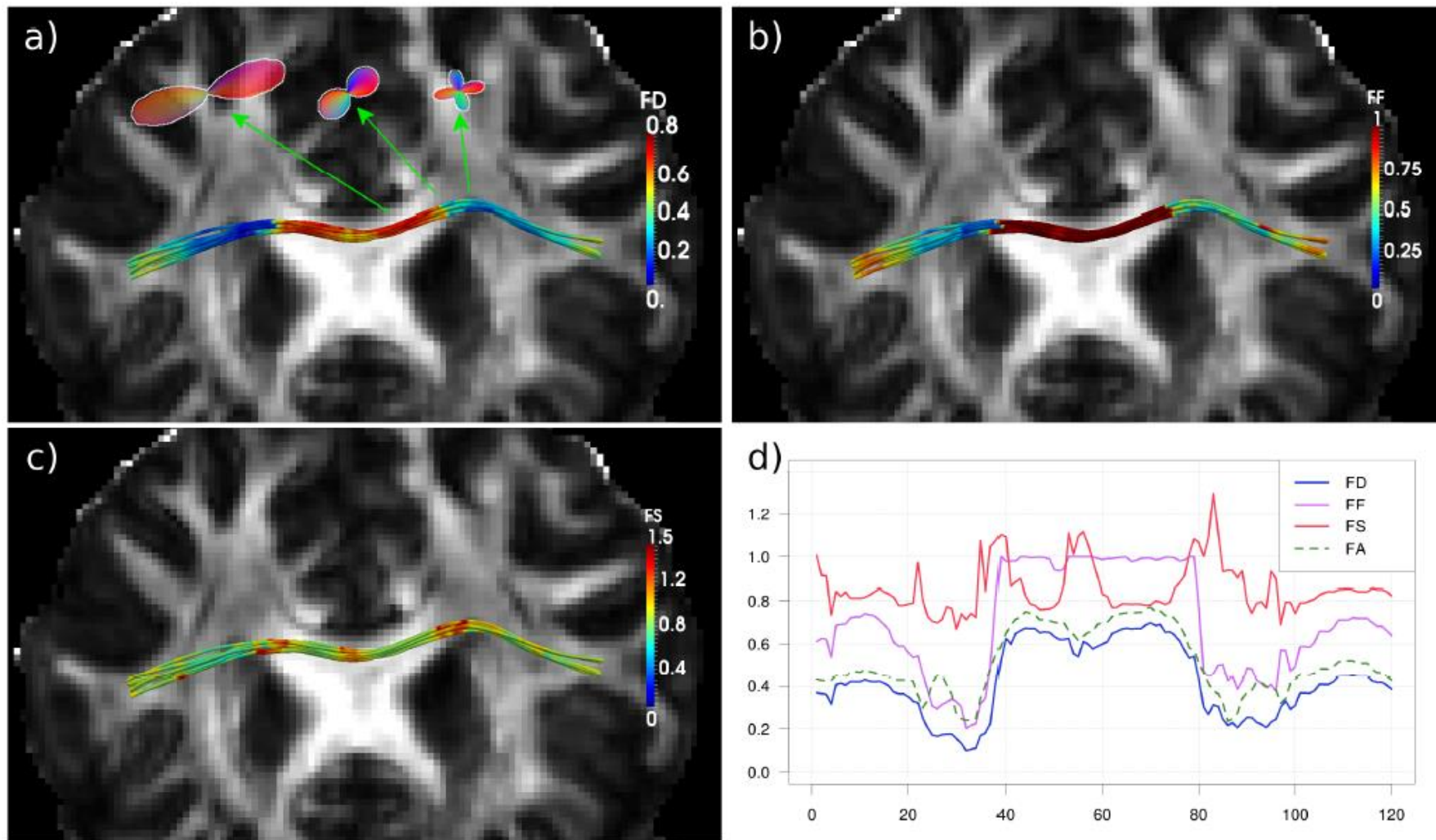




# Enrich the structural connectome by quantitative MRI

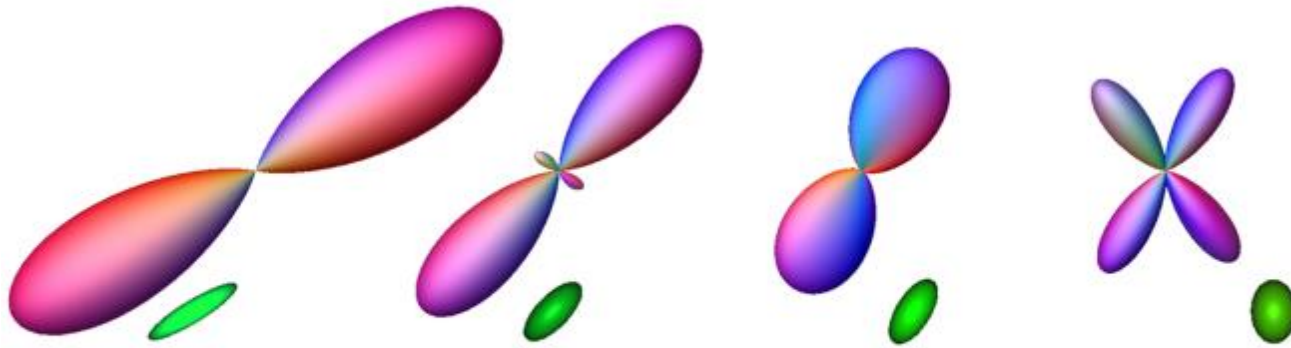


# Mapping of crossing fiber parameters

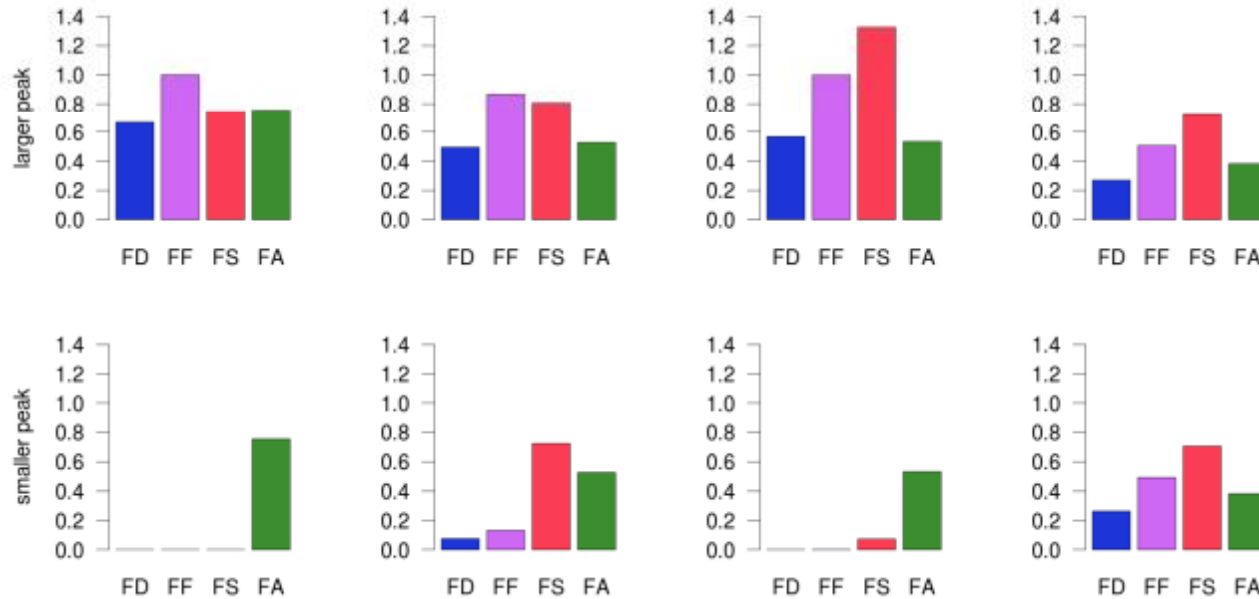


FD: fiber density, FF: fiber fraction, FS: fiber spread

# Additional microstructural parameters



- FD: fiber density
- FF: fiber fraction
- FS: fiber spread
- FA: fractional anisotropy

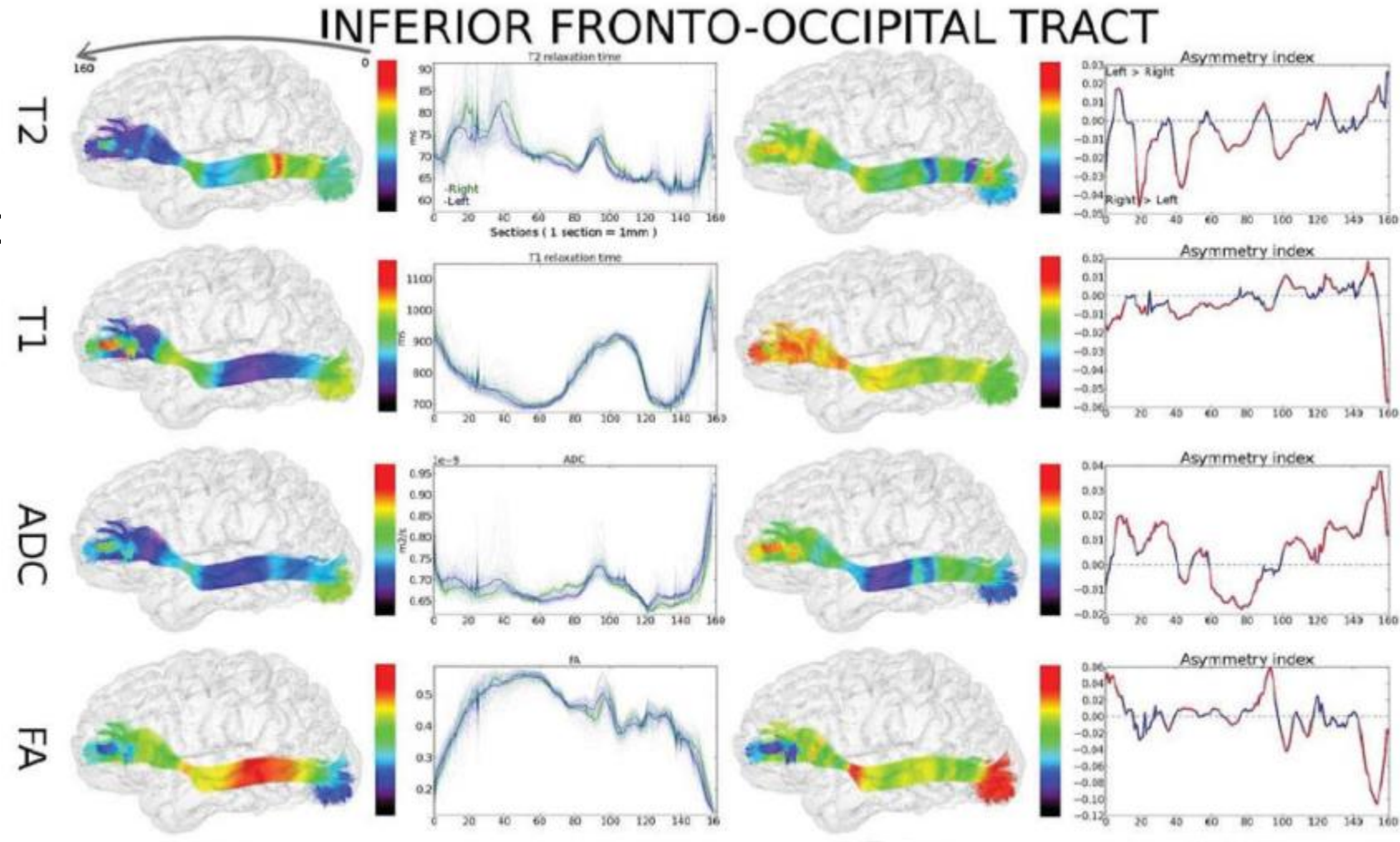
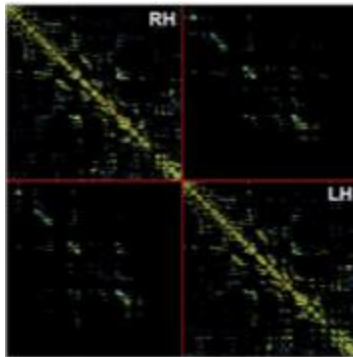


*Schreiber et al. Neuroimage 2014; Riffert et al. Neuroimage 2014*



# Edge weights for the enriched structural connectome?

- Log-number of streamlines
- Log-connection density
- FA or  $1/\text{ADC}$
- Normalize?
- Quantitative T1 and T2 relaxation time

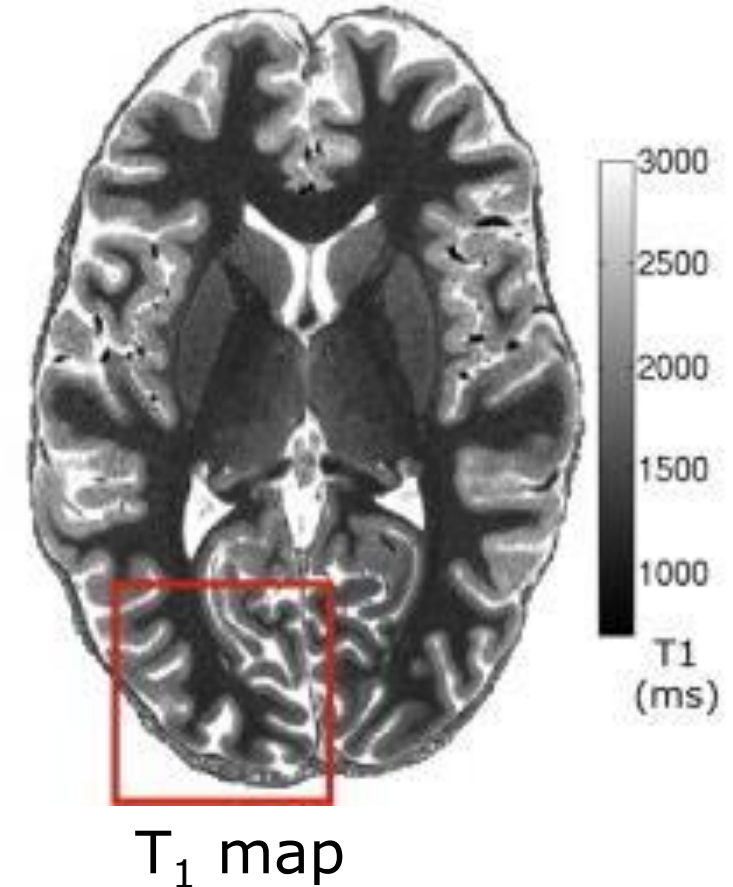
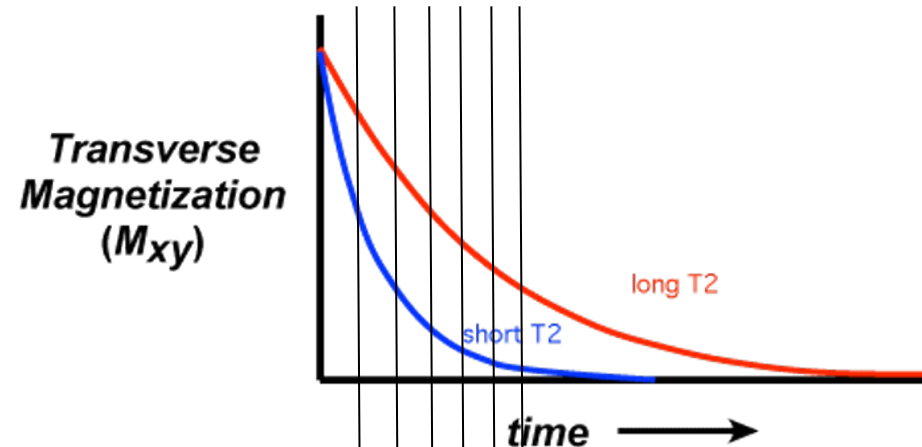
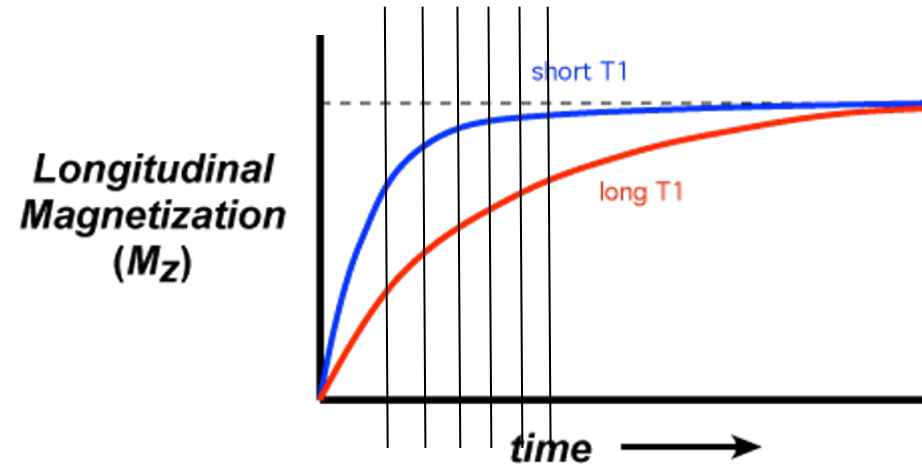
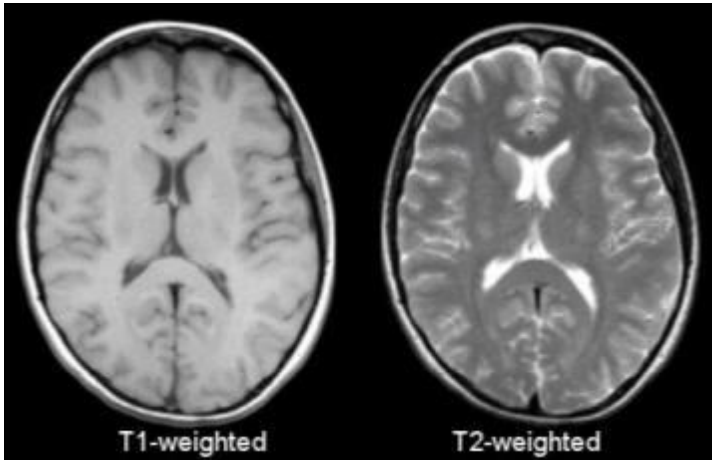


LeBois, PhD Thesis, 2014





# From $T_1$ and $T_2$ weighted images to $T_1$ and $T_2$ maps



<http://mriquestions.com>, Tardif et al. 2015



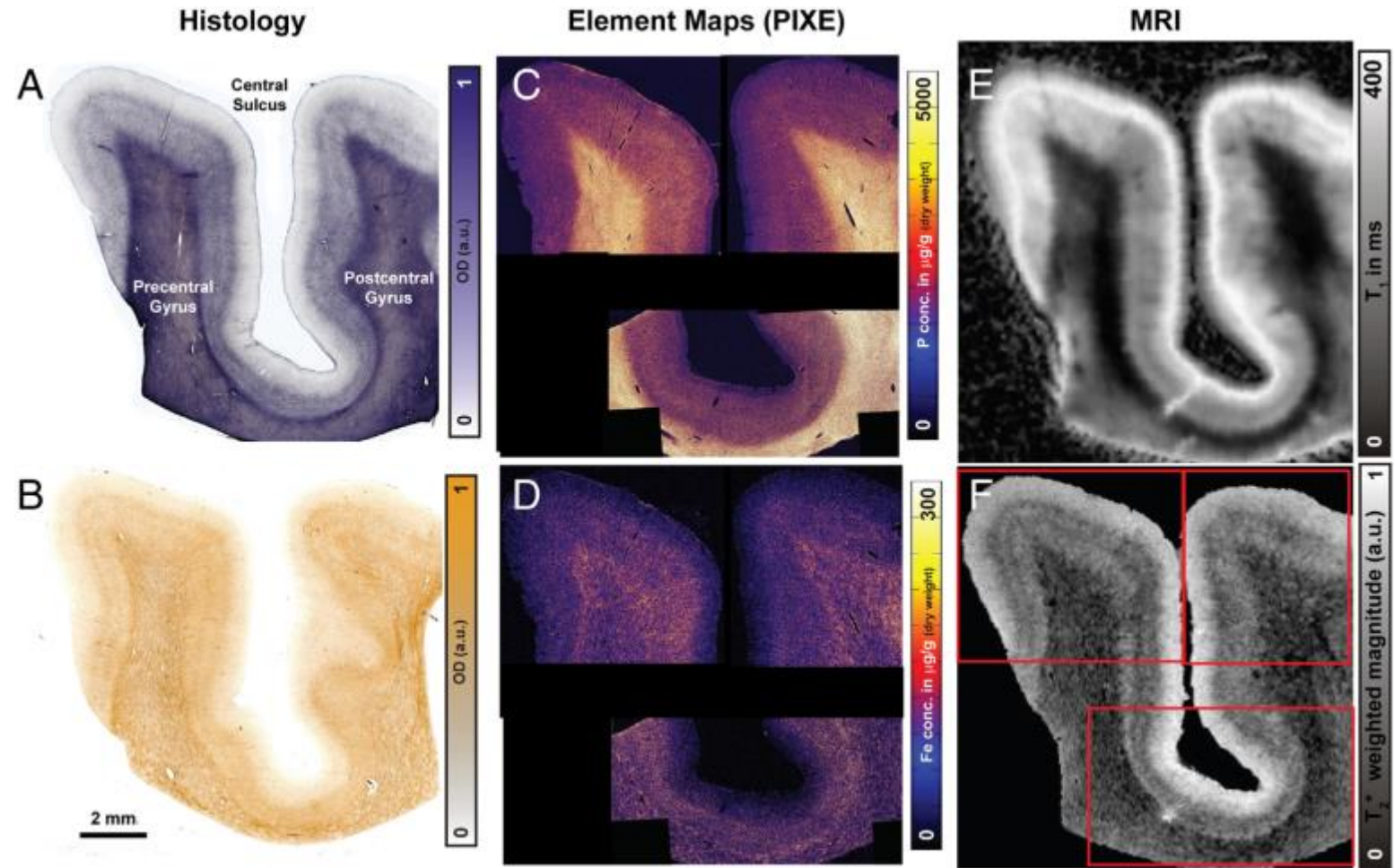
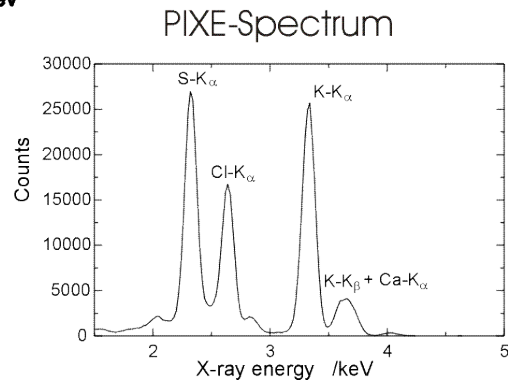
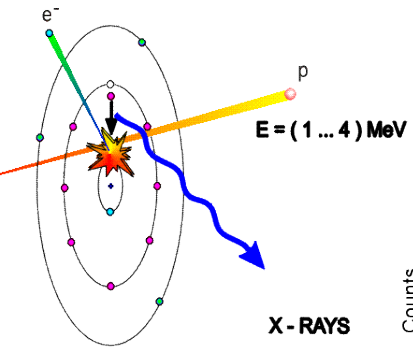
@AlfredAnwander

anwander@cbs.mpg.de CoBCoM 2017, Juan-les-Pins

Max Planck Institute for Human Cognitive and Brain Sciences

# From $T_1$ and $T_2$ maps to myelin

- Quantify myelin
- Proton induced X-ray emission



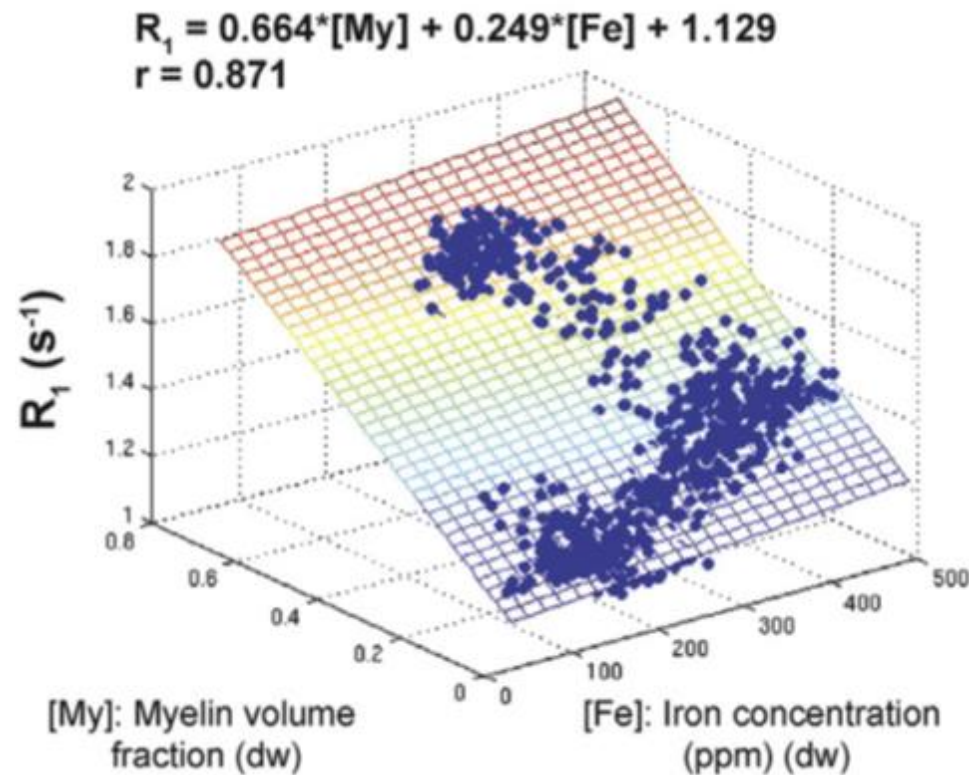
C. Stüber et al. *Neuroimage* 2014, <https://bloch.physgeo.uni-leipzig.de>



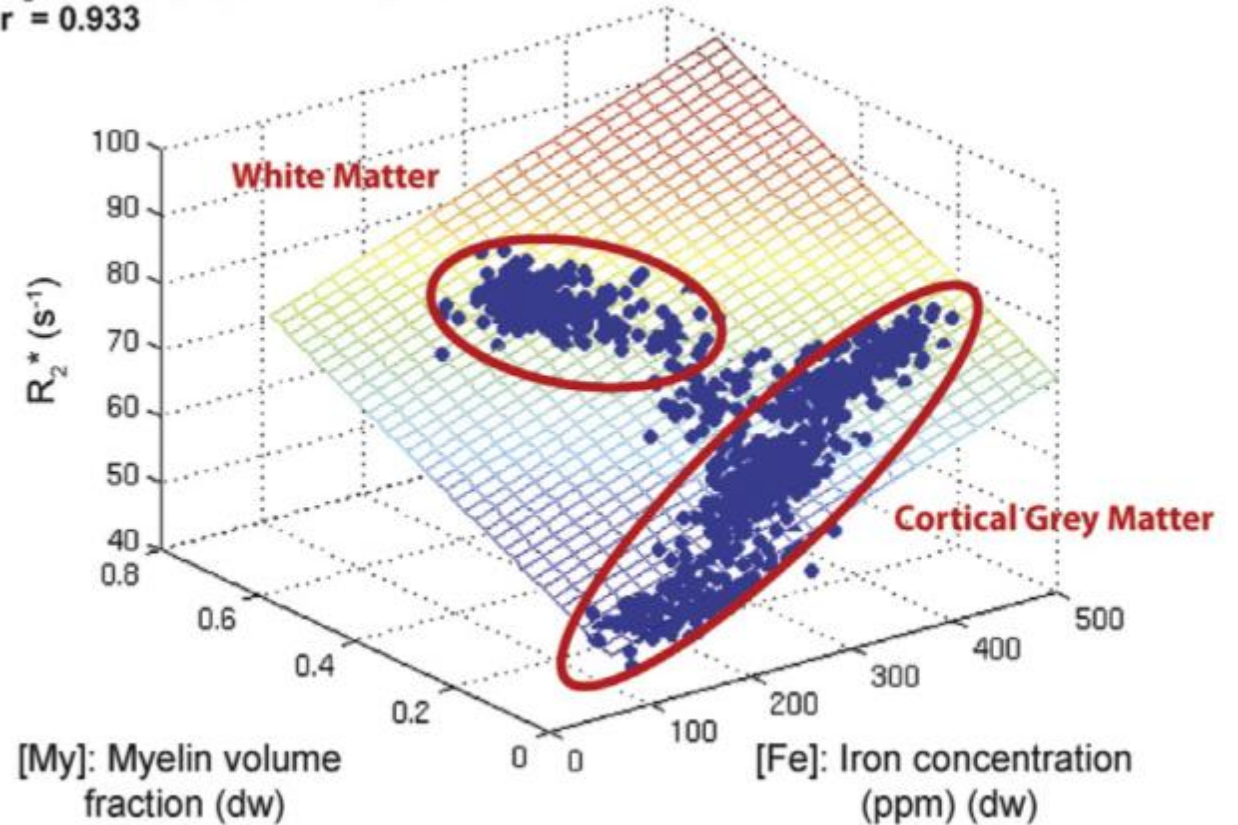


## From $T_1$ and $T_2$ maps to myelin ( $R_1=1/T_1$ )

- $R_1 = a_{Fe}C_{Fe} + a_{My}C_{My} + a_{Off}$
- $R_2^* = b_{Fe}C_{Fe} + b_{My}C_{My} + b_{Off}$



$R_2^* = 38.59 [My] + 0.0526 [Fe] + 45.87$   
 $r = 0.933$



**Multivariate Linear Regression**

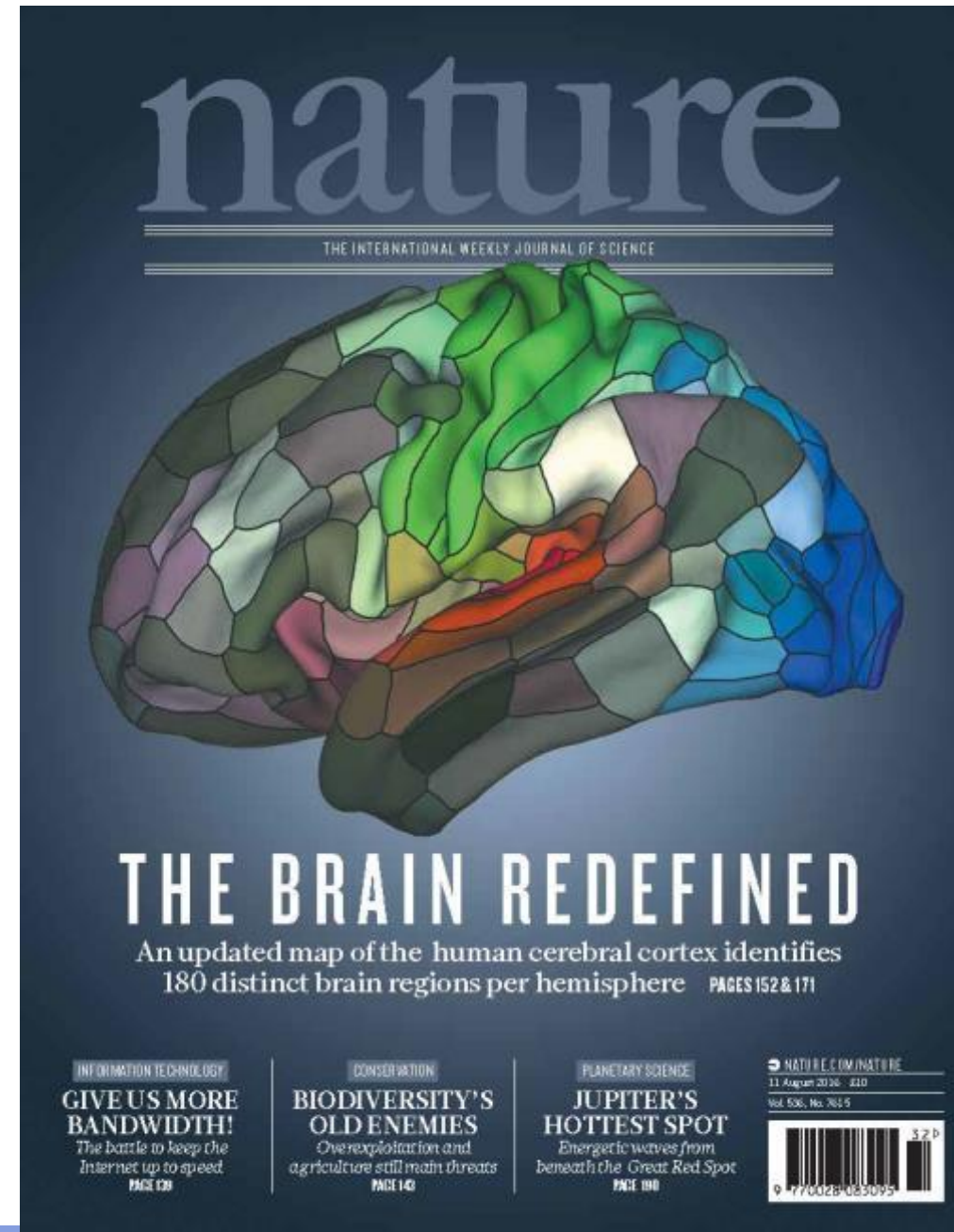
# Individual parcellation for structural and functional data?





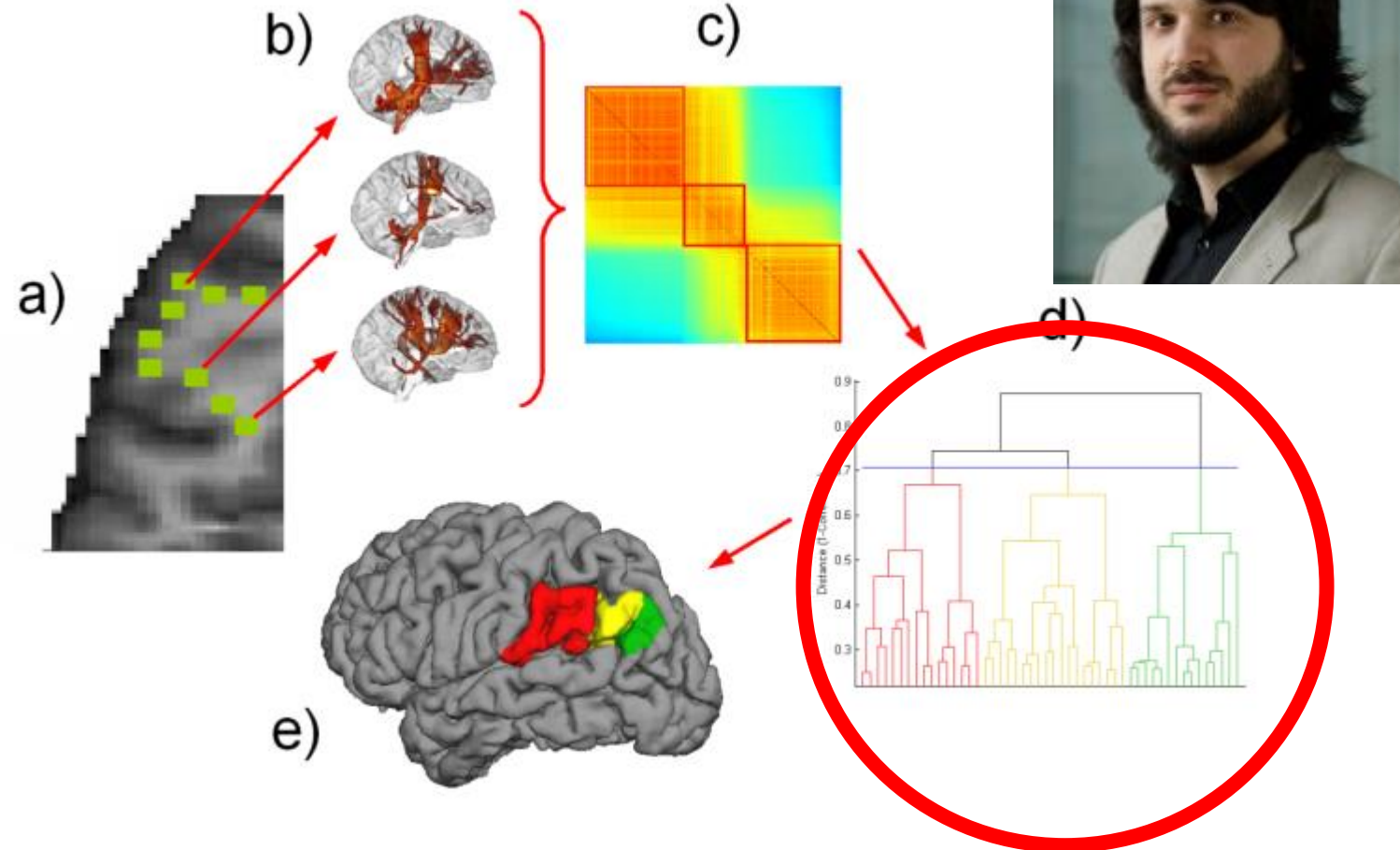
Is it solved?

*Glasser et al. Nature 2016*



# Tractography based hierarchical parcellation of the human brain

- Structural connectivity differs between cortical areas
- The difference in such characteristic tractograms can be evaluated statistically
- Similarity matrix of probabilistic tractography
- Connectivity matrix shows hierarchical structure
- Representation as hierarchical tree



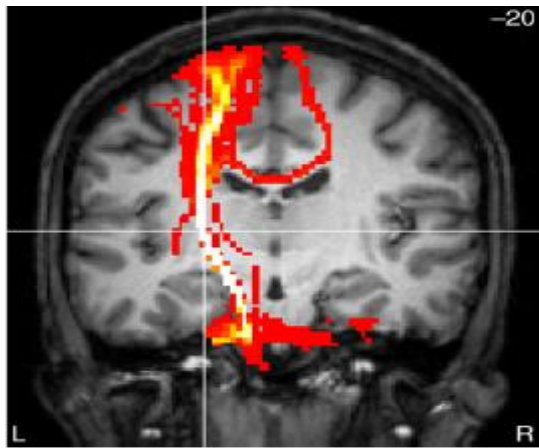
Anwander et al. *Cereb Cortex* 2007, Moreno-Dominguez et al. *Hum Brain Mapp* 2015



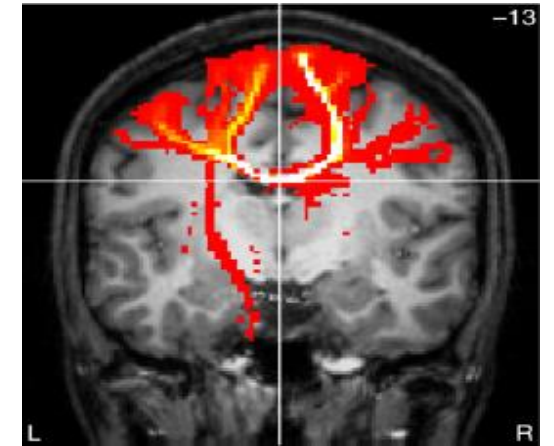
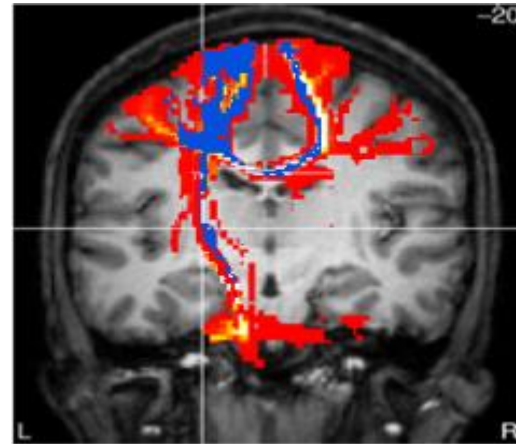
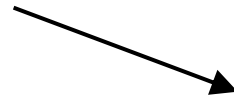
# Tractogram dissimilarity

Similarity  $\rightarrow$  normalized scalar product.  $[0,1]$

Distance =  $1 - \text{Similarity}$



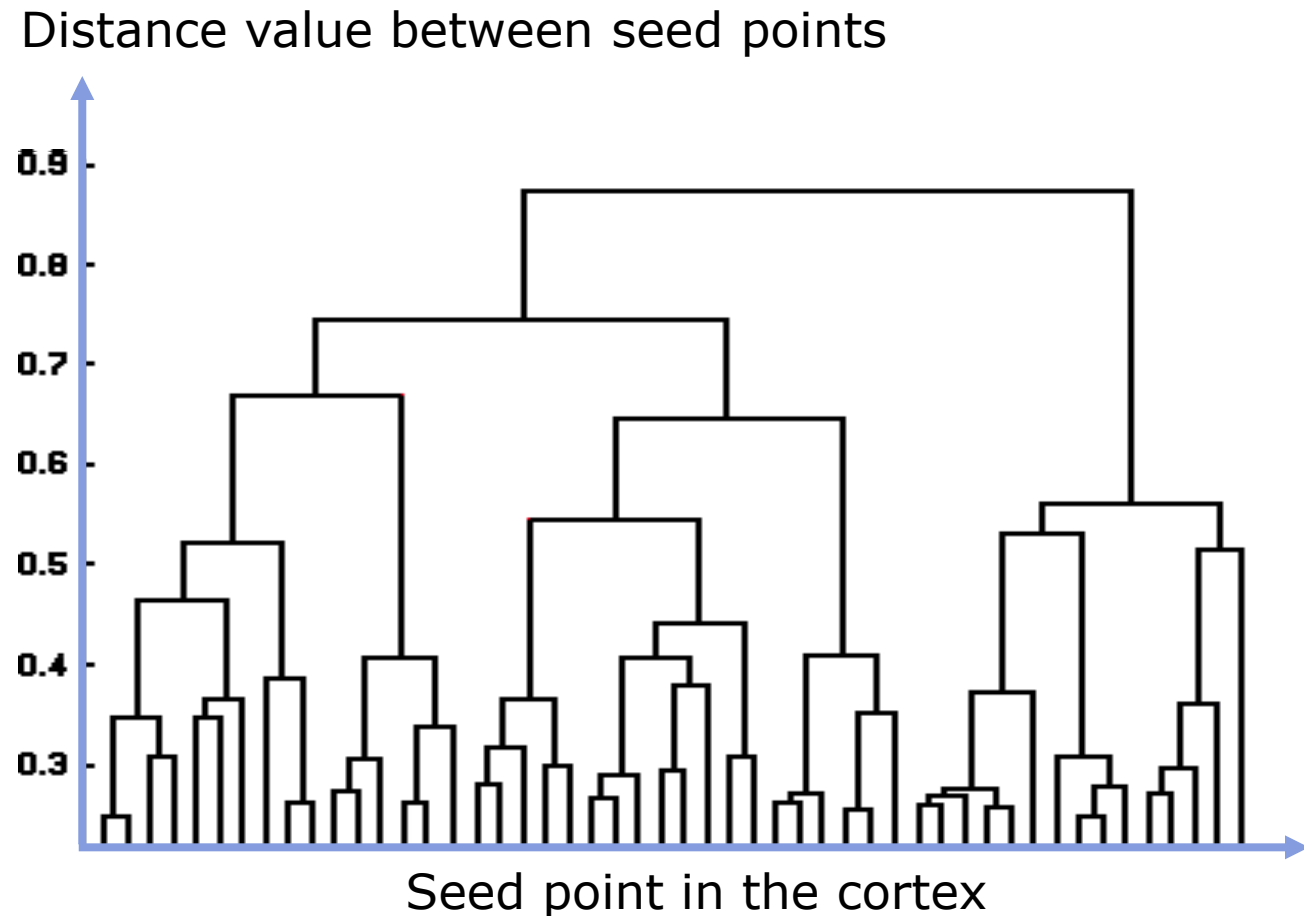
Distance = 0  $\rightarrow$  Same tractogram  
Distance = 1  $\rightarrow$  No overlap



Similarity = 0.3  
Distance = 0.7

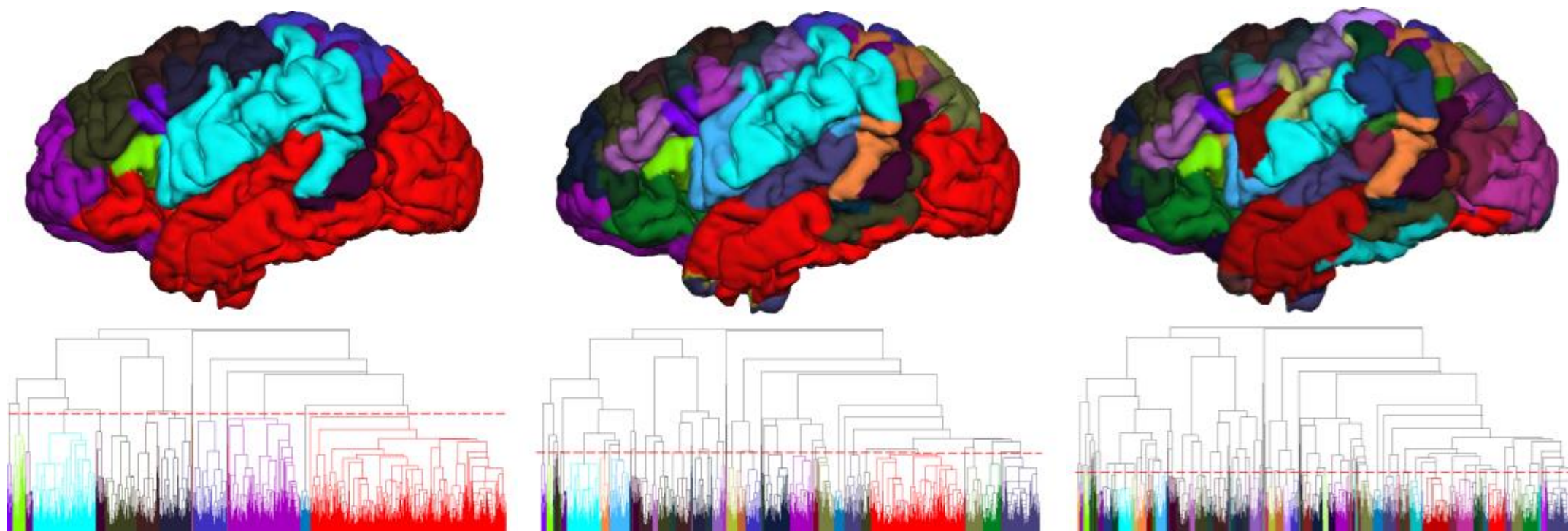
# Agglomerative hierarchical clustering

- Start with single points
- Join the two most similar elements
- Compute new distance to the other nodes
- Iterate until only one element remains (all original nodes)
- Initial elements are called leaves, all other elements nodes.





## Hierarchical parcellation of the human brain

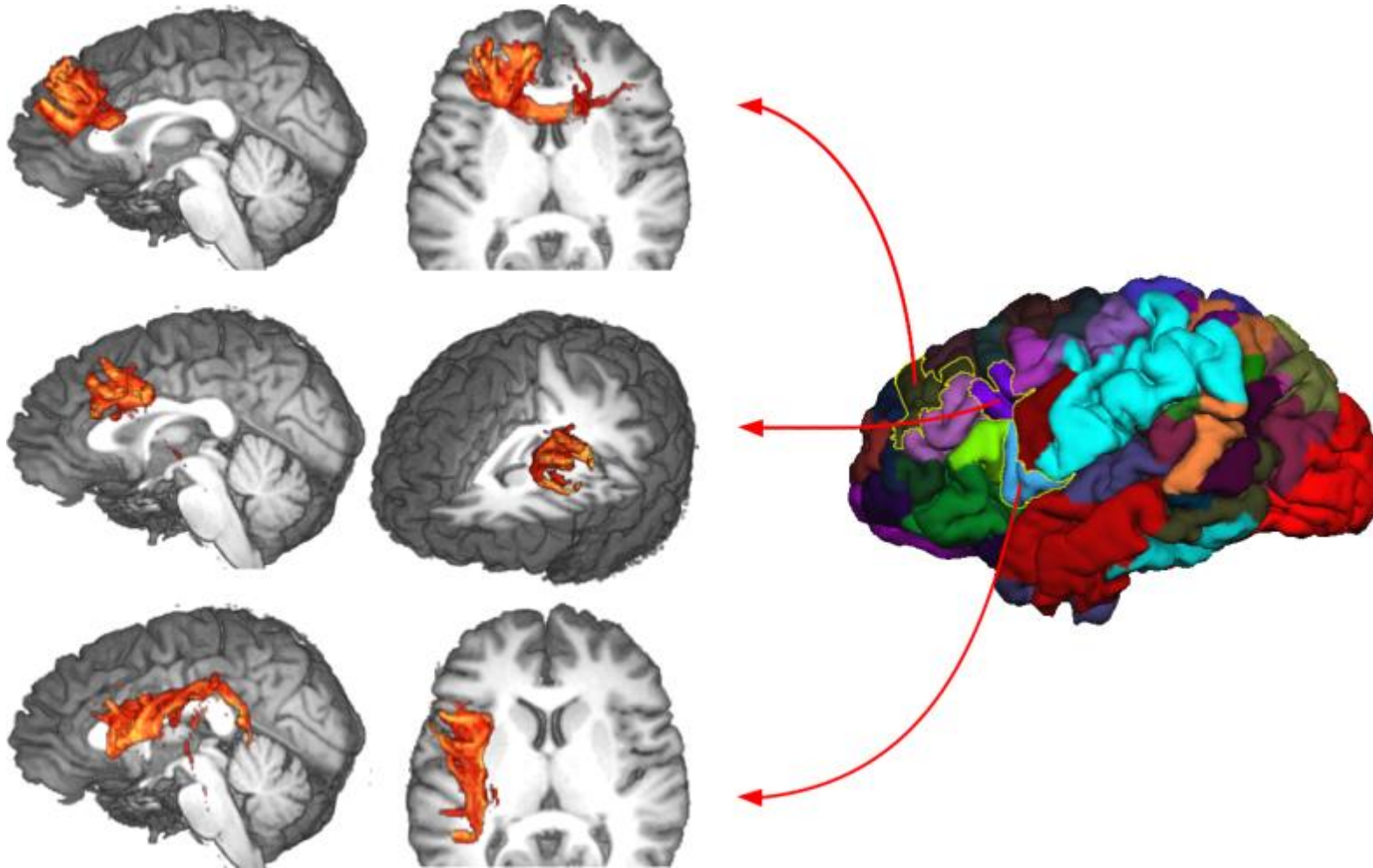


- Best representation of the tree by a **series** of parcellations
- Partitions yielding **15, 50 and 100** clusters for the left-hemisphere tree
- Different **criteria** for selecting parcellations proposed

*Moreno-Dominguez, Anwander et al. Hum Brain Mapp 2015*

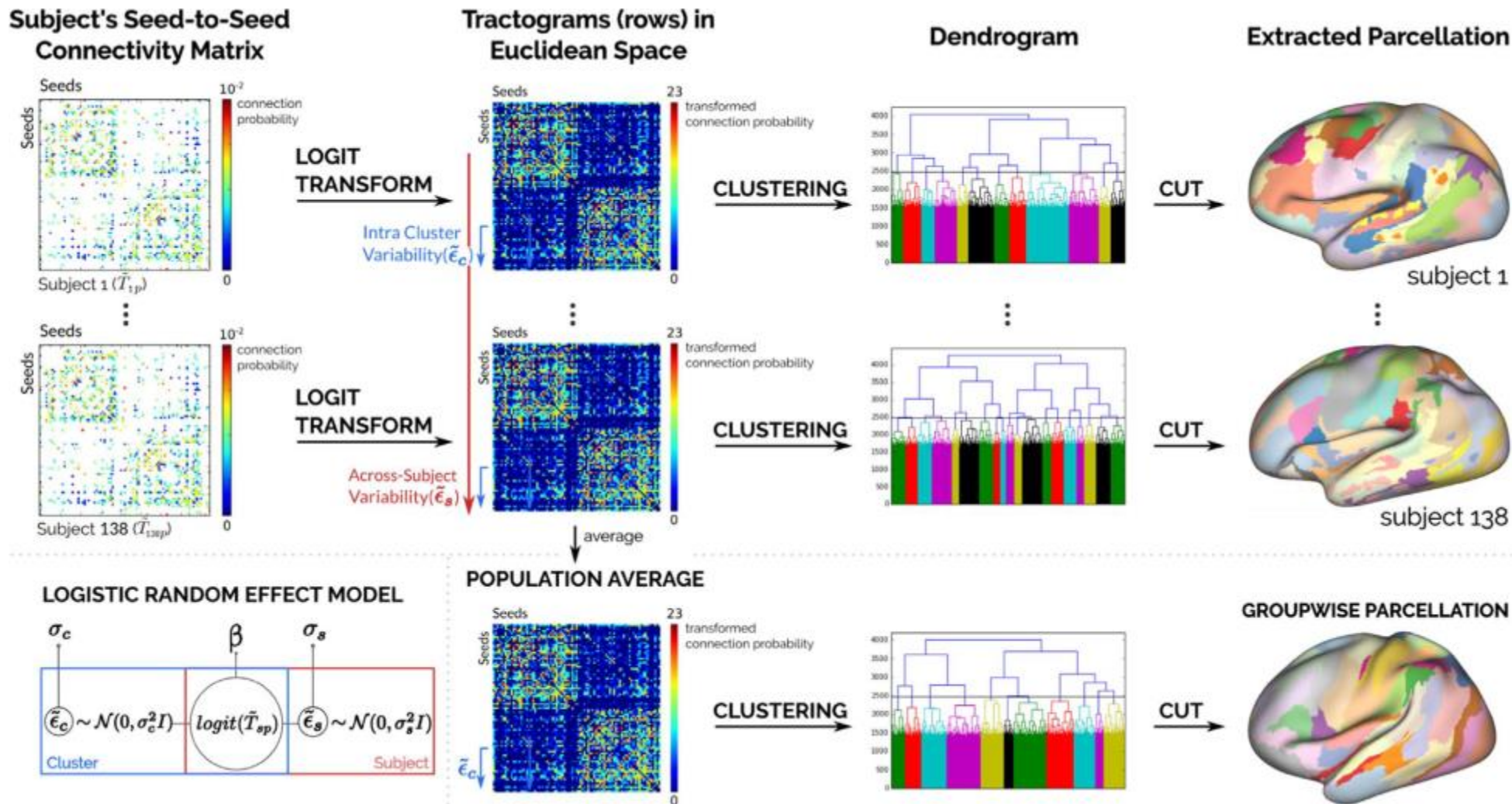


# Hierarchical connectom: Connectivity between regions



Mean tractograms of clusters  
on the superior and lateral  
frontal lobe.

# Groupwise structural parcellation



G. Gallardo et al., Neuroimage 2017



@AlfredAnwander

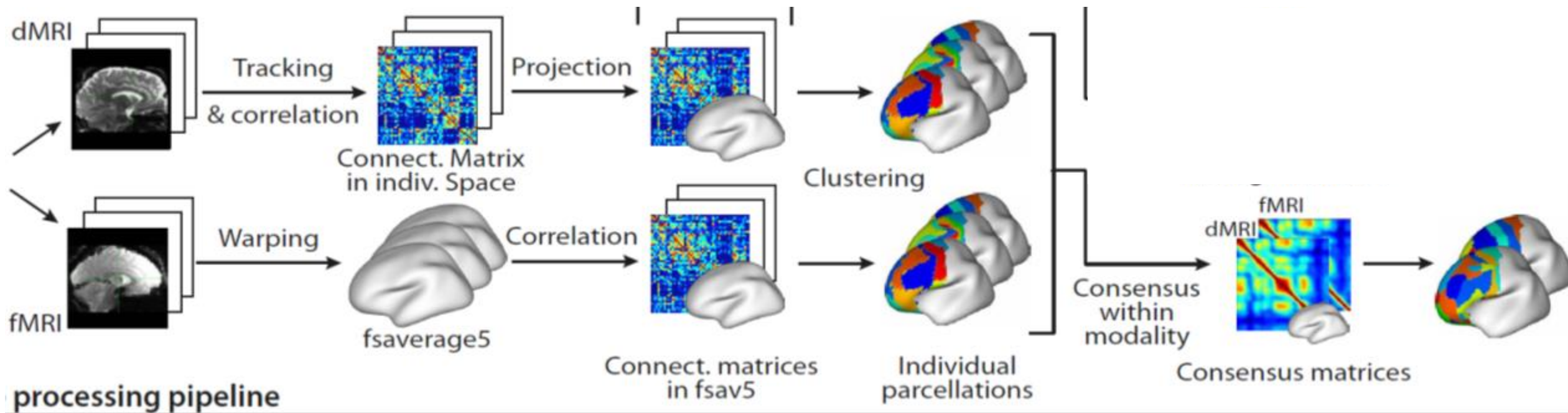
anwander@cbs.mpg.de CoBCom 2017, Juan-les-Pins

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# Functional and structural parcellation of the individual brain

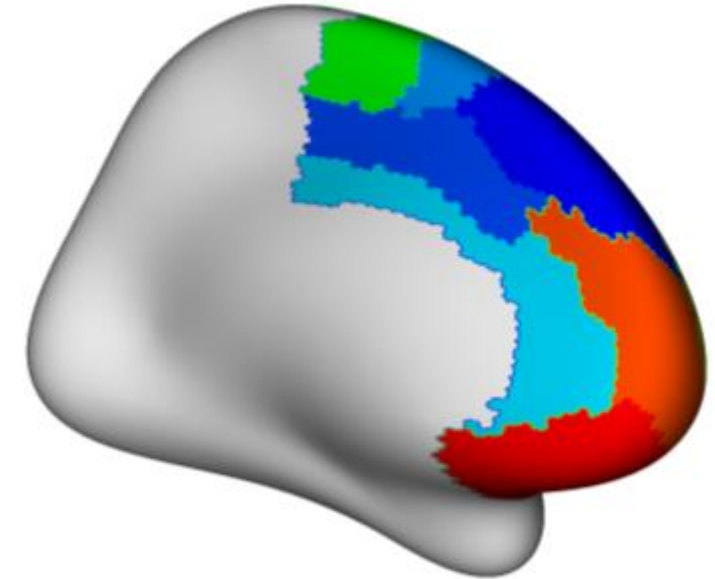
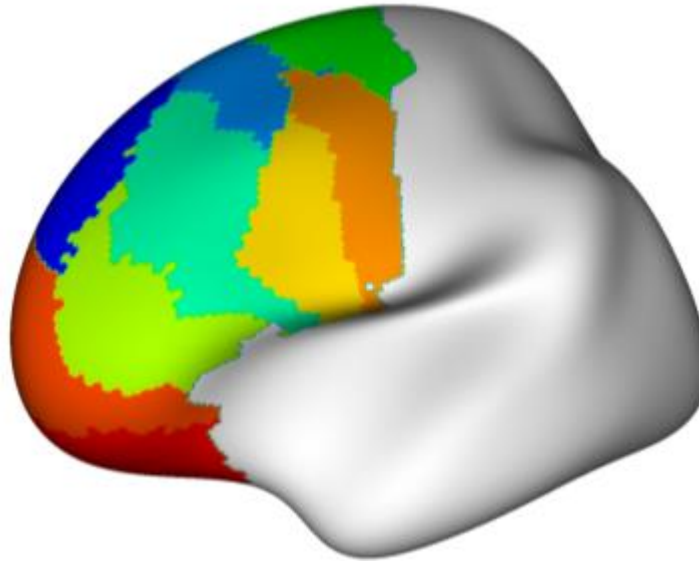
- Separate individual parcellation based on the structural and functional connectivity matrix
- Consensus clustering over groups



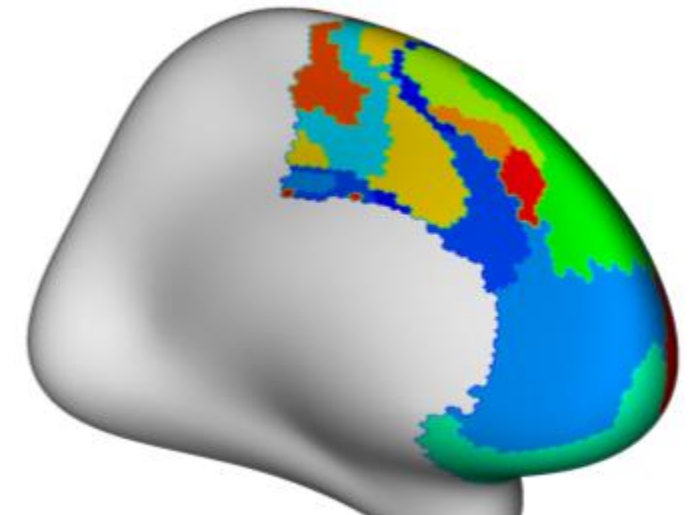
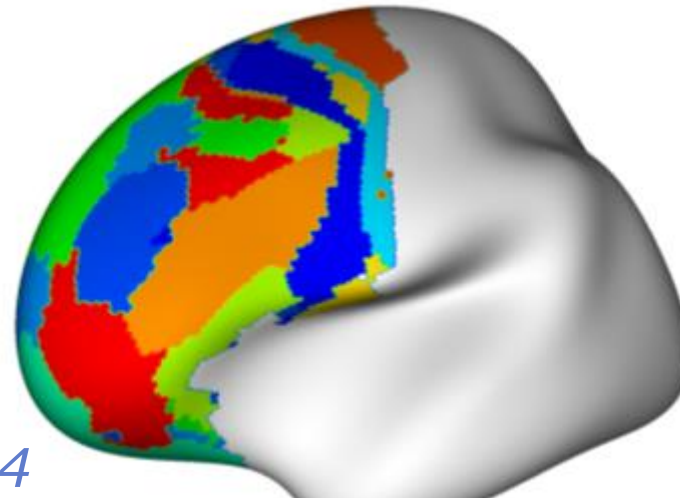
Moreno-Dominguez et al. OHBM 2014

# Functional and structural parcellation of the individual brain

- Diffusion MRI tractography based consensus parcellation



- fMRI connectivity based consensus parcellation
- See also poster 90: Guillermo Gallardo



*Moreno-Dominguez et al. OHBM 2014*



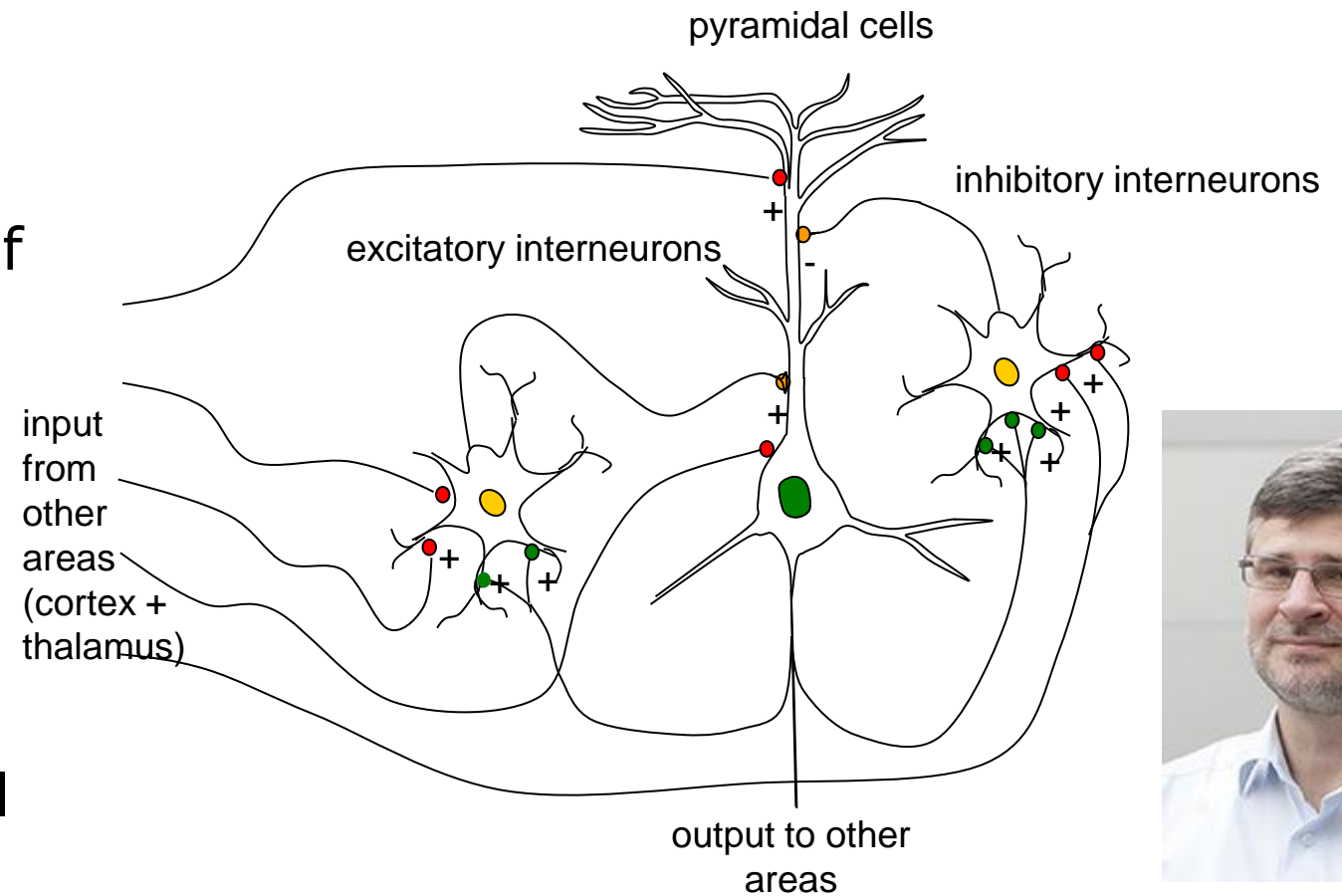
Can we do better?

Can we predict functional data?



# Computation of functional connectivity from the connectome

- Non-linear neural mass model
  - Neural mass: region of homogeneous activity
  - pyramidal cells
  - interneurons
- Balloon-Windkessel hemodynamic model to compute the BOLD signal



Courtesy: T.R. Knösche

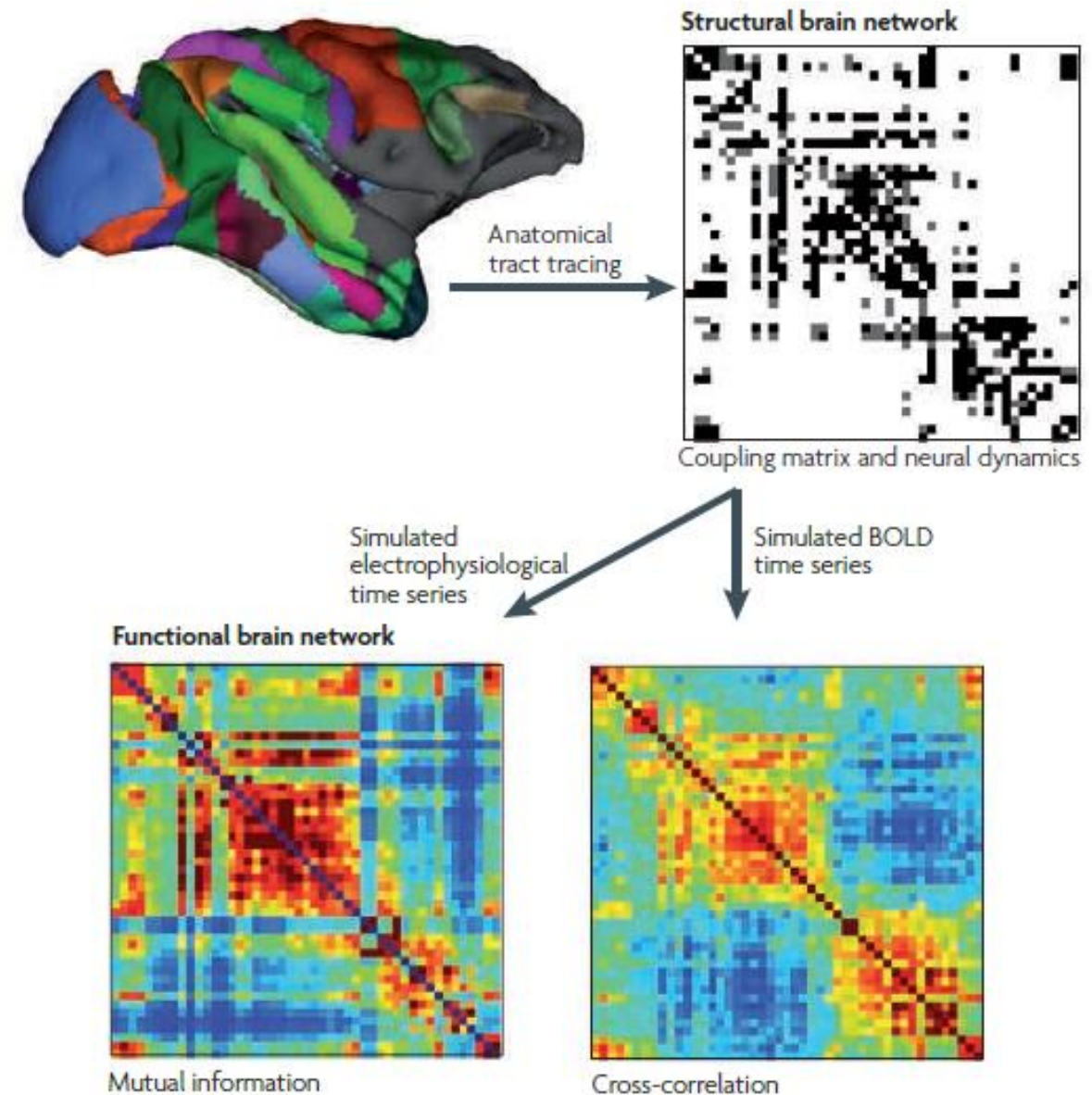
*Siegler et al Neuroimage 2010; Breakspear et al. 2003; Buxton, MRM 1998*





# Computational models to simulate dynamic patterns of activity

- Neural mass model – conductance based model of neural dynamics
- Emulate neuronal dynamics in macaque neocortex
- Simulated electrophysiological data
- Simulated BOLD data
- Compute connectivity matrices from the data

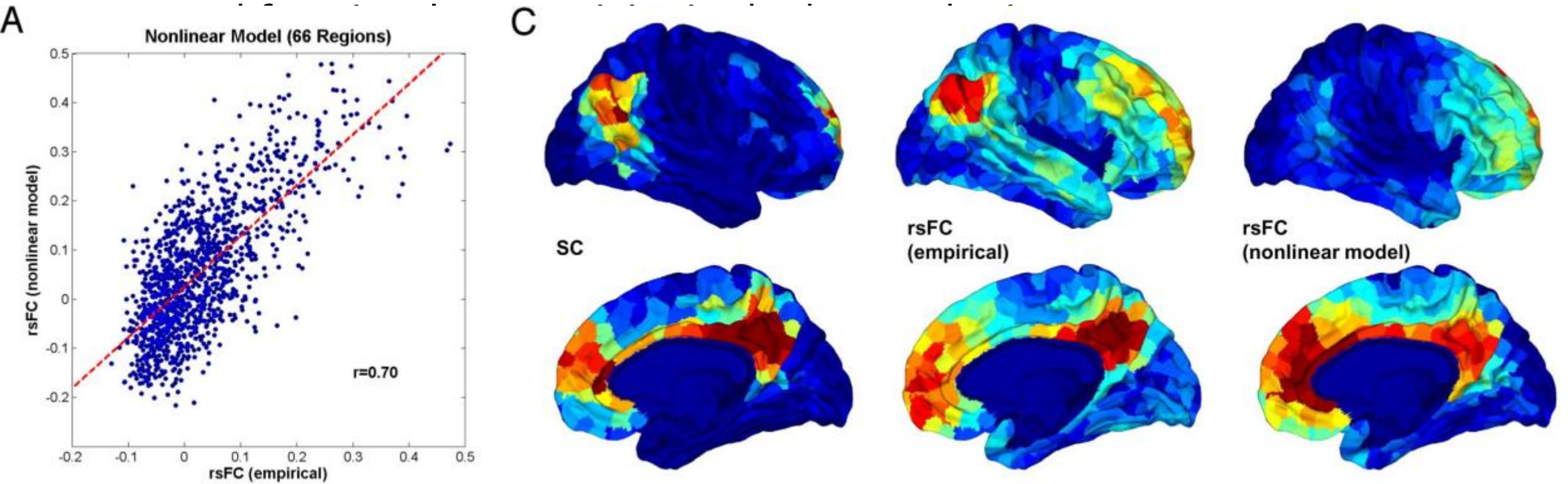


*Bullmore & Sporns Nat Rev Neurosci 2009, Honey et al. PNAS 2007*



# Predicting human resting-state functional connectivity from structural connectivity

- Systematic analyses of the relationship between structural



*Honey et al. PNAS 2009*



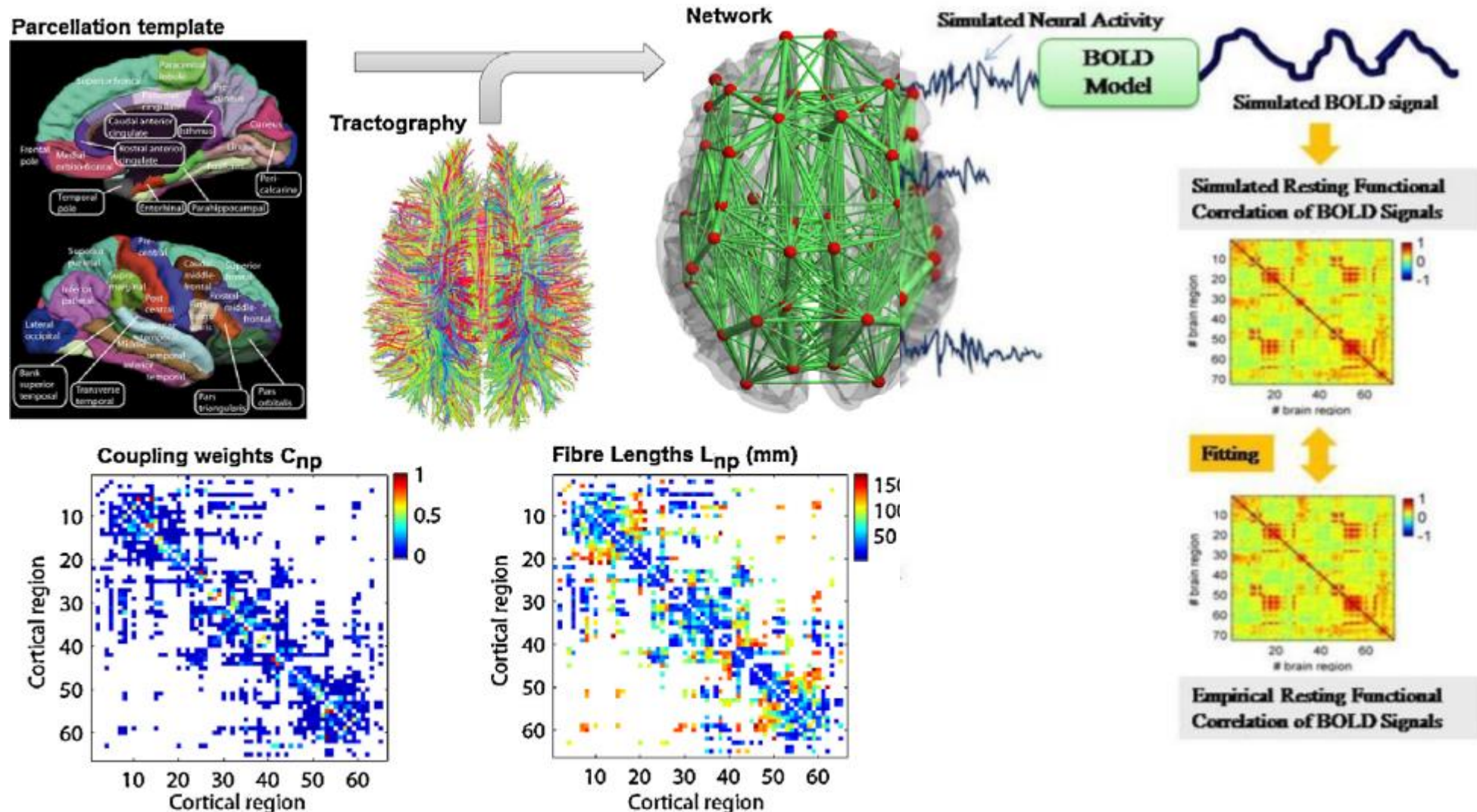
Can we do better?

Include the enhanced connectome





# Exploring the network dynamics

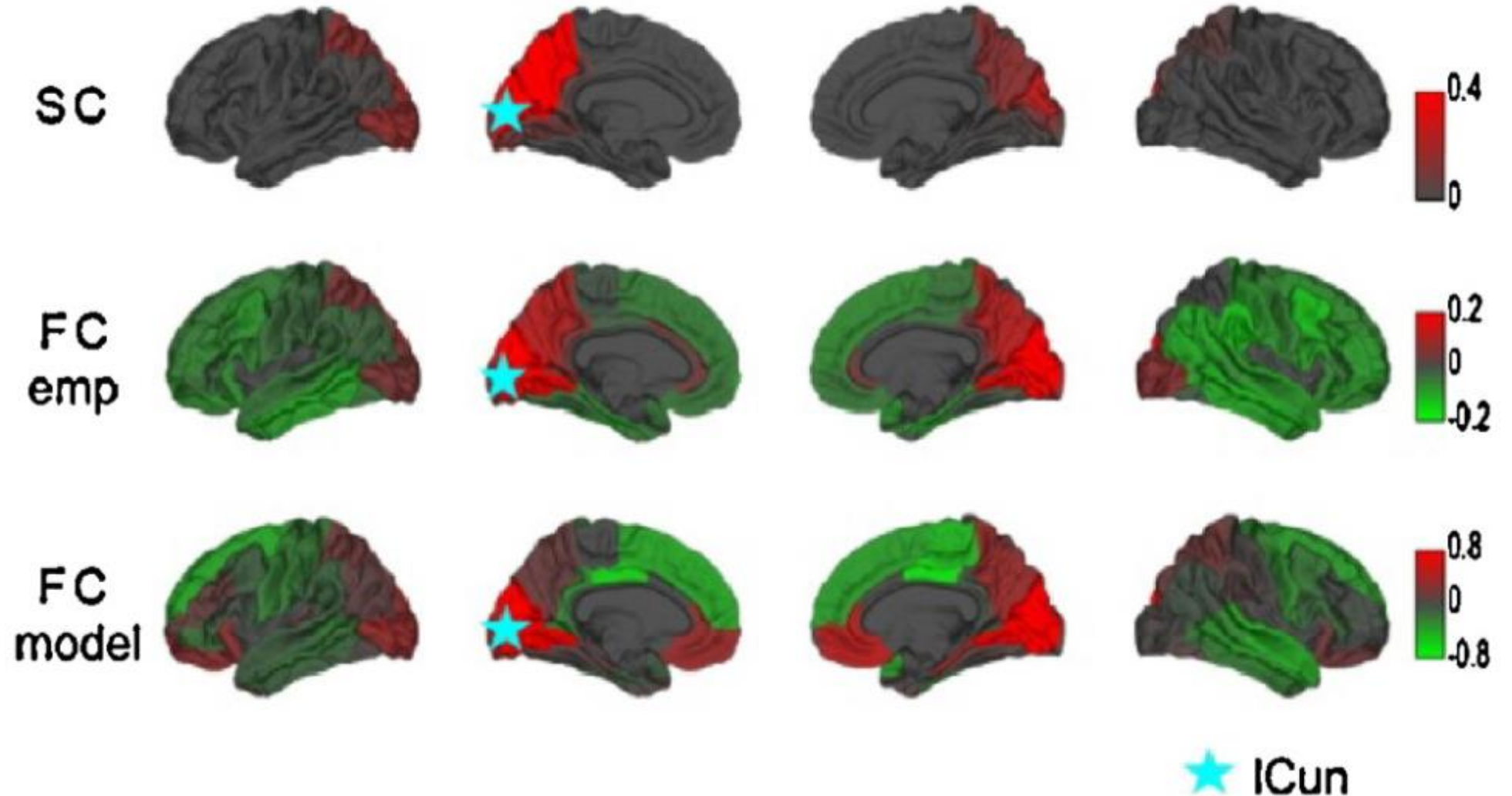


Cabral et al. Prog Neurobiol 2014, <http://www.thevirtualbrain.org>

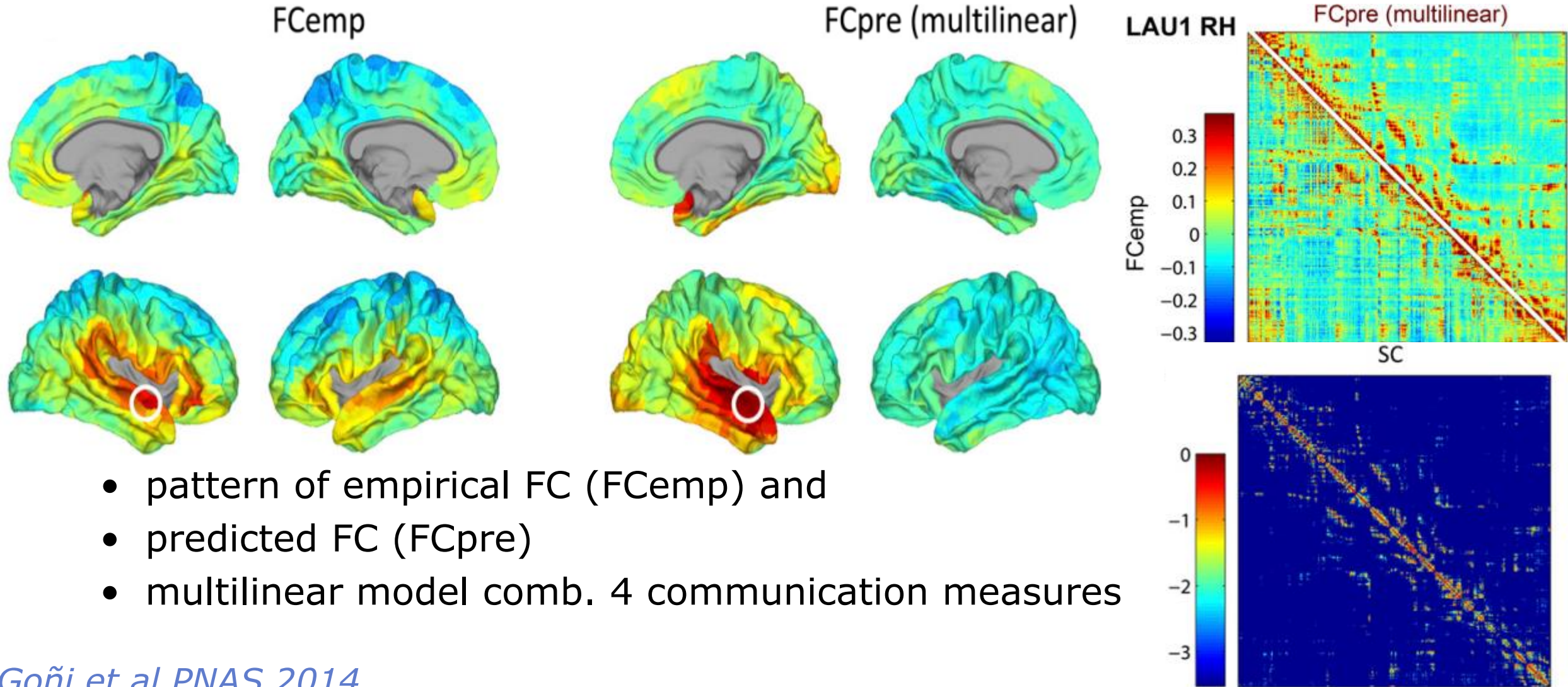




# Exploring the network dynamics



# Prediction of functional connectivity



Goñi et al PNAS 2014



Can we do better?

Compute directed connectivity



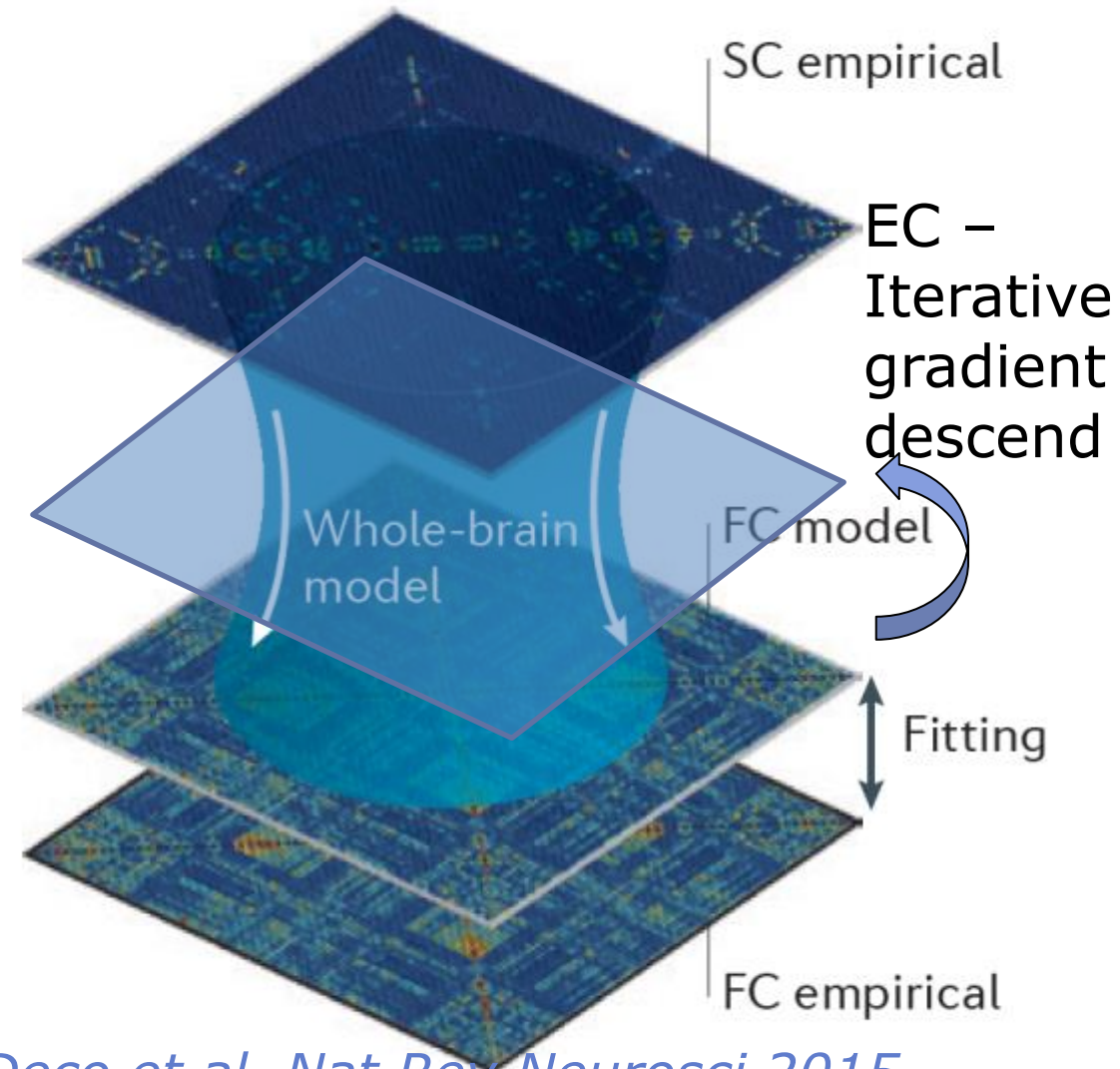


# Directed effective connectivity from fMRI and dMRI

- Structural connectome provides empirical data
- Interaction depends also on the dynamical properties: excitation / inhibition
- Directedness of regional interaction can be incorporated



Optimize effective connectivity parameters in a gradient descent iterative algorithm



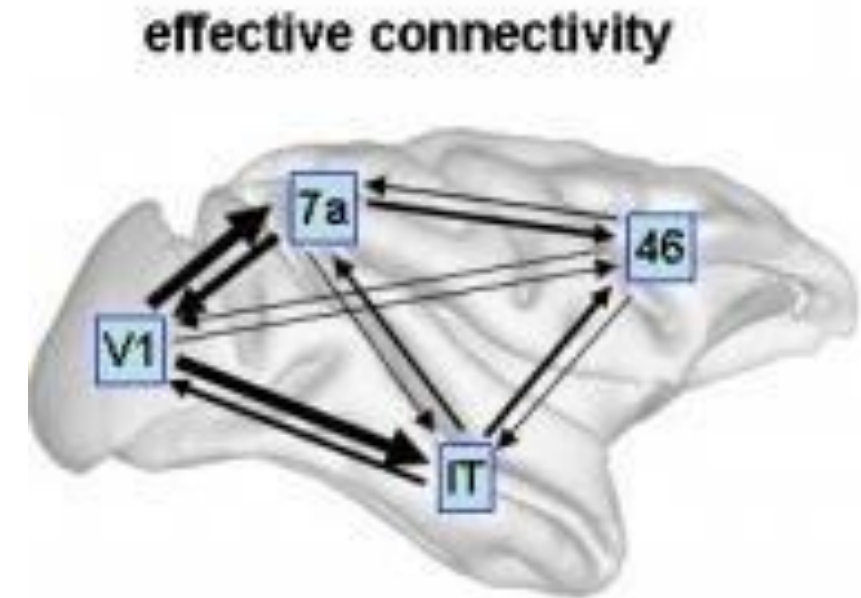
*Gilson PLoS Comput Biol. 2016, Deco et al. Nat Rev Neurosci 2015*





# Structure and function must be linked to compute effective connectivity

- Functional connectivity **correlates** with structural connectivity
- Causal relation to structural connectivity
- Functional connectivity can be **computed from structural** connectivity
- **Enriched connectomes** improves the prediction
- Advanced computational neuroscience models provides Effective connectivity: directed (causal) interregional interaction



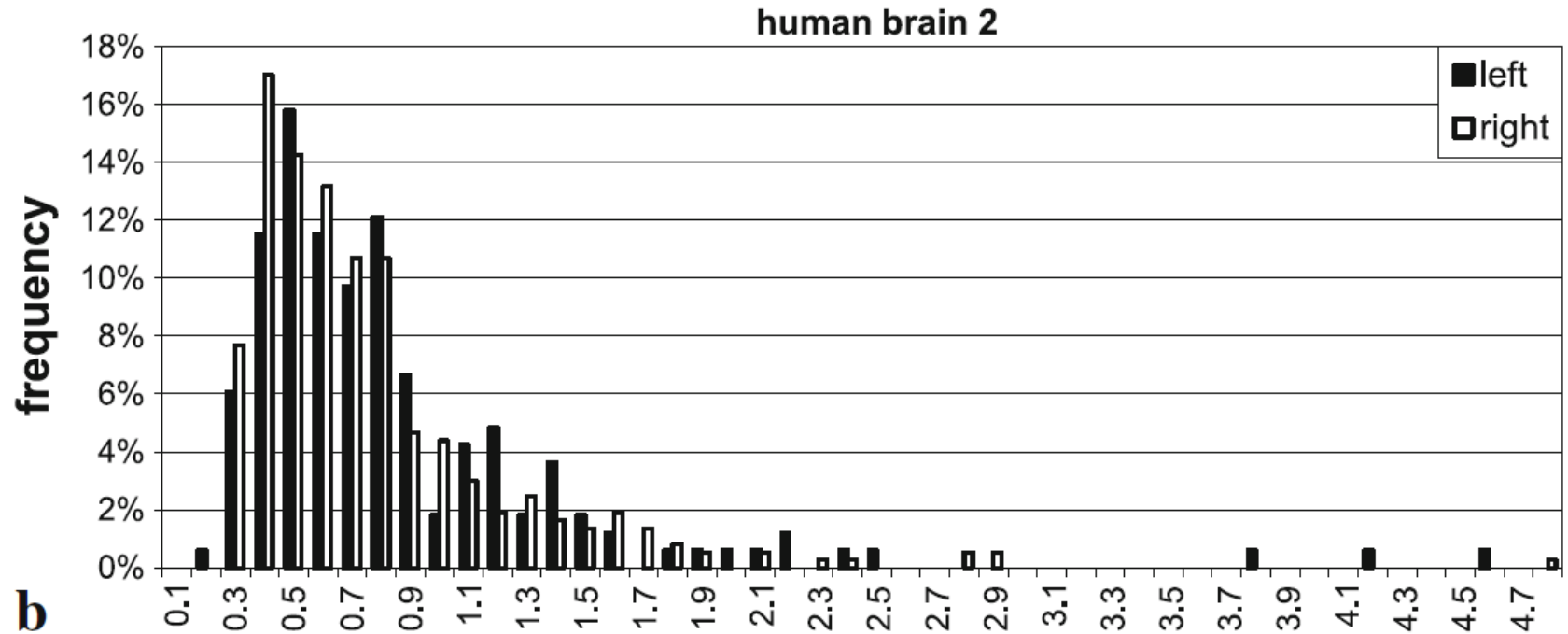
# Information transfer in the brain

- Axonal conduction speed  $\sim$  axonal myelination
  - R1/MT in MPM
- Axonal conduction speed  $\sim$  axonal diameter
  - AxCaliber
- Connection strength  $\sim$  axonal density
  - NODDI / CHARMED
- Combined models needed



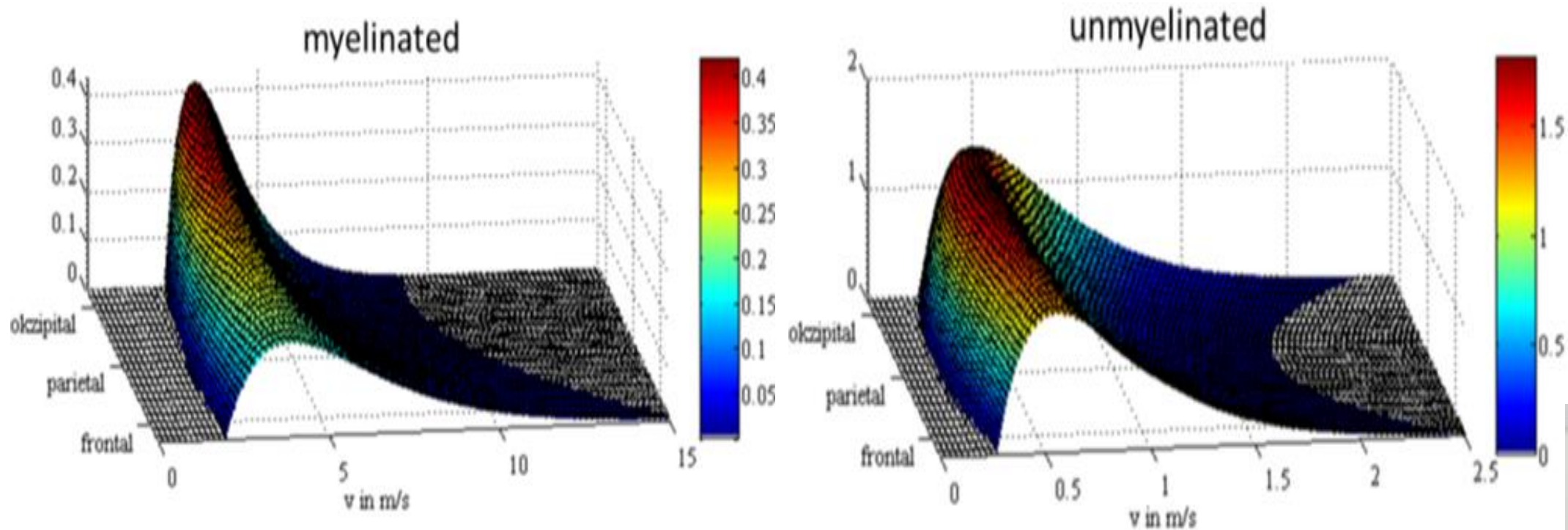
# Information transfer speed in the connectome

- axonal delay time
- tract length
- axonal density
- myelination
- g-ratio
- axonal diameter



- Axonal diameter distribution of myelinated axons in the superior longitudinal fascicle of the three human brains in the *left* and *right* hemisphere

# Estimated velocity profiles for myelinated and unmyelinated fibers in the corpus callosum



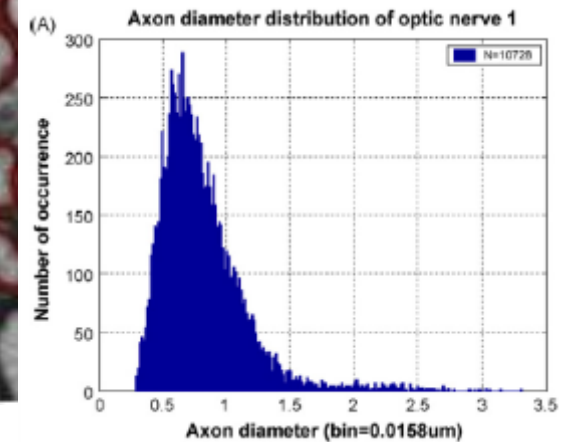
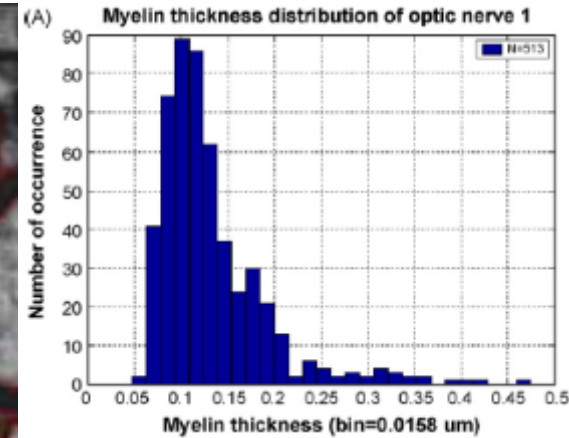
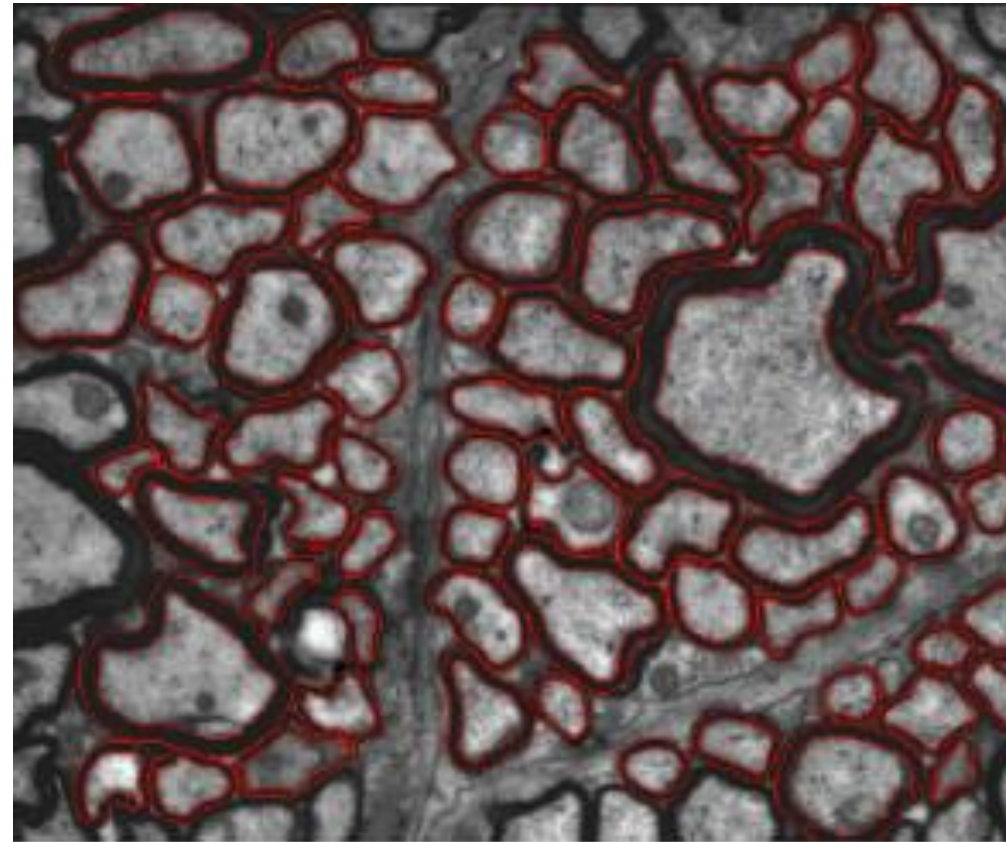
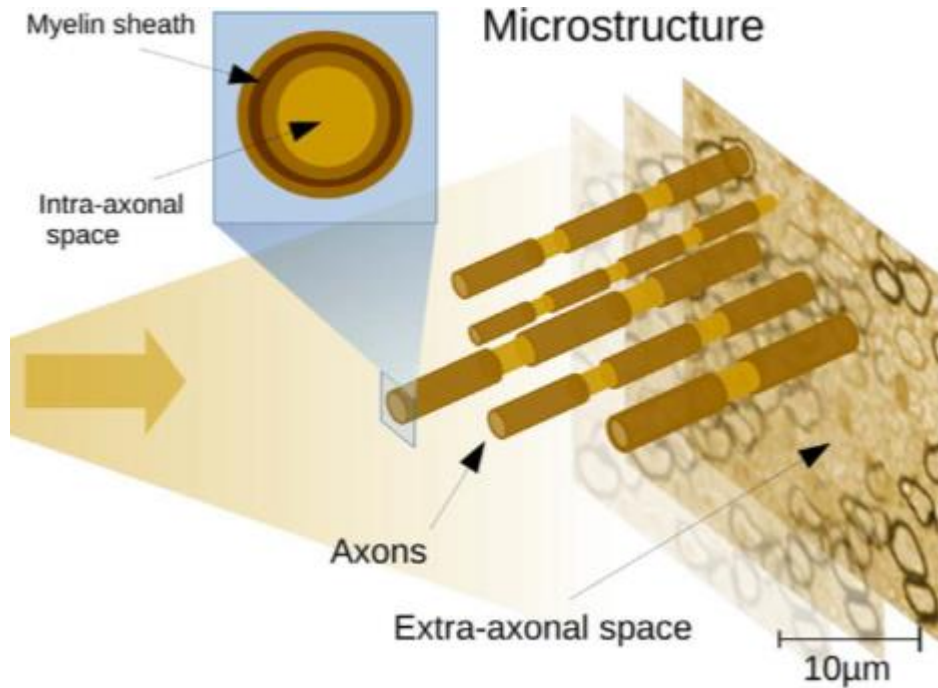
- Estimated velocity profiles in the rat's corpus callosum, based on axonal caliber measurements of Partadiredja et al.

*Koch Master 2011, Partadiredja et al. J Neurocytology, 2003*





# But how can we measure the axonal diameter? Electron microscopy



*M. Reisert et al. Neuroimage 2017; Zhao et al., Comput Med Imaging Graph 2010*



# MRI models for micro-structural properties

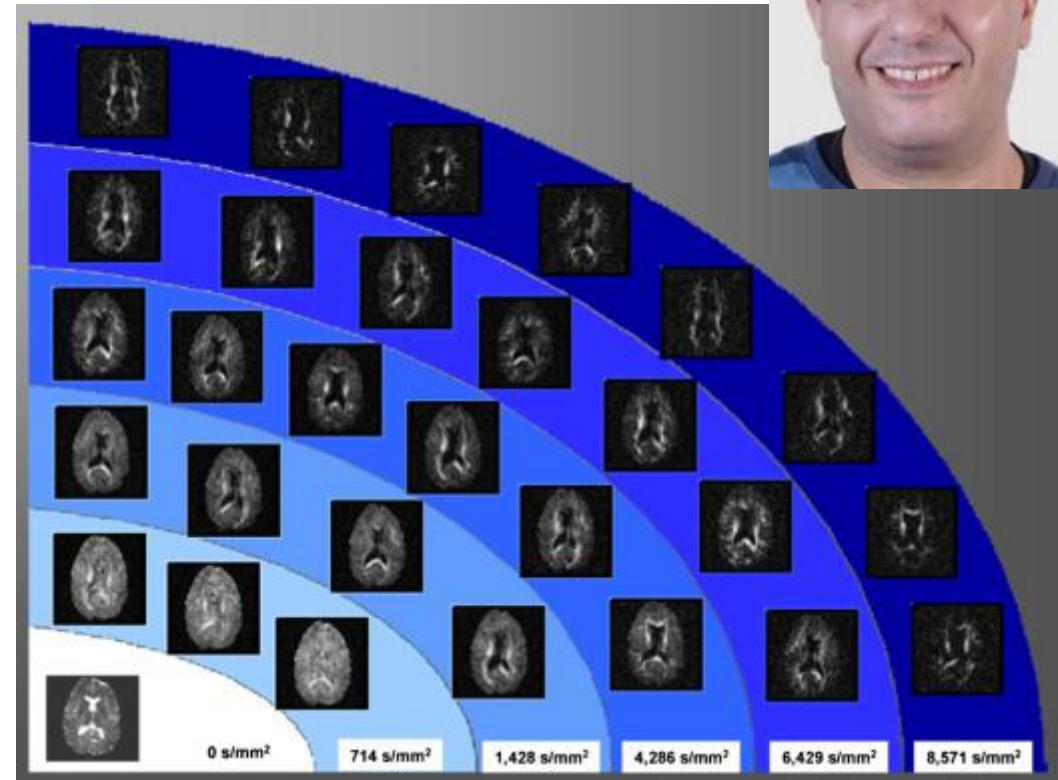


CHARMED (Composite hindered and restricted model of diffusion: Assaf 2004)

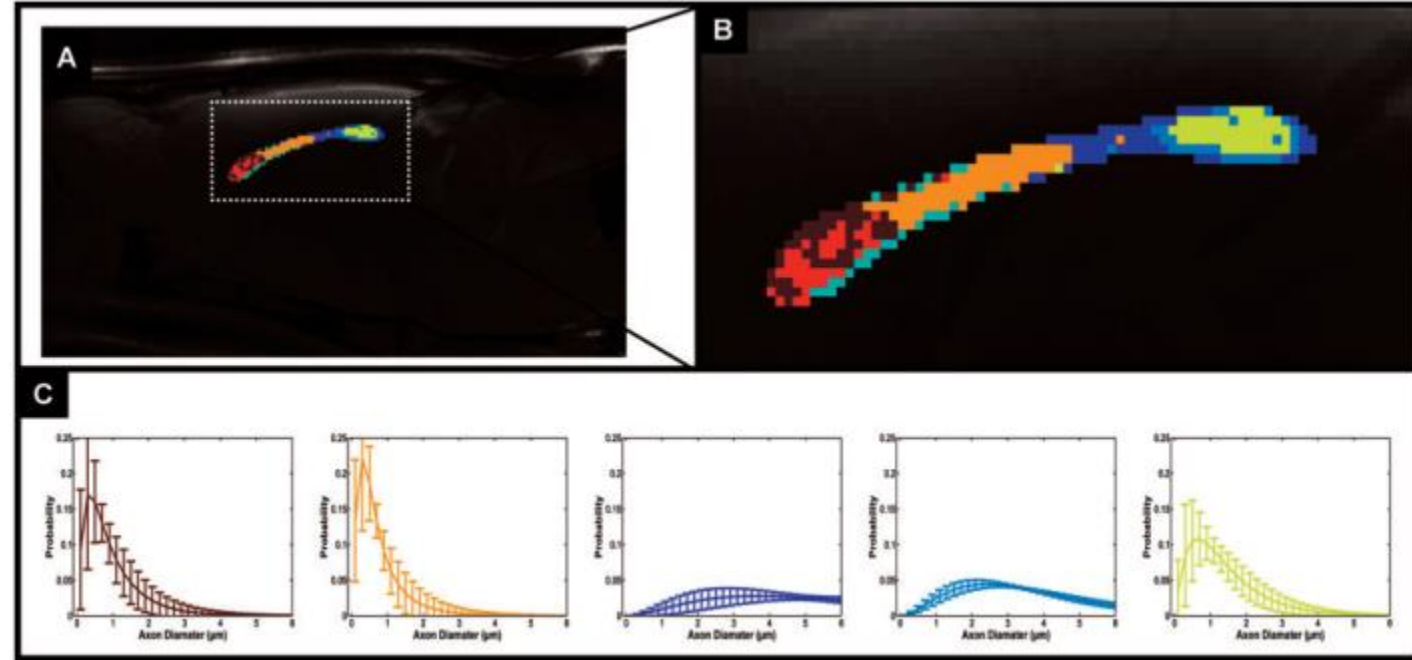
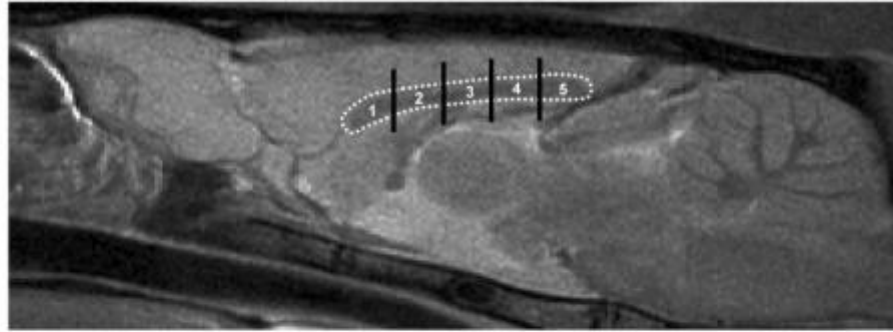
- **axonal density**
- two diffusion comp.: hindered and restricted
- Multi-shell acq. -> high b-values

AxCaliber (Assaf et al. 2008)

- axonal diameter distribution
- acquisition **perpendicular** to the fiber direction (e.g. CC)
- **Multi-shell + multi-diffusion time measurement**



# MRI of axon diameter distribution in the corpus callosum



- AxCaliber: intra- and extra-axonal water diffusion
- Axon diameter distribution (ADD)
- Restricted diffusion in the axon, restricted outside

*Assaf et al. Magn Reson Med 2008; Barazany et al. Brain 2009*

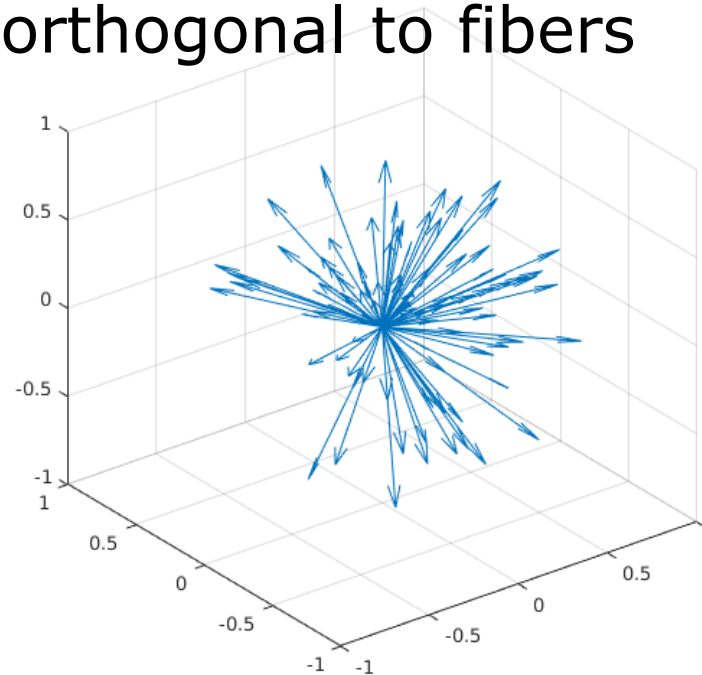




# Axon diameter modelling AxCaliber 3D 300 mT/m gradients (with Assaf group and Prof. Weiskopf)



- Diameter of crossing fibers
- Full sphere acq. - compute data orthogonal to fibers
- 79 directions
- 6 b-values (multi-shell)
- b-value=500 - 5000 s/mm<sup>2</sup>
- 3 CHARMED scans with different diffusion times 16 - 40 ms
  - (Prisma: 40 - 95ms)
- Fast pulses: delta=9ms



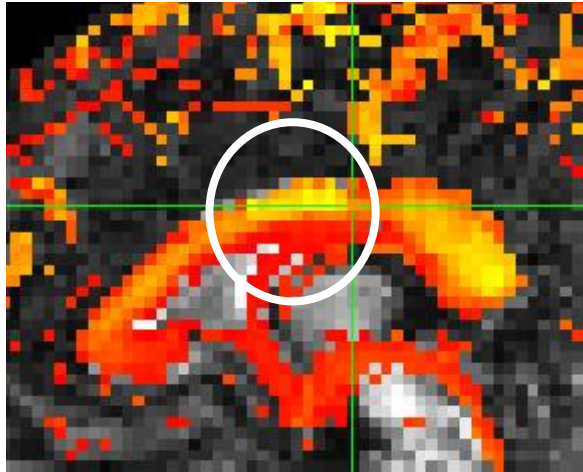
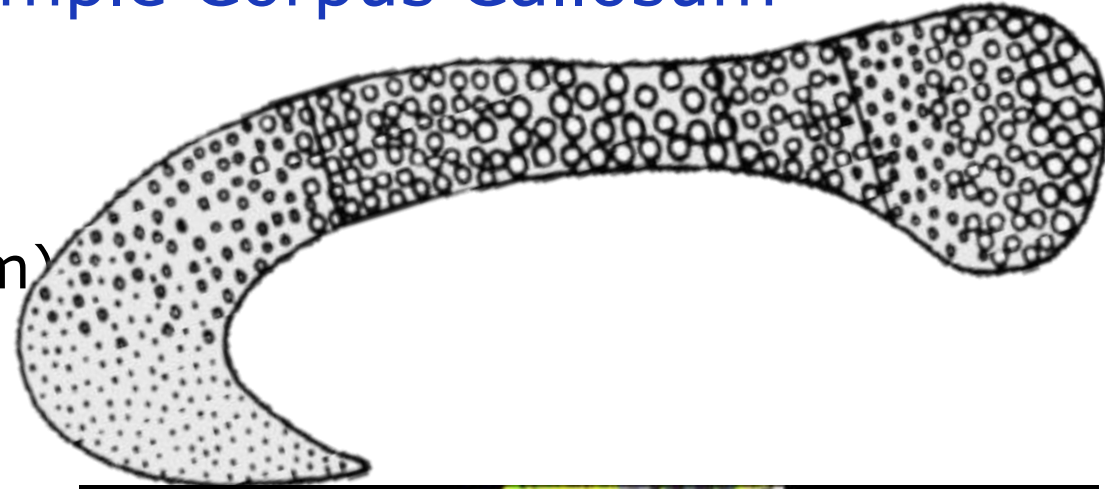
Bval (s/mm <sup>2</sup> )	Number of directions
500	8
1000	17
2000	12
3000	13
4000	14
5000	15



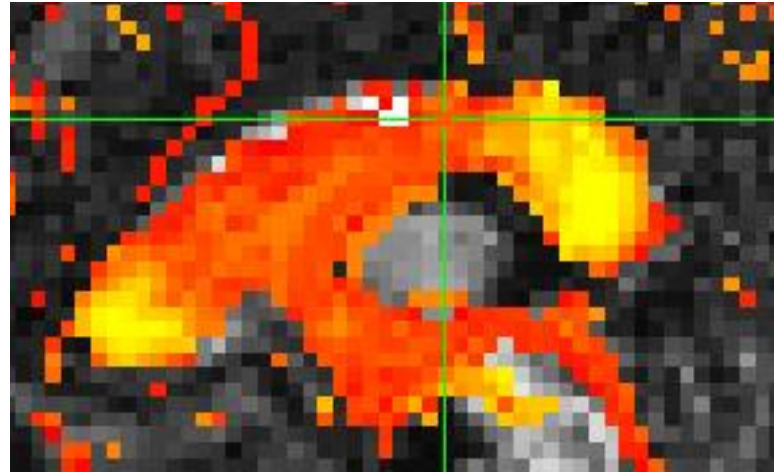


# Axon diameter modelling – example Corpus Callosum

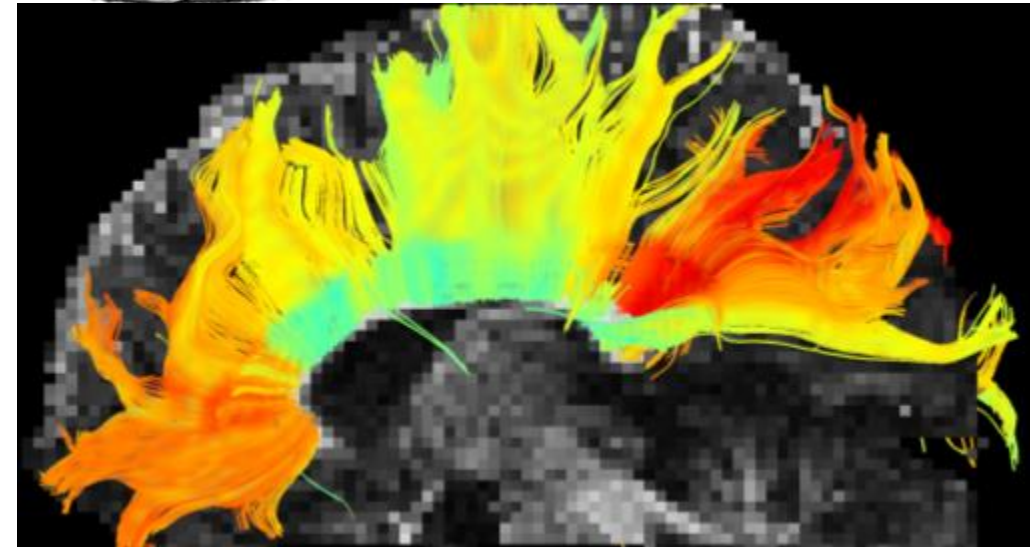
- A CSF component, a hindered diffusion
- Two axonal populations
  - small axons: narrow distr.: center  $1.5\mu\text{m}$
  - large axons: broad distr.: center  $4\mu\text{m}$



**large axons**



**small axons**



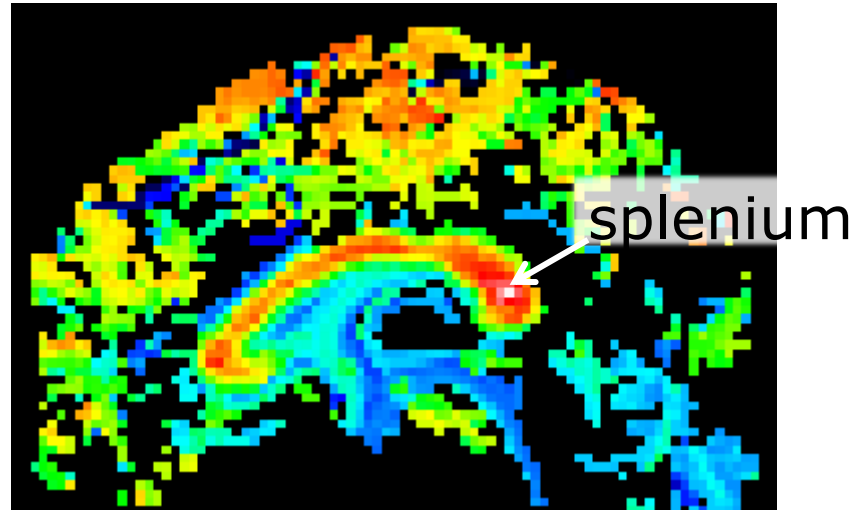
min **small axons** max

# Density and Ratio of small/big fibers

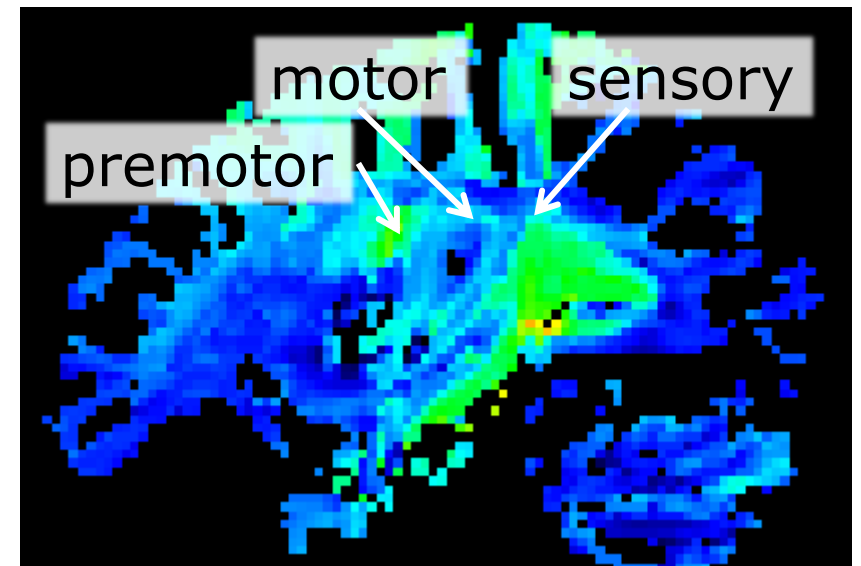
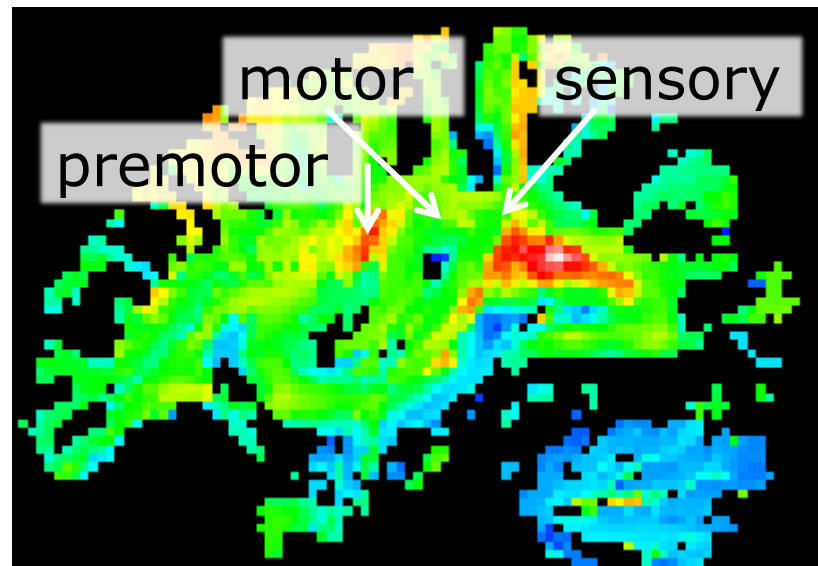
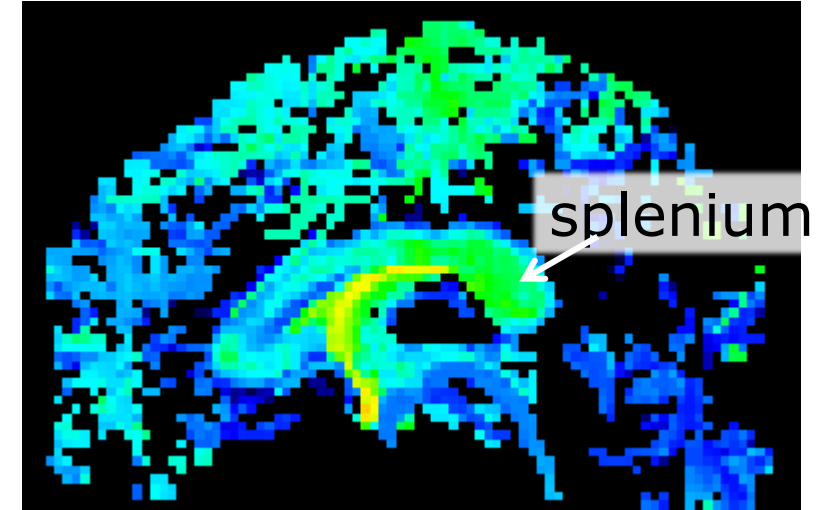
subj 1



### Relative fiber density



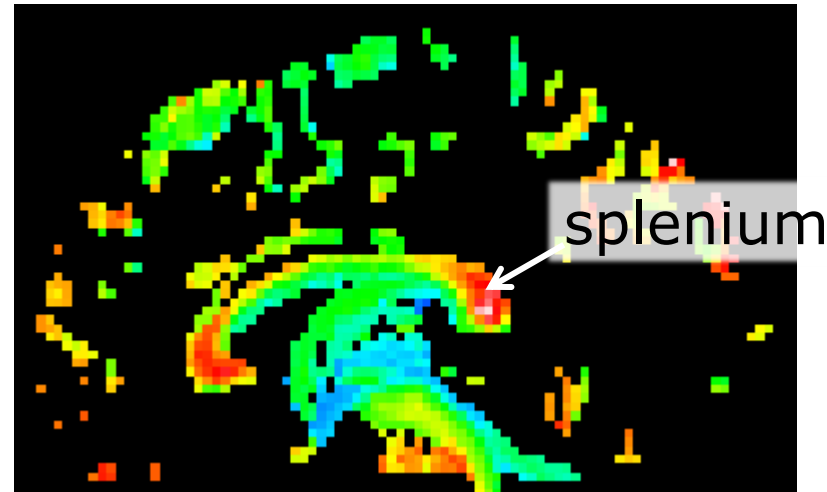
### Ratio small/large fibers



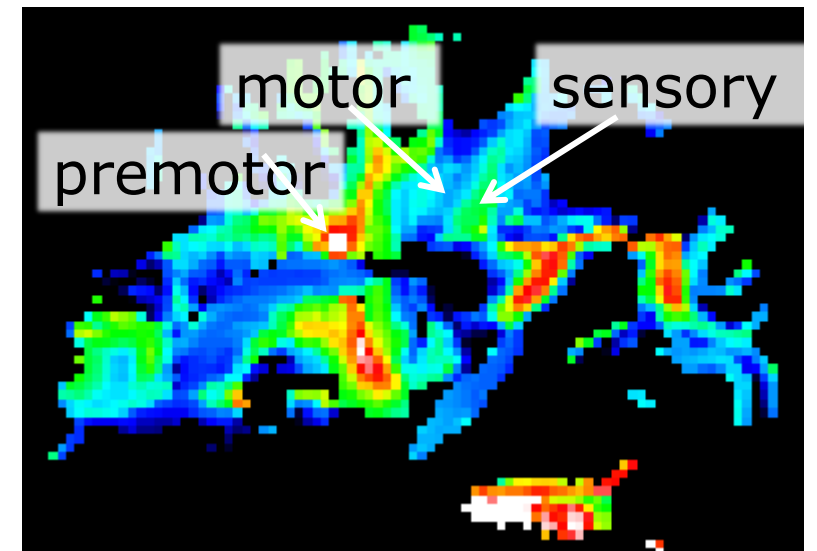
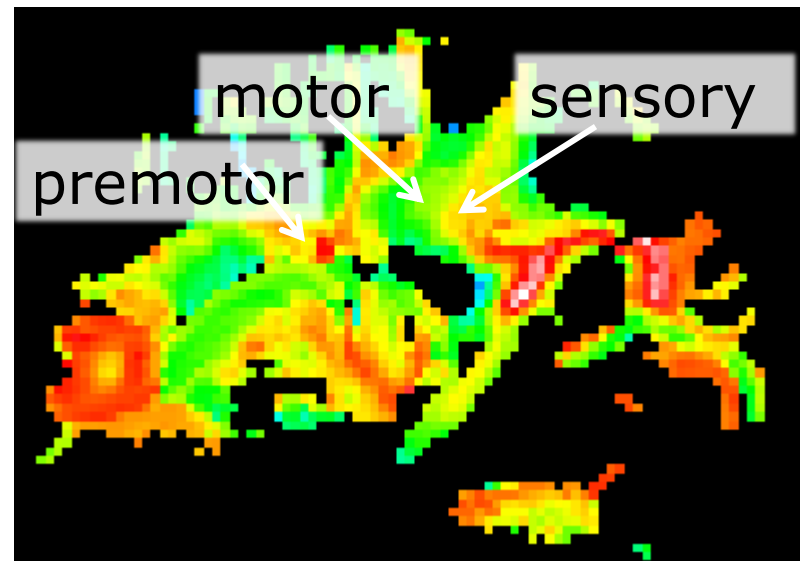
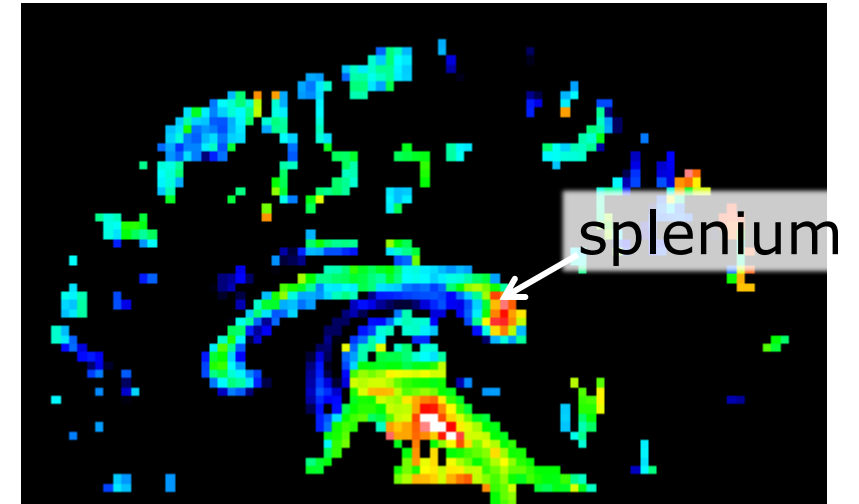
# Density and Ratio of small/big fibers

subj 2

### Relative fiber density



### Ratio small/large fibers



In collaboration with Yaniv Assaf and Assaf Horowitz, Aboitiz et al. 1992

## Axonal diameter - Perspectives

- Stronger gradients allowed to
  - reduce  $\delta$  (from 22 to 9 ms compared)
  - reduce  $\Delta$  (from 100 to 40 ms)
  - increasing the sensitivity to shorter displacements
- Optimize 3D AxCaliber model / acquisition
  - crossing fibers + myelin
- Combination with MEG measurements
  - with T. Knösche and G. Deco
  - transfer speed, synchronization, information flow
- **Can we detect plastic changes in axonal diameter?**



PhD and Post-doc positions available





# Quantitative Brain Plasticity: Application to in second language learning



Prof. A.D.  
Friederici



Tomás  
Goucha

How does adult brain **change**  
when **learning** a second language?

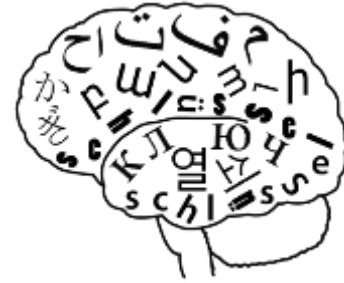
What are the dynamic mechanisms of  
long term brain plasticity?



# In 2015, we had a crazy idea!



# Second language acquisition



90 Arabic mother tongue speakers

- Intensive course — 6 Months — 5 h x 5 days a week
- ~300h of language learning : level B1 (CEFR)

T<sub>0</sub> – before course  
only **Structural MRI**

T<sub>1</sub> – after 3 months  
**Structural and functional MRI**

T<sub>2</sub> – after 6 months  
**Structural and functional MRI**

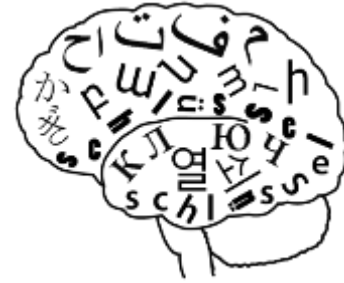
56 complete datasets

50 German control datasets without training

**Follow up: 6 months (35 people & Connectom)**

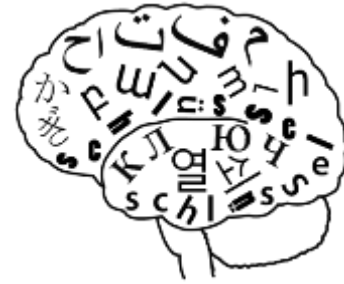


# MRI protocol



- High resolution **diffusion** MRI (PRISMA)
  - 1.3 mm isotropic
  - 60 directions,  $b=1000$ , SMS 2, GRAPPA 2, 21 min
- **NODDI** (neurite orientation dispersion and density imaging), 7 min
- Quantitative **Multiparametric Mapping** (qMPM) sequence
  - Multi-echo 3D FLASH (25 min) including:
    - predominant T1-, PD-, and MT-weighting
    - RF transmit field map, static magnetic ( $B_0$ ) field map
- Task **fMRI**. 2.5 mm isotropic, TR 1.5 sec



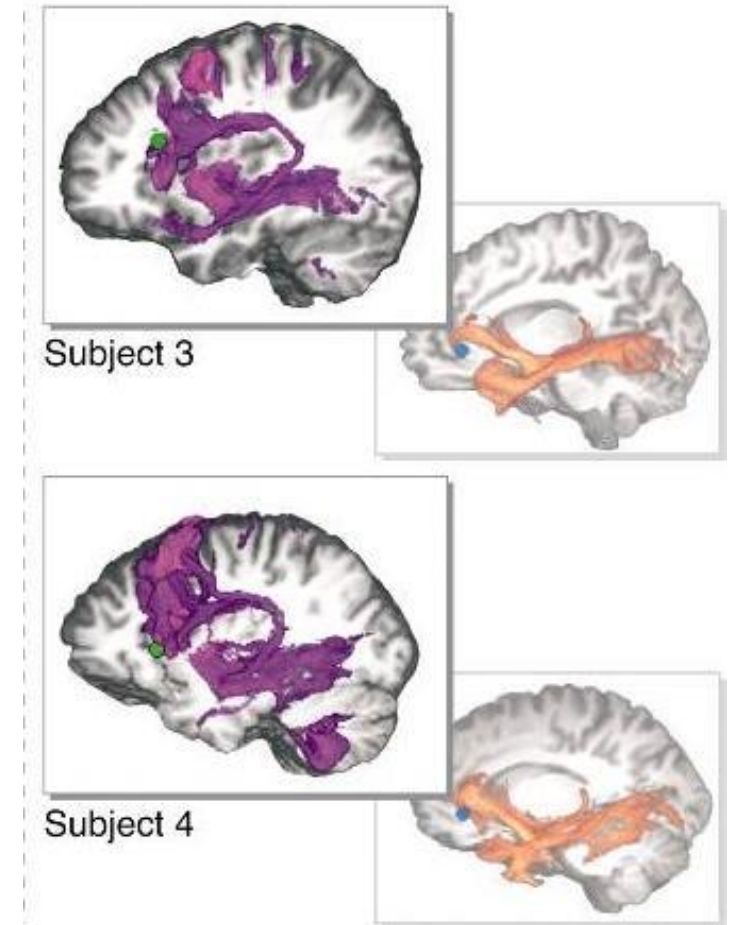
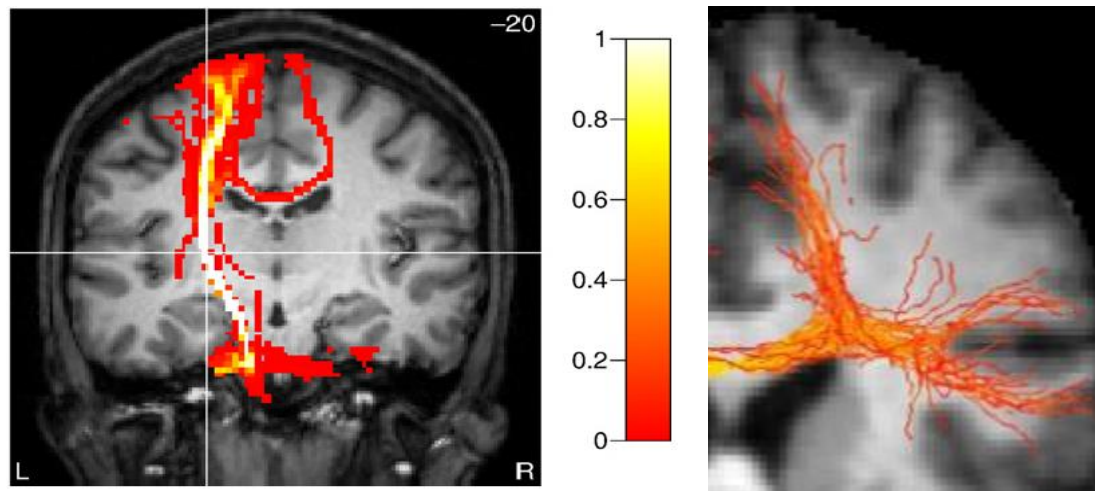


- Initial research questions:
- Do we find differences in the mother tongue language networks?
- Does the network of L2 learners adapt to the shape of the new language?



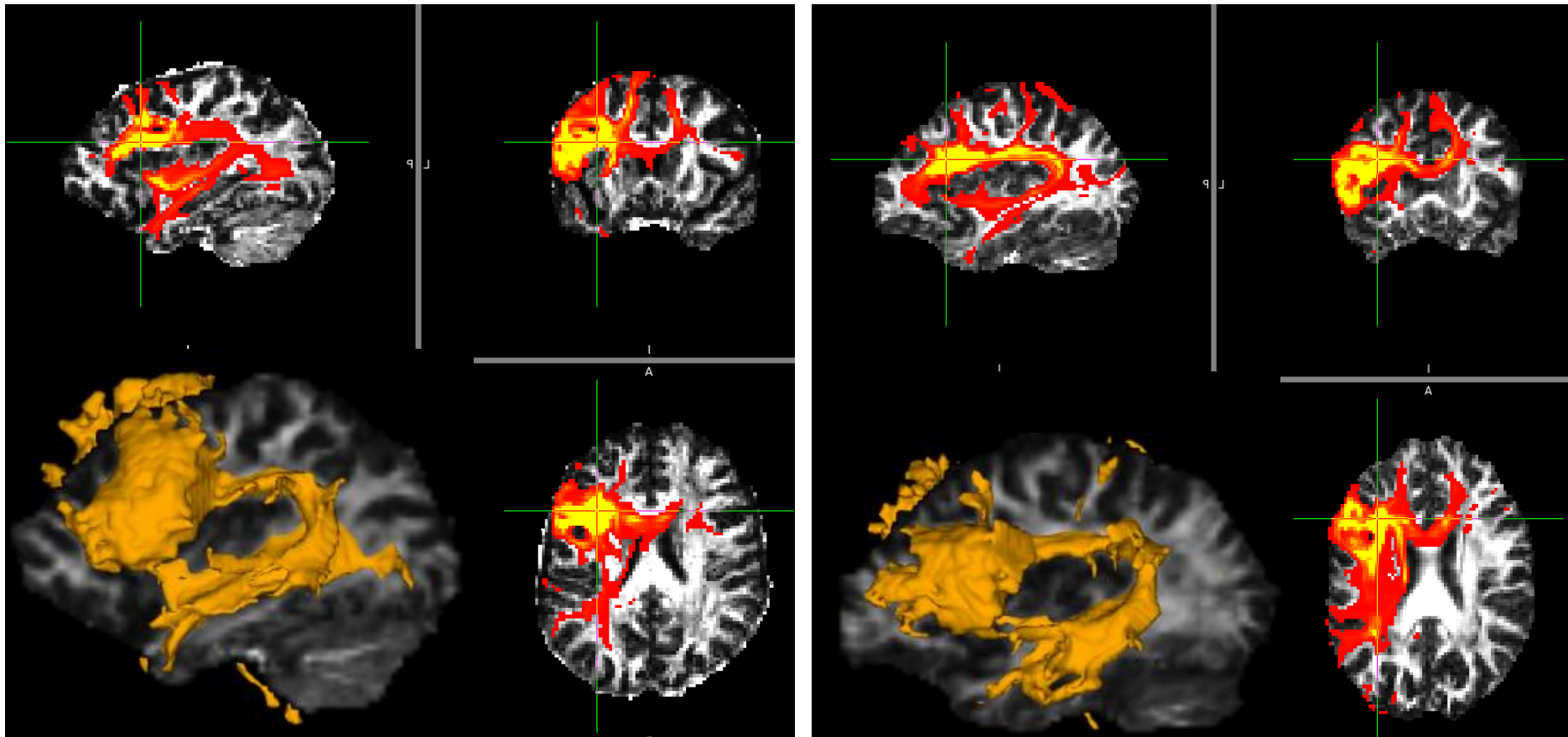
# New method: Directly compare probabilistic connectivity maps

- “Free” probabilistic tracking from seed ROI:  
Example: Broca’s area and FOP
- Value in every voxel correspond to the rel. number of streamlines



# How can we compare two connectivity maps?

- Example: BA44 connectivity of two participants



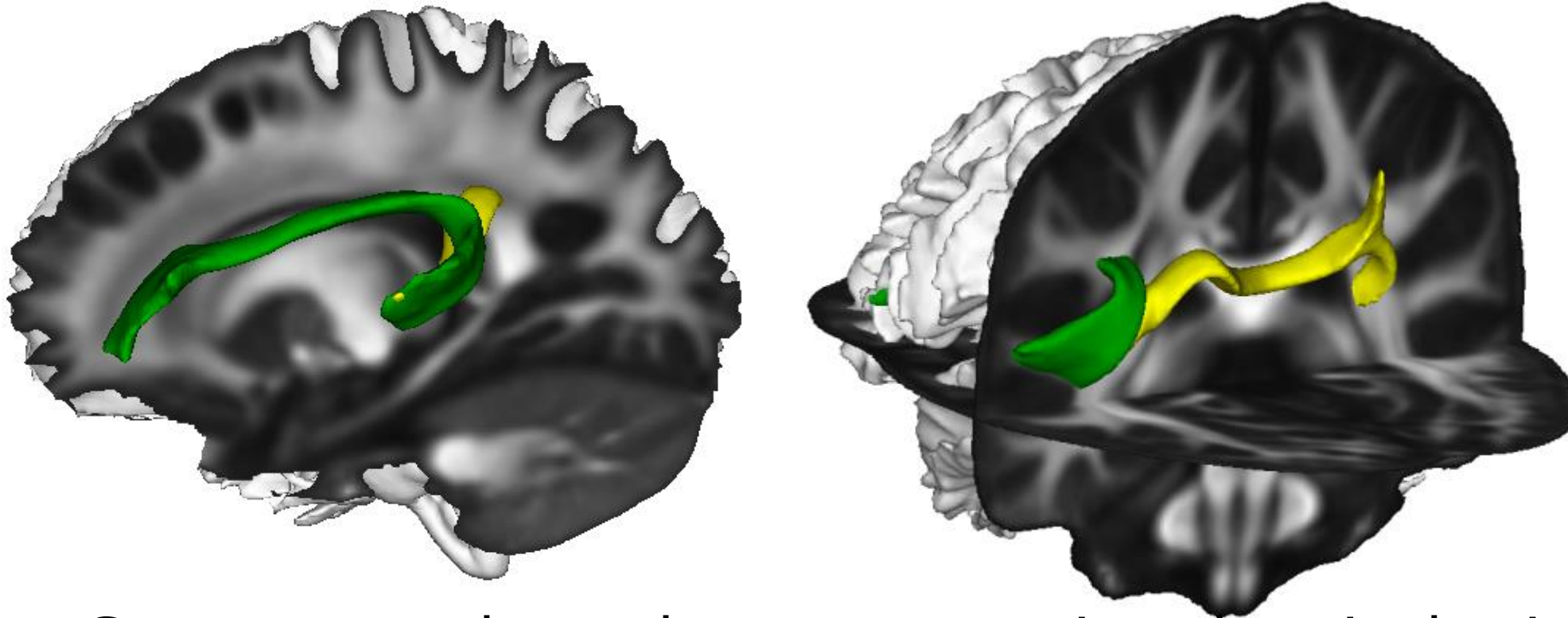
# Statistical comparison: 3 Steps

- 1. Normalize connectivity maps** to common template (using the TBSS no-FA procedure on connectivity maps; without skeletonization).
- 2. Mask noisy voxels** with low connectivity values: Probabilistic tractography is only reliable in region of high connectivity (sufficient sampling).
- 3. Voxel based statistics** using SPM with cluster level correction





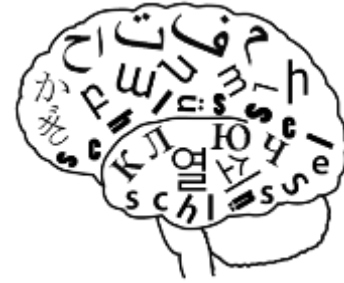
# Mother tongue comparison ( $T_0$ ) – German vs Arabic



Helyne  
Adamson

- German speakers show stronger intrahemispheric connectivity (**green**) (prob. Tract. From post. STP)
- Arabic speakers: stronger interhemispheric connect. (**yellow**)

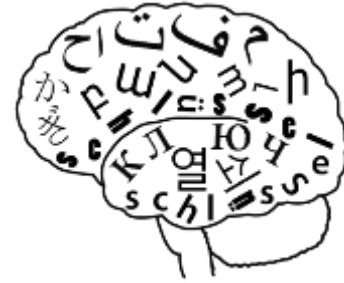




The **language network**, through **lifelong** exposure, bears **traces** of a subject's mother tongue

How does this **mature** network **change** when **learning** a second language?

# Language fMRI experiment L1/L2



- **Lexical task (word level semantic) :**
  - Word list with matching / non-matching target word; ex.:  
*"house – apartment – room      target word: **door**"*
- **Sematic task (sentence level):**
  - Sentence with matching / non-matching target word; ex.:  
*"The hardworking student reads in the library **a tree**"*
- **Grammar task:**
  - Grammaticality judgment of a sentence  
*"The book, that read me, is long."*



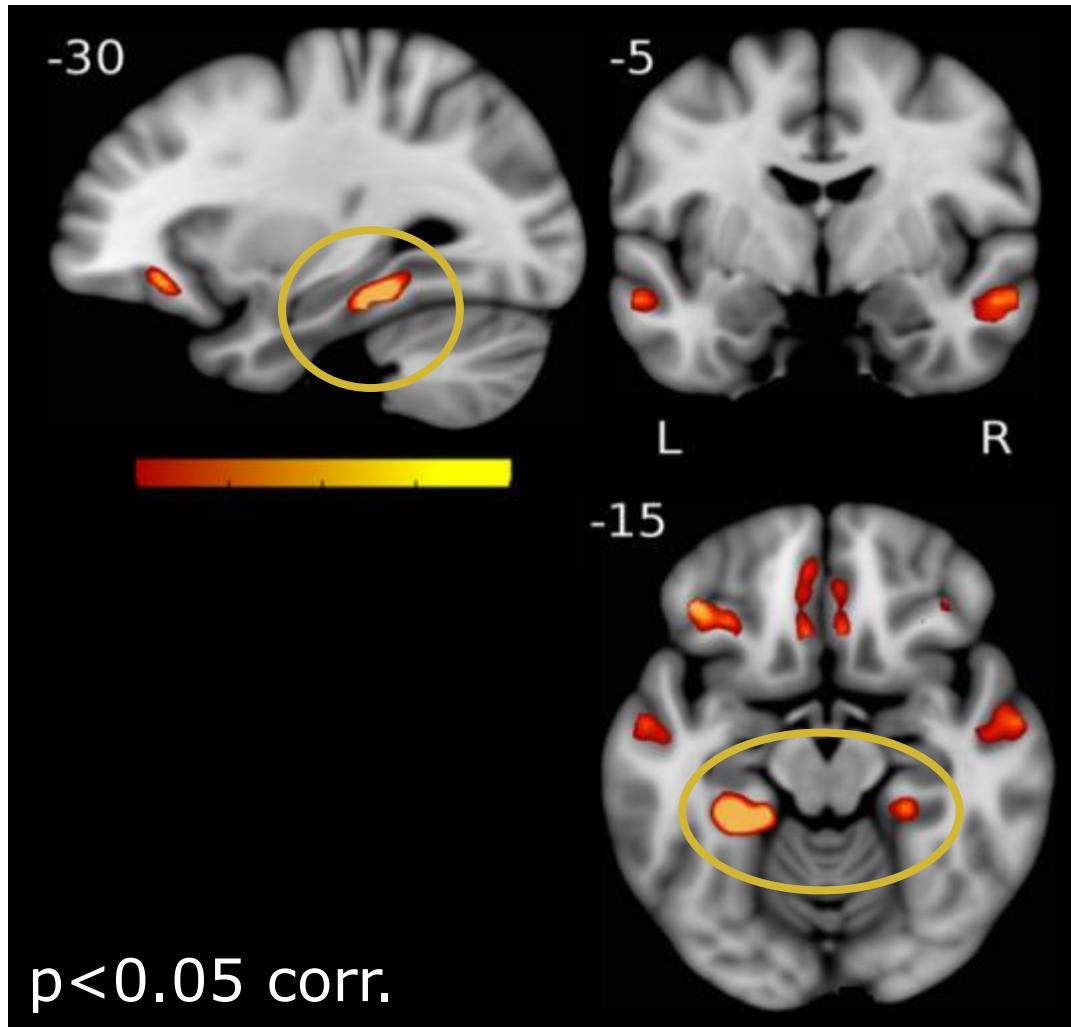
Martin  
Lisanik



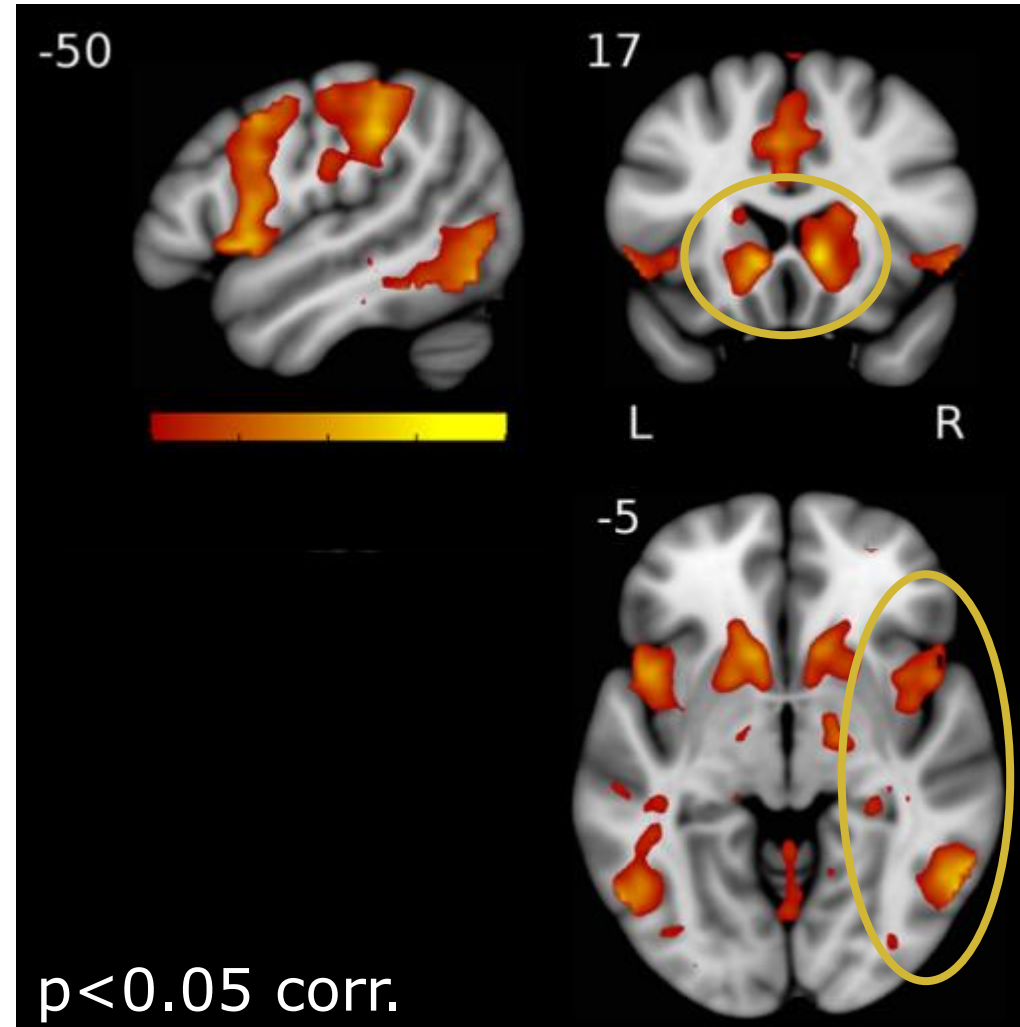
# L2 fMRI after 3 months learning



fMRI semantic > lexical task

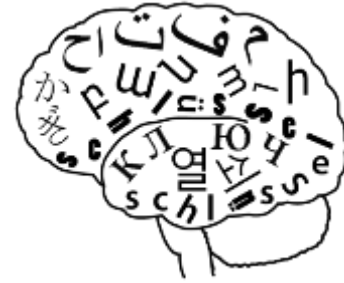


fMRI syntactic > lexical task





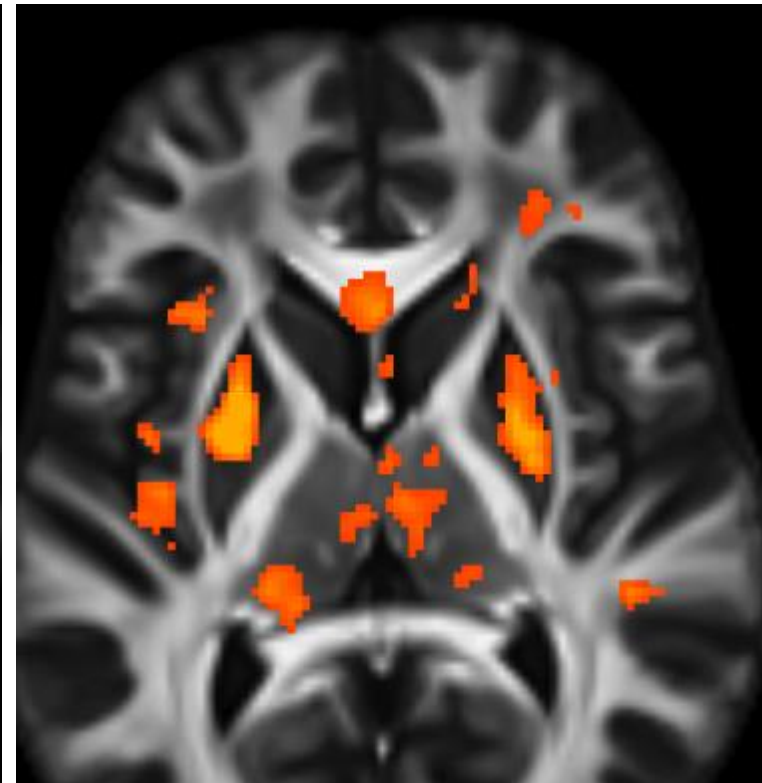
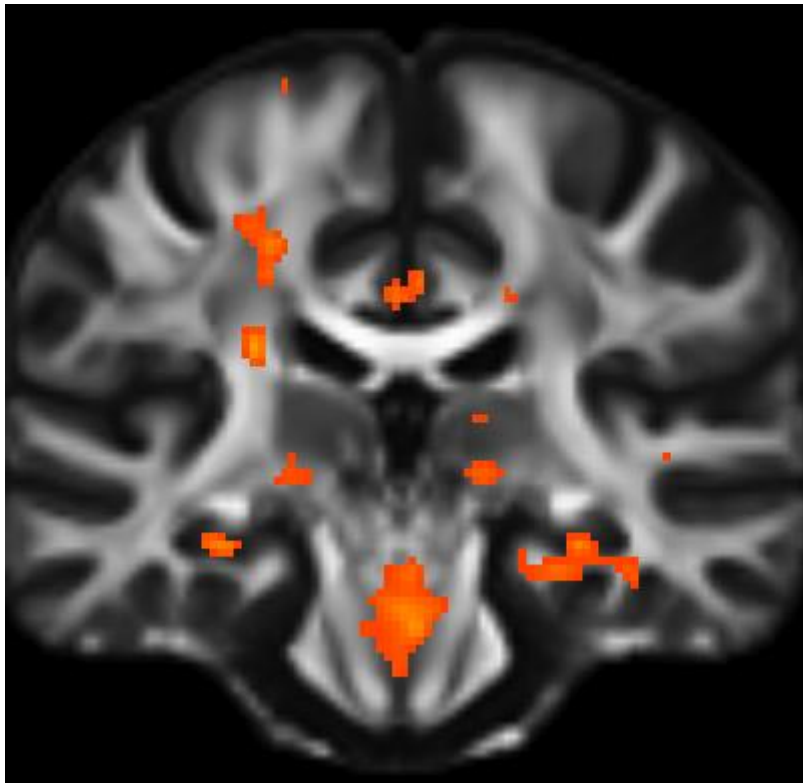
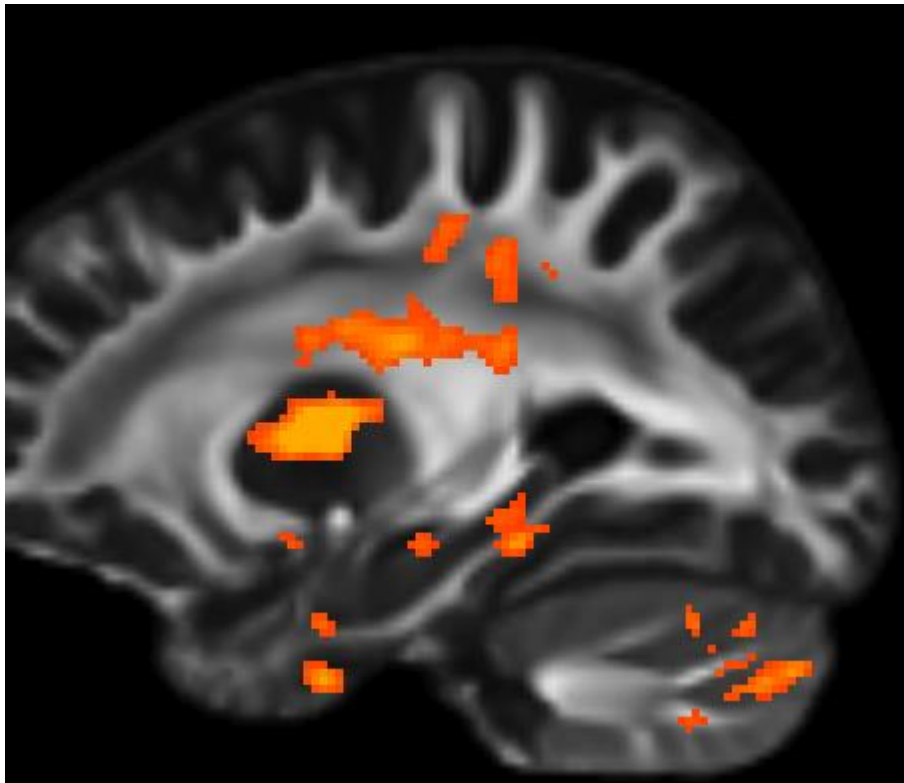
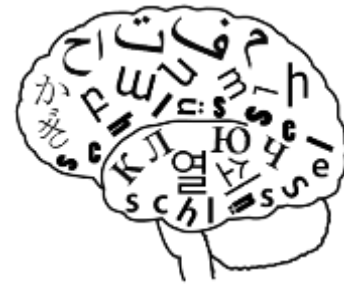
# Longitudinal diffusion MRI analysis



- 3\* 60 diffusion directions, **1.3 mm isotrop**
- **dwidenoise** (MrTrix)
- **TopUp/eddy** artefact correction (FSL)
- DTI fit and FA computation
- ANTS **within subject** and **group FA template** generation
- Normalization on single subject and group template
- 3mm FWHM smoothing
- SPM – VBS statistics:
  - **f-test** on all timepoints and
  - **t-test** between timepoints



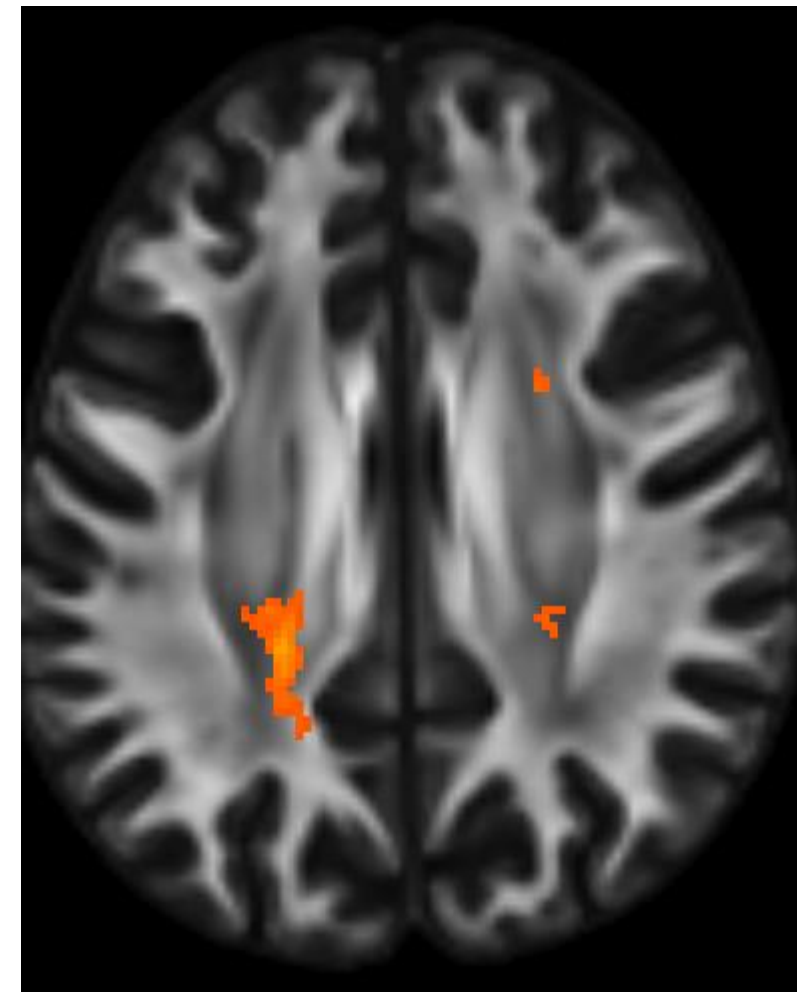
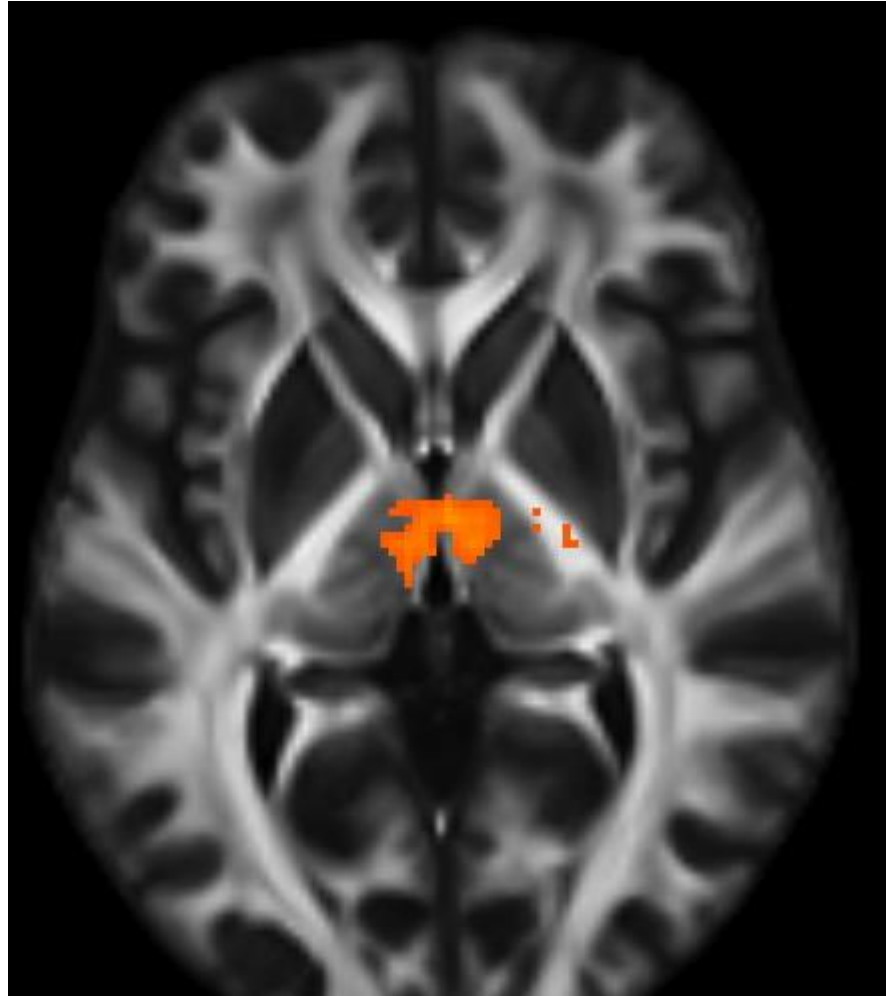
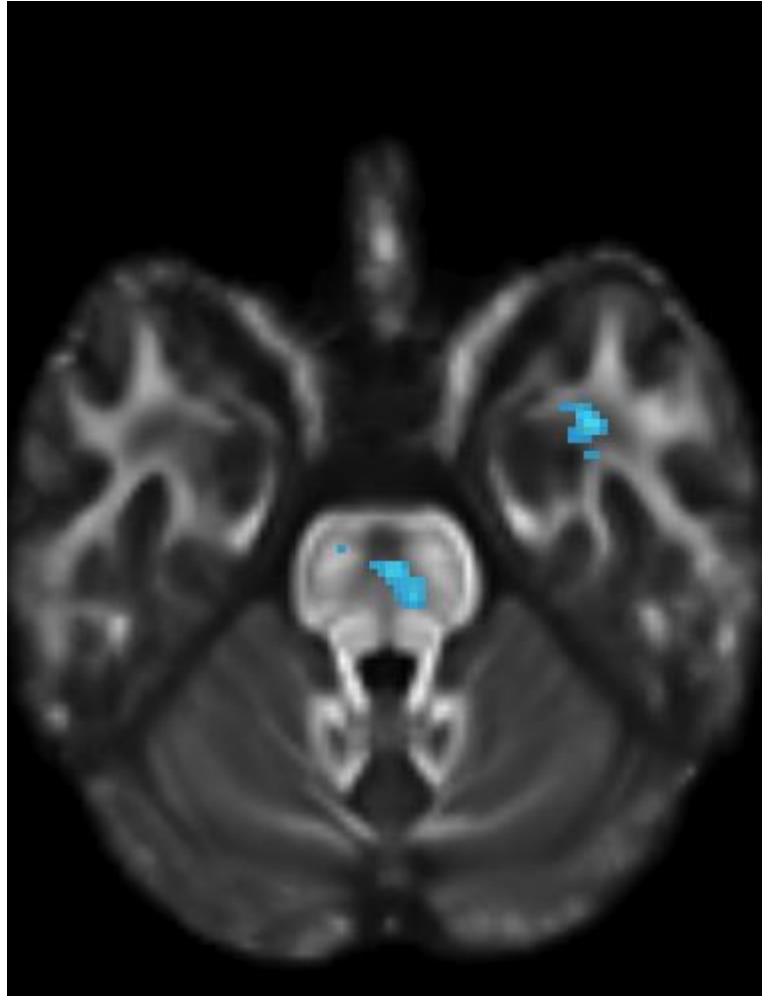
# FA changes within 6 months learning



- Clusters ( $p < 0.05$  corr.) of significant FA changes ( $N = 56$ ) after learning German as second language (f-test)



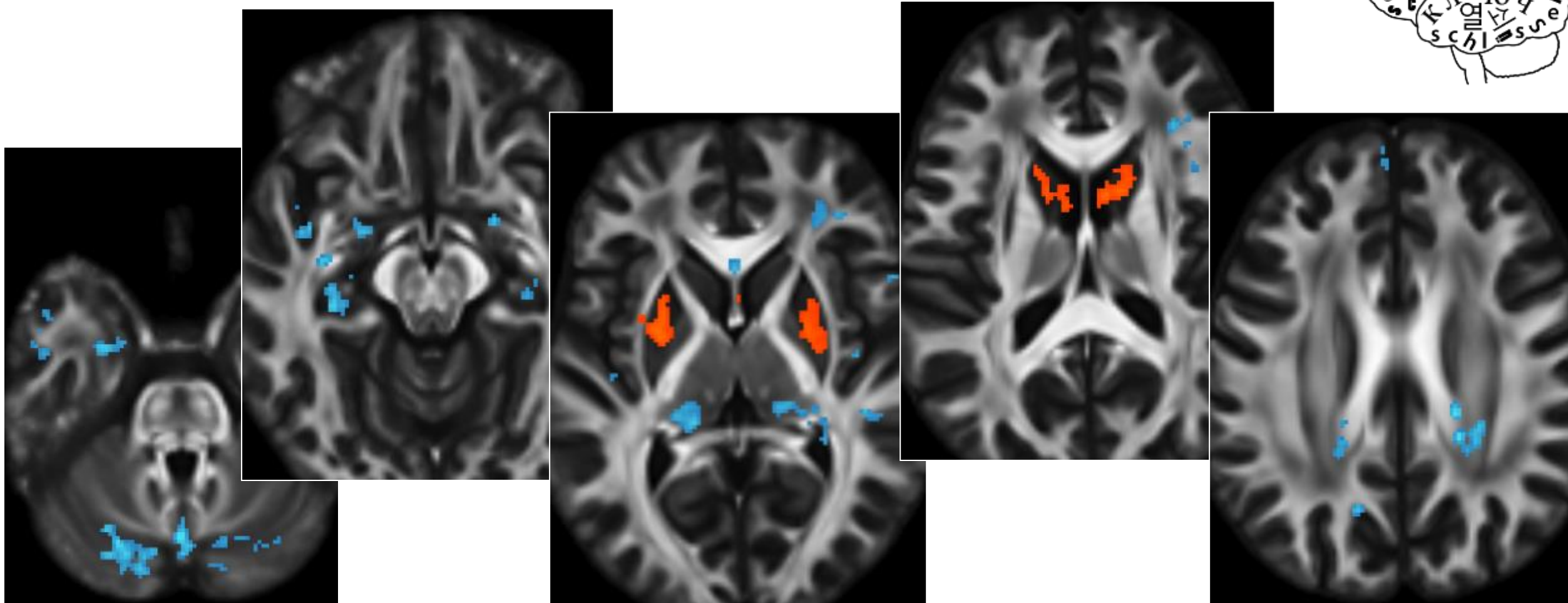
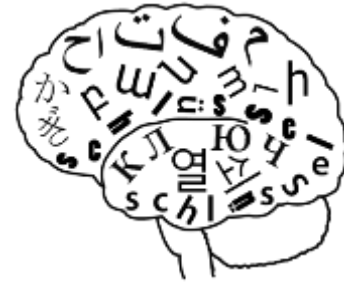
## FA increase/decrease: month 0-3



- Clusters ( $p < 0.05$  corr.) of significant FA changes (N=56)  
**blue: decrease; orange: increase**



# FA increase/decrease: month 4-6



- Clusters ( $p < 0.05$  corr.) of significant FA changes (N=56)  
**blue: decrease; orange: increase**





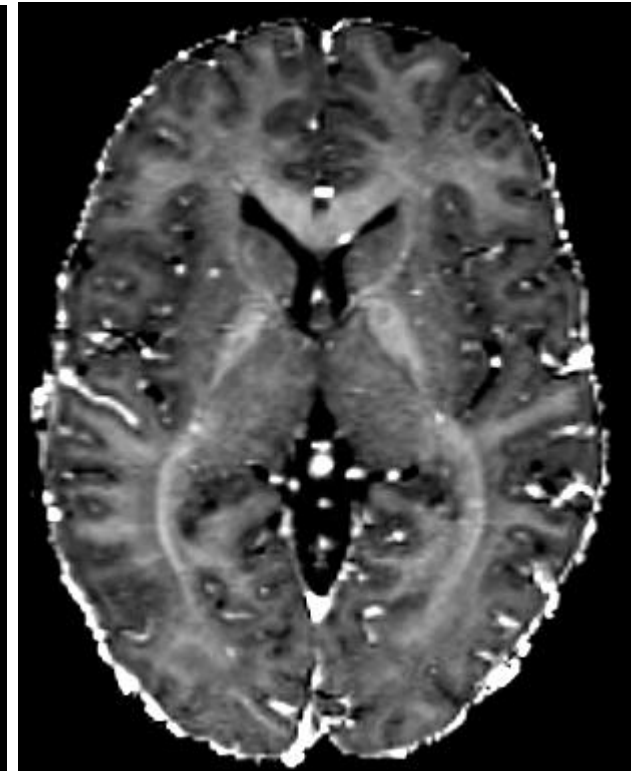
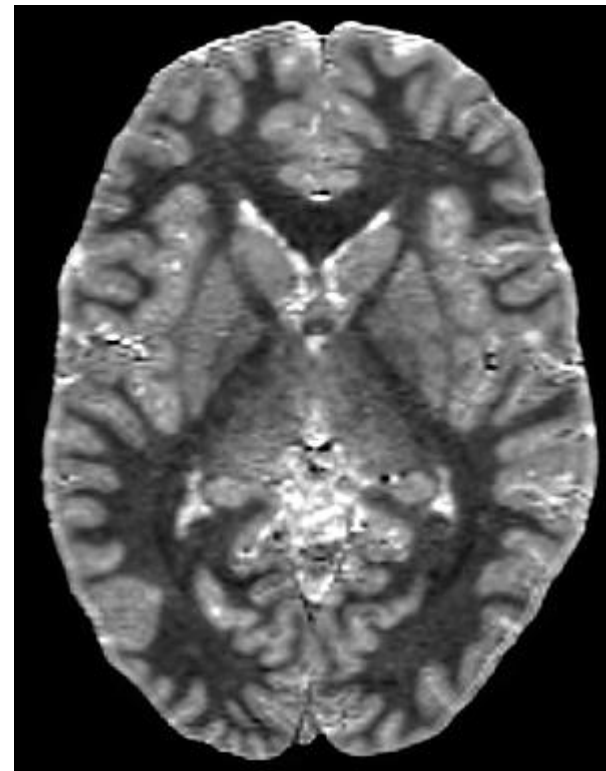
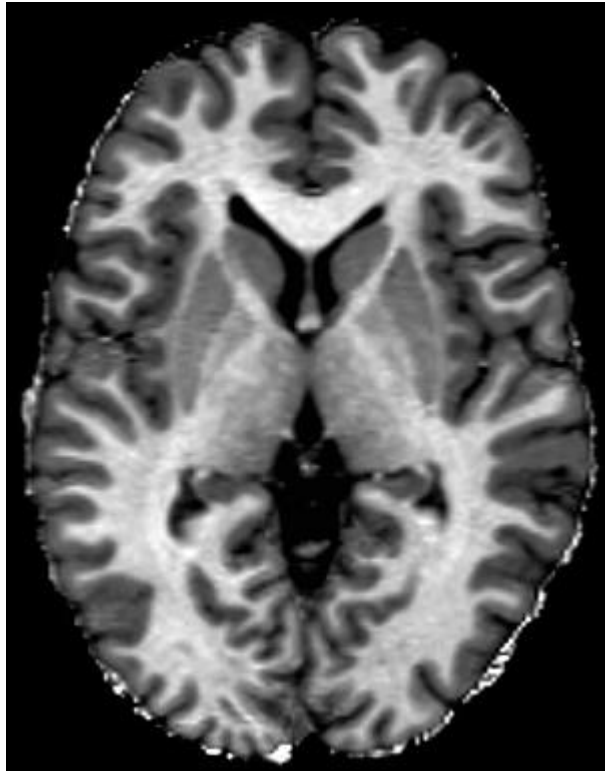
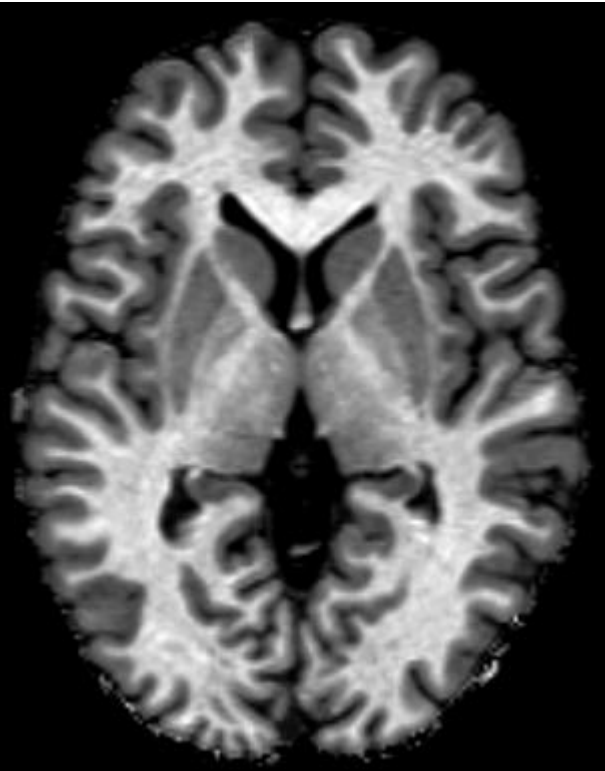
# Longitudinal analysis of quantitative MPMs

**MT maps  
(magnetization  
transfer)**

**R1 maps (T1  
relaxation rate)**

**PD maps  
(proton  
density)**

**R2\* maps (T2  
relaxation rate)**



*Weiskopf et al., CurrOpinNeurol 2015*



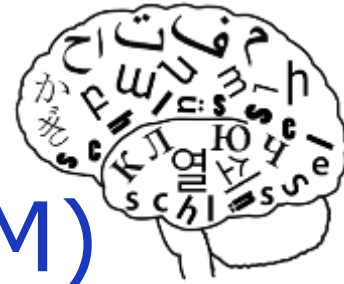
@AlfredAnwander

anwander@cbs.mpg.de

CoBCoM 2017, Juan-les-Pins

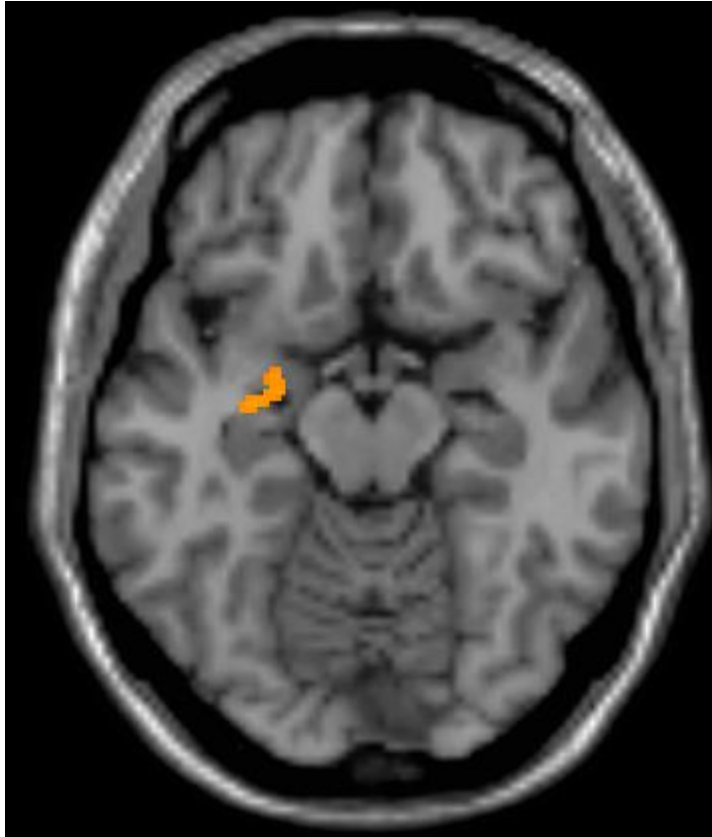
Max Planck Institute for Human Cognitive and Brain Sciences

# Longitudinal analysis of quantitative multiparametric maps (MPM)



- 1mm isotropic
- Processing with the **SPM-VBQ** toolbox
- Segmentation, normalization
- Tissue specific smoothing (5mm FWHM)
- T-Test between timepoints (SPM)

# Preliminary results: MT changes month 0-3



- **orange: increase** in 3 months within **gray matter**  
Clusters ( $p < 0.05$  corr.) of significant MT changes (N=56)

# Preliminary results: R1 changes in 3/6 months



- **orange: increase** in 6 months within **white matter**
  - **blue: decrease** in the first 3 months within the **gray matter**
- Clusters ( $p < 0.05$  corr.) of significant R1 changes (N=56)



# Relate changes to language performance

- Cognitive assessment
- Language proficiency
  - comprehension, production
  - semantics
  - phonetic
  - grammaticality judgement
- Executive functions
  - e.g. working memory



## Conclusion and perspectives

- Understand the biological mechanisms of brain plasticity
- Use of additional quantitative modalities to characterize the dynamic changes (**NODDI**, tract based analysis)
- Build combined models of the multiparametric maps and the diffusion parameters including **axonal diameter**
- Use of machine learning and multivariate analysis to predict performance from the brain data





**Thank you!**

**شكراً جزيلاً!**

**Nik Weiskopf**

**Angela D. Friederici**

**T. Goucha**

**A. Lutti, T. Leutritz**

**T. Witzel**

**M. Schwendemann**

**M. Lisanik, H. Adamson**

**Departments of**

**NPHY and NPSY @**

**MPI CBS and all**

**collaborators**

**and you**

**for your questions!**